

# Geometric optics

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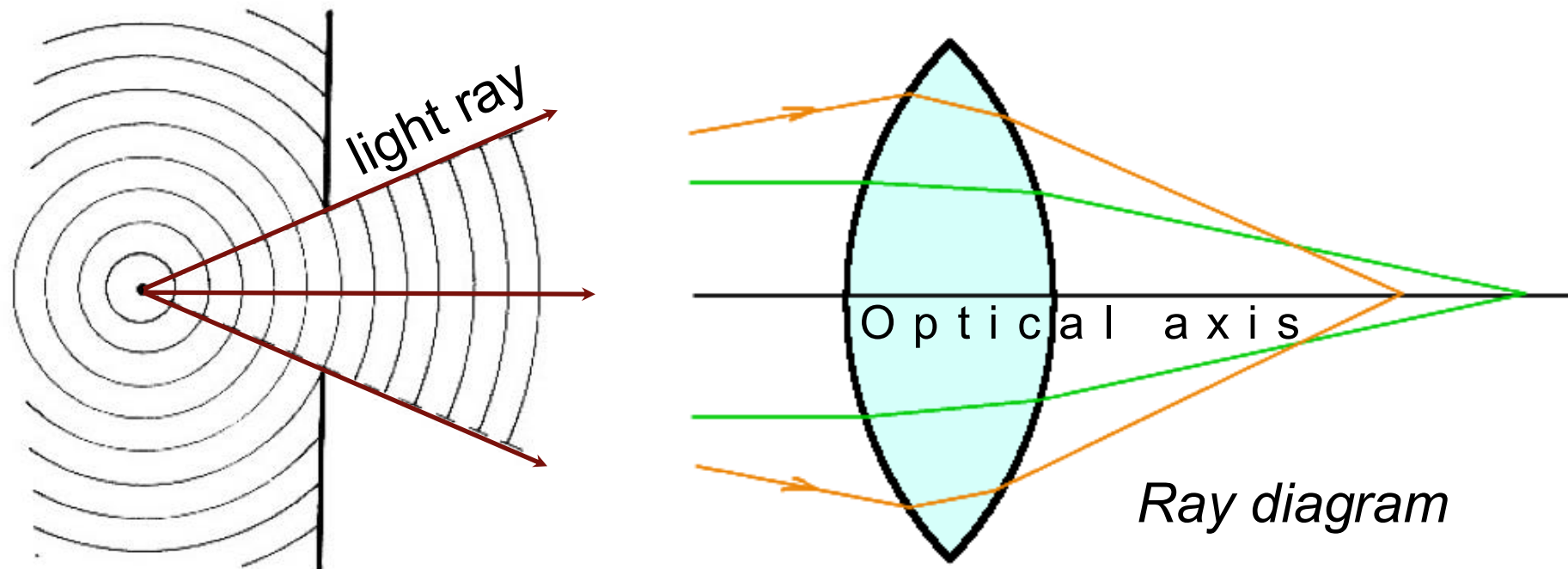


**SEMMELWEIS**  
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# Geometric optics

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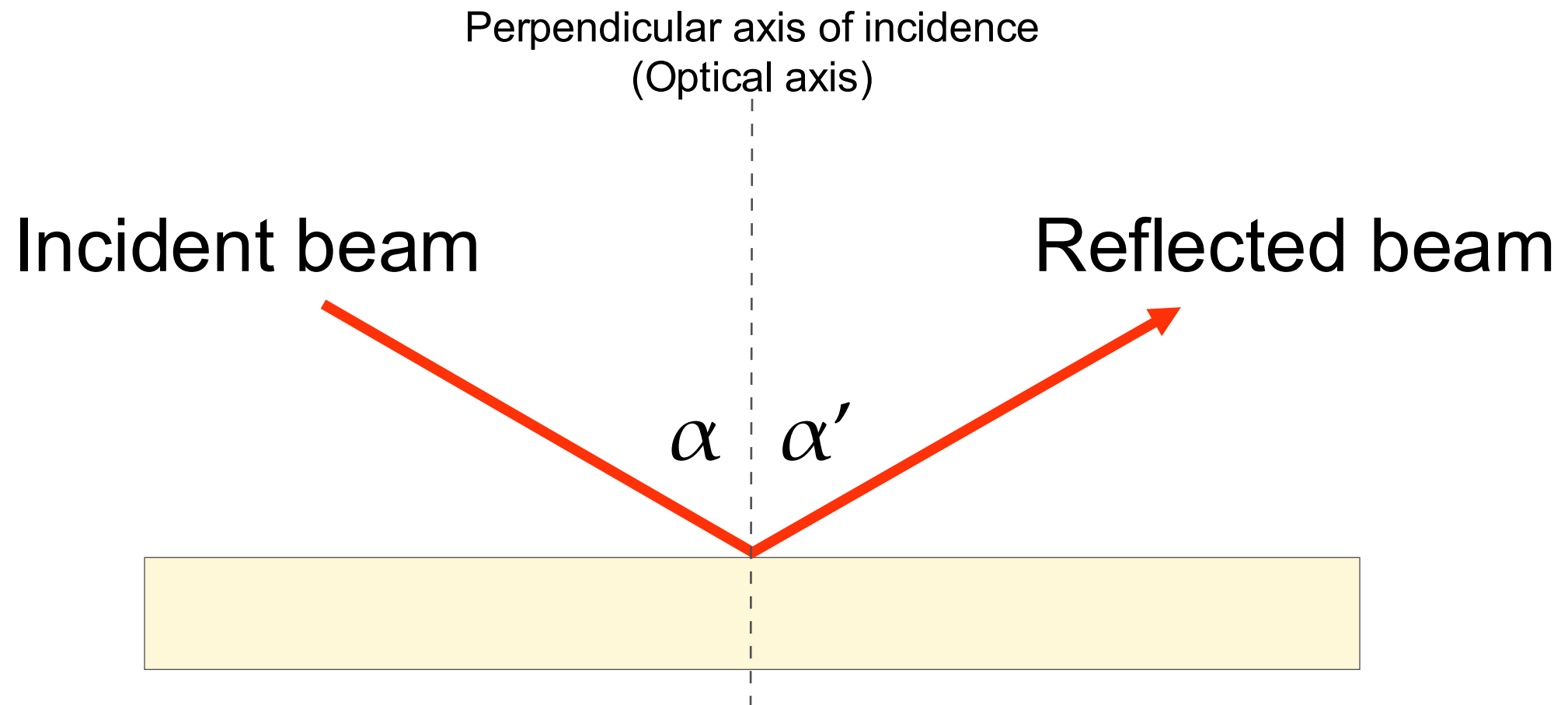
If light propagates through a slit much larger than its wavelength, then the spreading of the wavefront (phase) may be simplified into a line (“light ray”).



- Optical (light) ray (“light beam”): abstraction, mathematical line.
- Arrows represent the direction of energy propagation.
- Optical axis: line connecting the midpoint of optical components (e.g., lenses).
- Principle of reversibility: the direction of energy propagation (arrows) may be reversed.

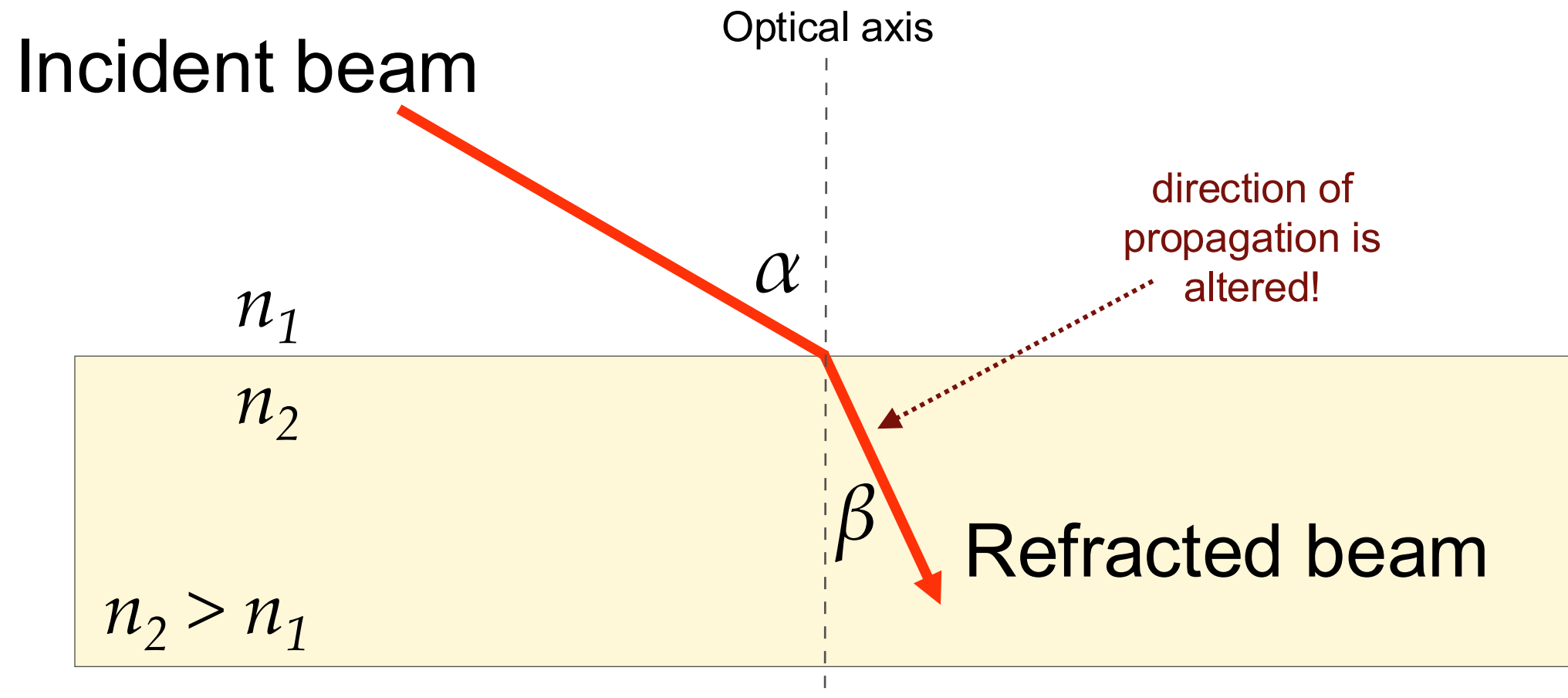
# Reflection

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- $\alpha$  = angle of incidence;  $\alpha'$  = angle of reflection.
- Incident beam, reflected beam and optical axis are in the same plane.
- Incident and reflected angles are identical ( $\alpha = \alpha'$ ).

# Refraction

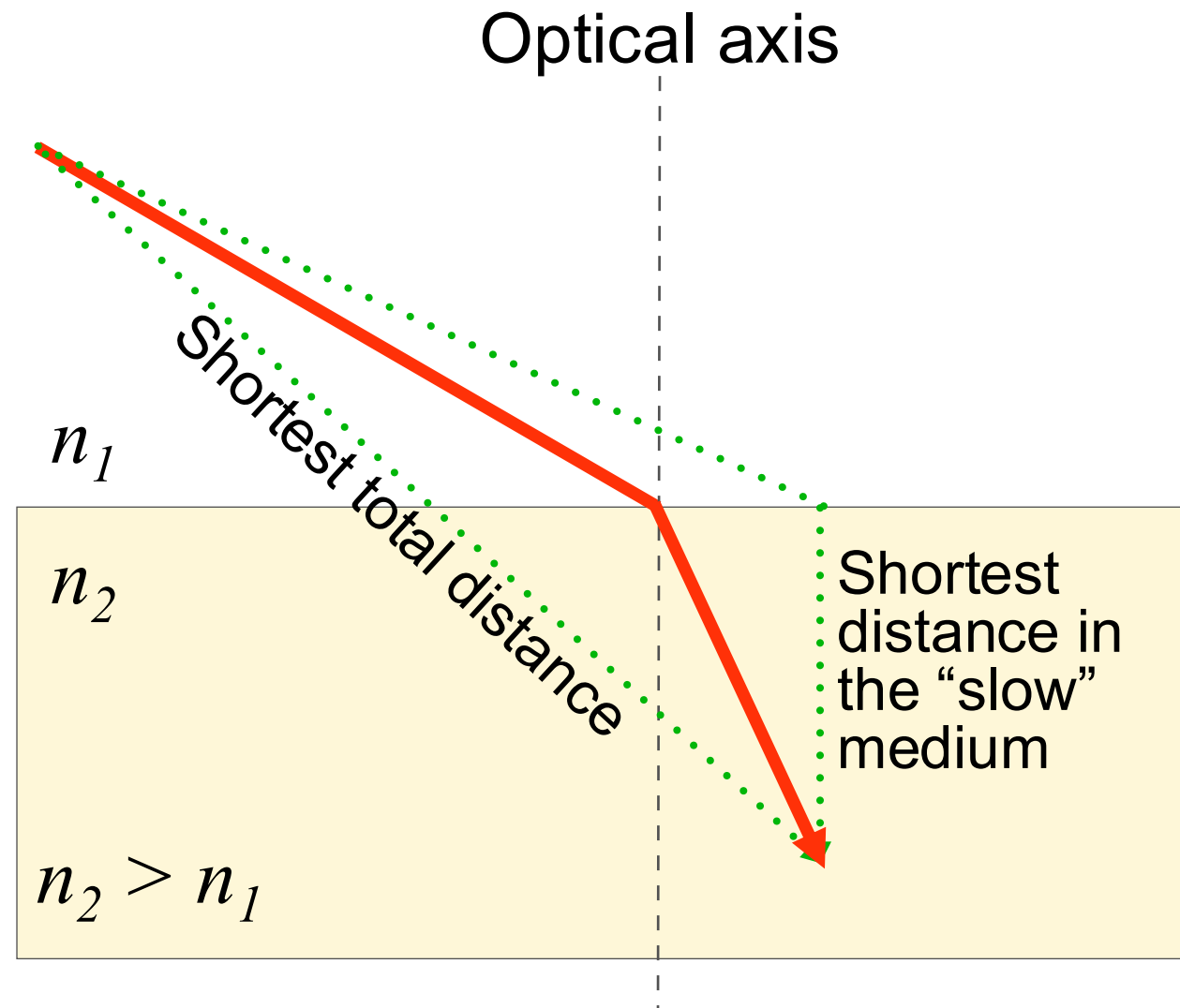


- $\alpha$  = angle of incidence;  $\beta$  = angle of refraction.
- Incident and refracted beams and axis of incidence are in the same plane.
- Snell's law:

$$\frac{\sin \alpha}{\sin \beta} = \frac{c_1}{c_2} = \frac{n_2}{n_1}$$

# Explanation of refraction: Fermat's principle of least times

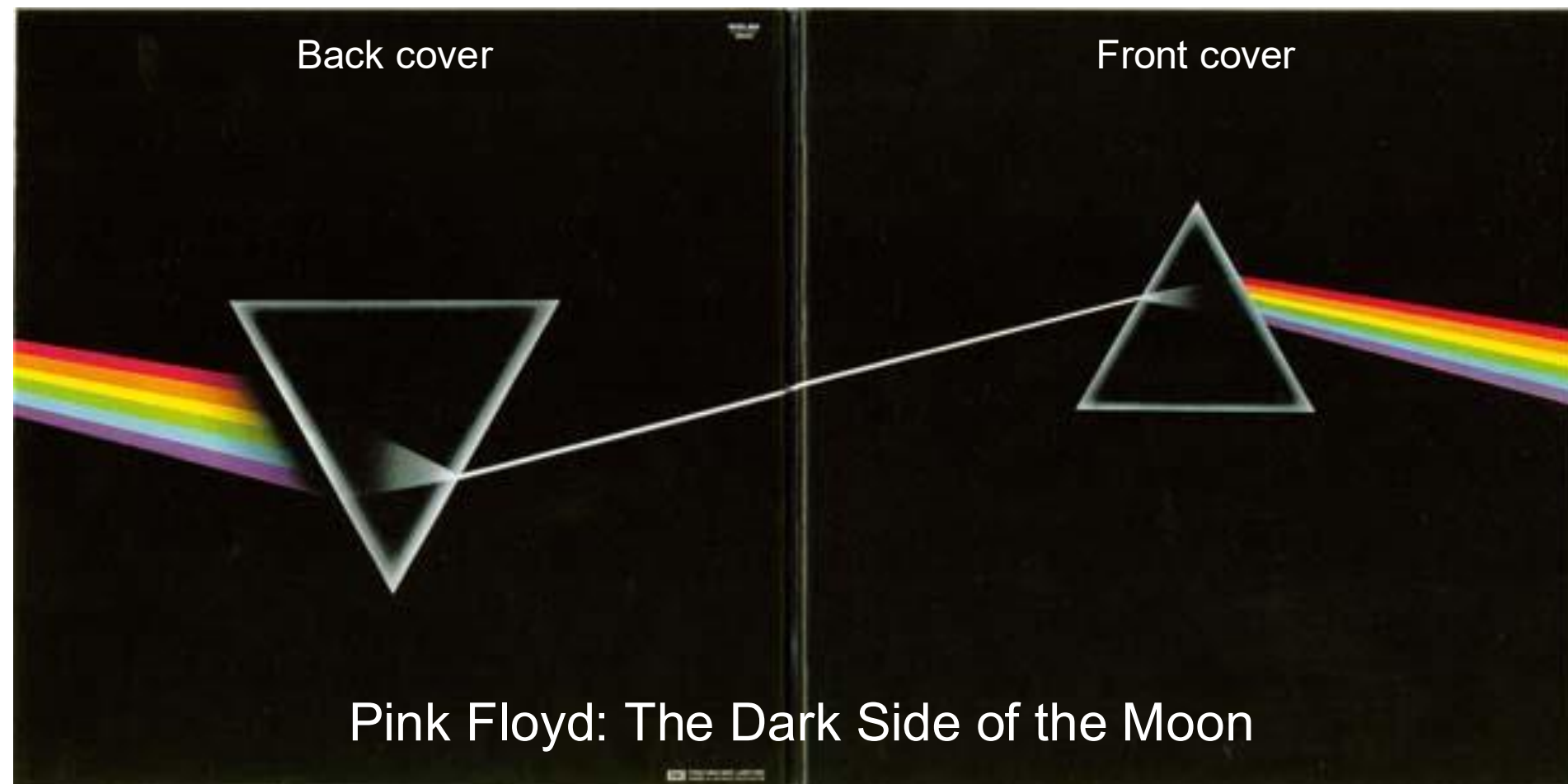
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Light “chooses” the path that can be covered in the least time  
(i.e., fastest).

# Dispersion

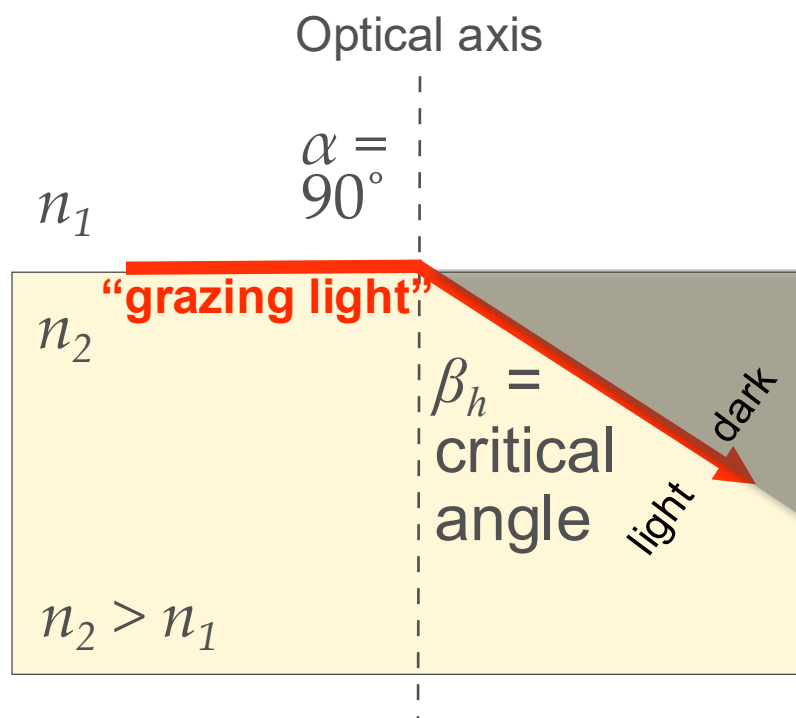
Index of refraction depends on frequency!



- The greater the frequency of light - the greater the refractive index.
- A prism decomposes white light according to frequency (physical color).

# Analytical application of refraction: Refractometry

## Boundary condition of refraction



Since  $\sin(90^\circ) = 1$ , according to Snell's law:

$$n_1 = n_2 \sin \beta_h$$

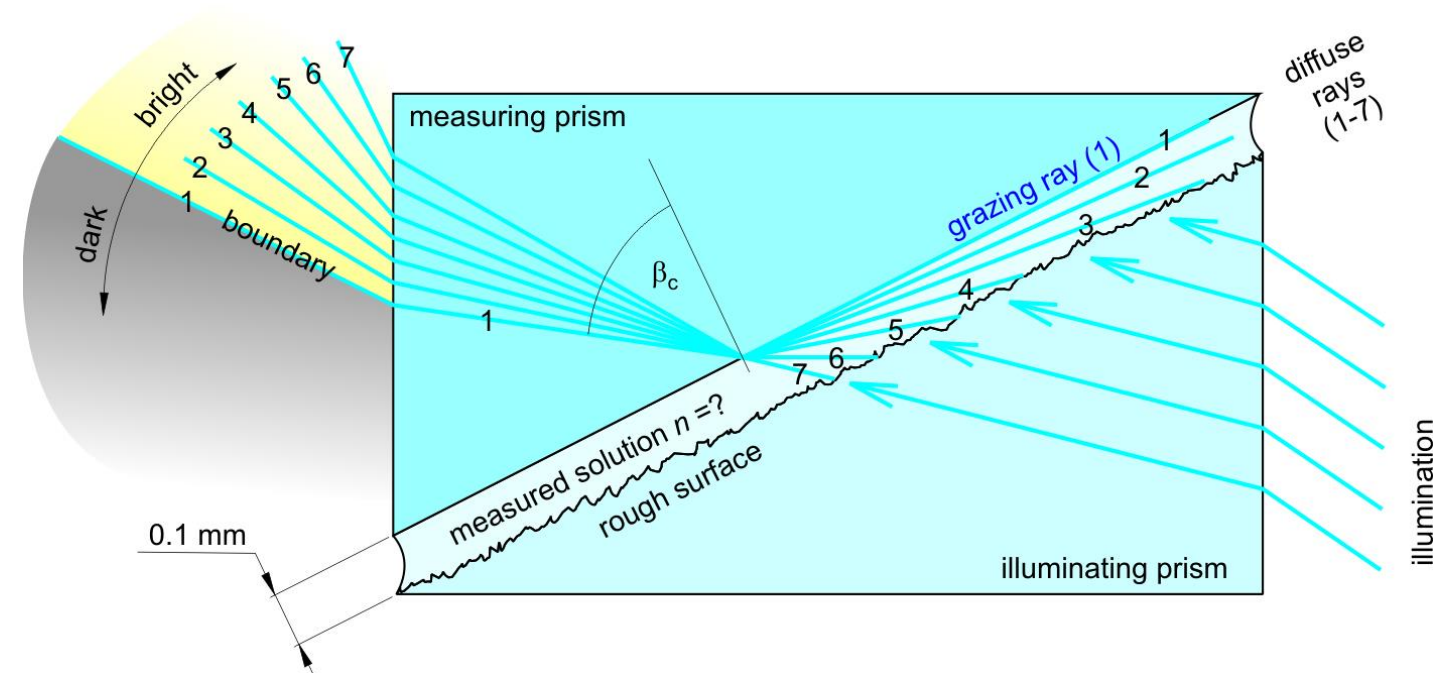
Thus, in case we know  $n_2$ , by measuring  $\beta_h$  the refractive index of the incident medium ( $n_1$ ) may be obtained.

## Refractometry

Refractive index of dilute solutions ( $n_1$ ) depends on solute concentration ( $c$ ):

$$n_1 = n_0 + k \cdot c$$

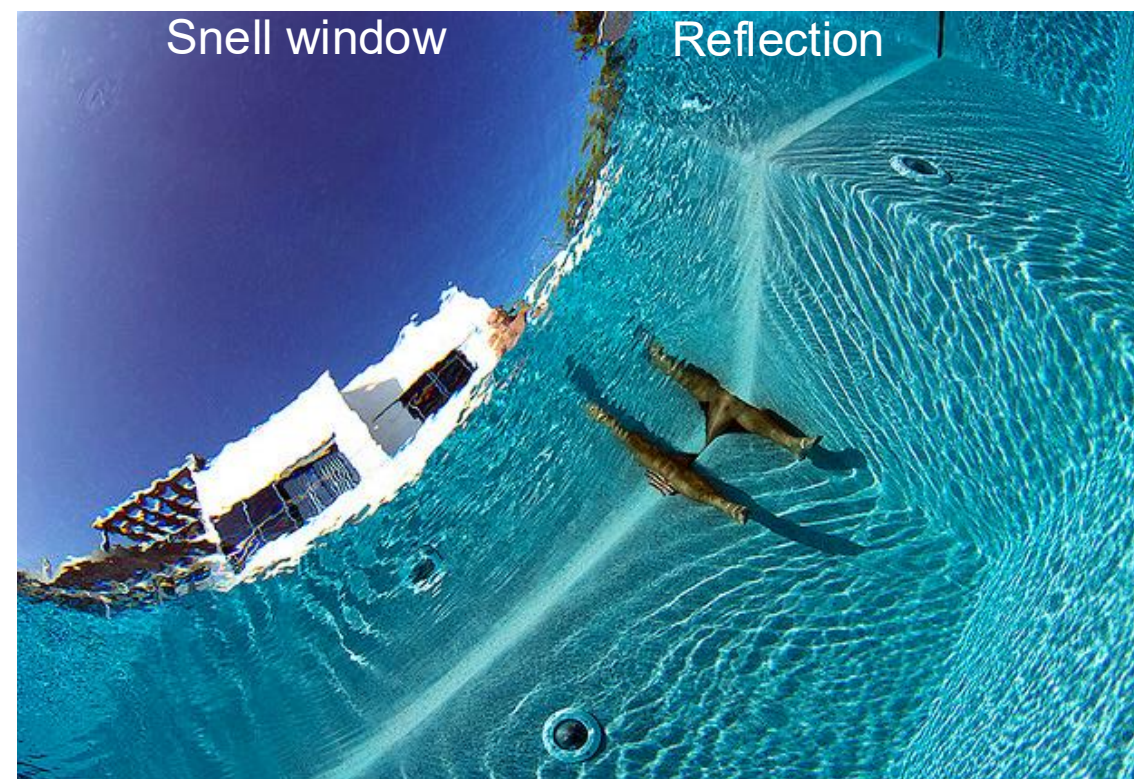
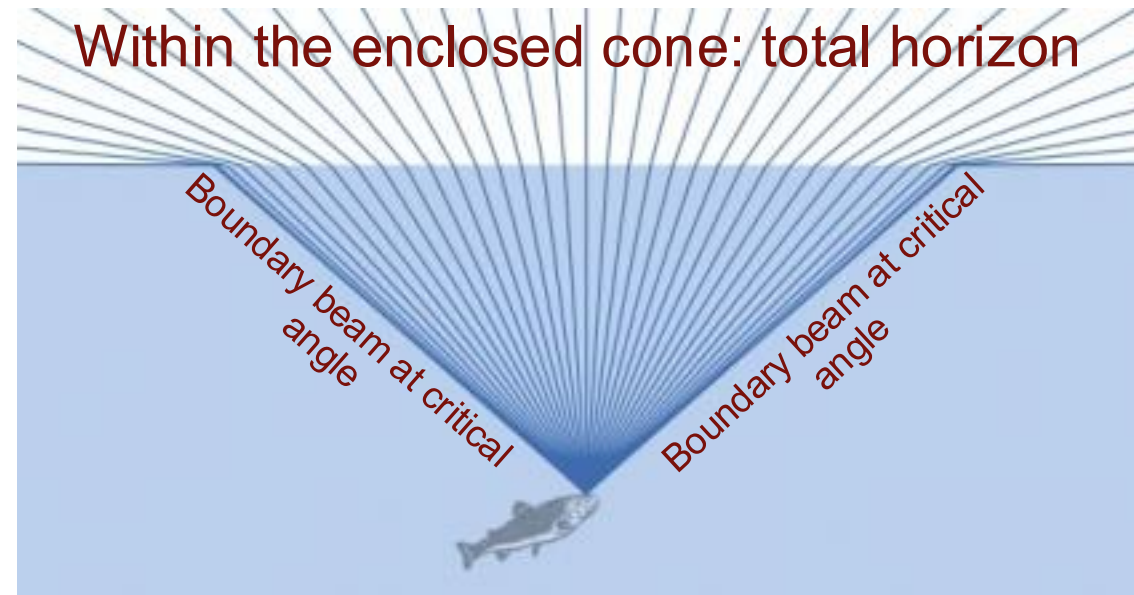
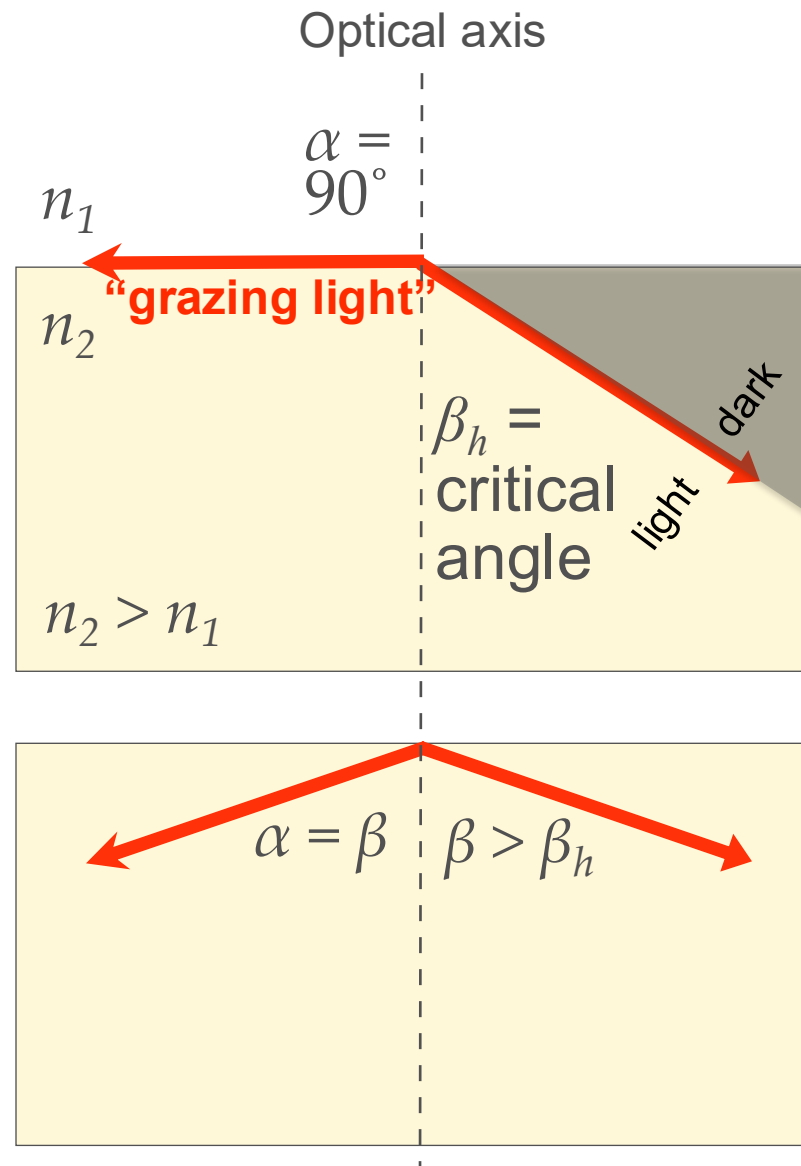
$n_0$  = refractive index of solvent,  $k$  = constant



### Conditions of applicability:

- Liquid sample
- Sample is transparent
- Refractive index of sample is smaller than that of the measuring prism.

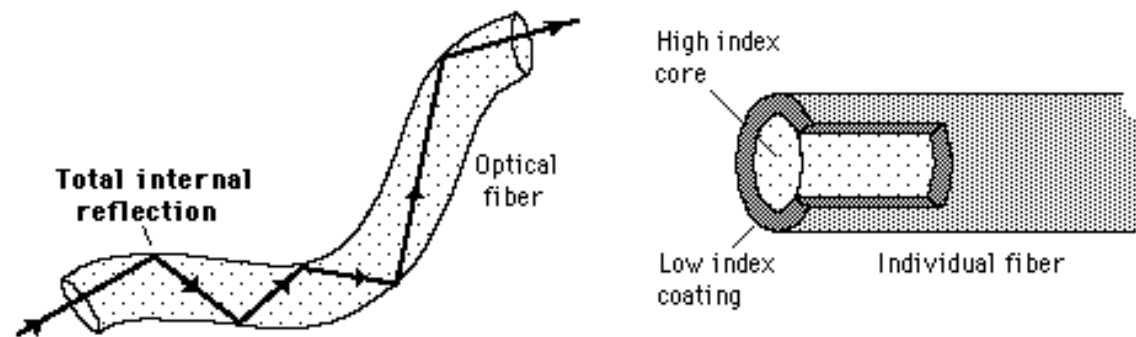
# Total internal reflection



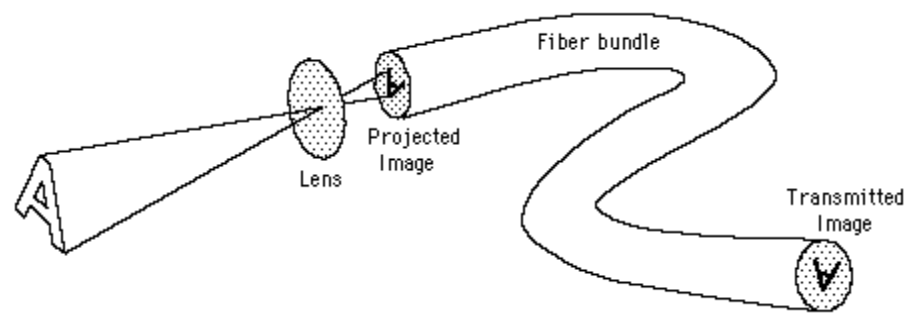
Total reflection within the optical medium of greater refractive index (“total *internal* reflection”, TIR)

# Biomedical Application of TIR: optical fibers

## Single fiber



## Highly ordered fiber bundle



If the arrangement of fibers is maintained within the bundle, then the image is faithfully transmitted.

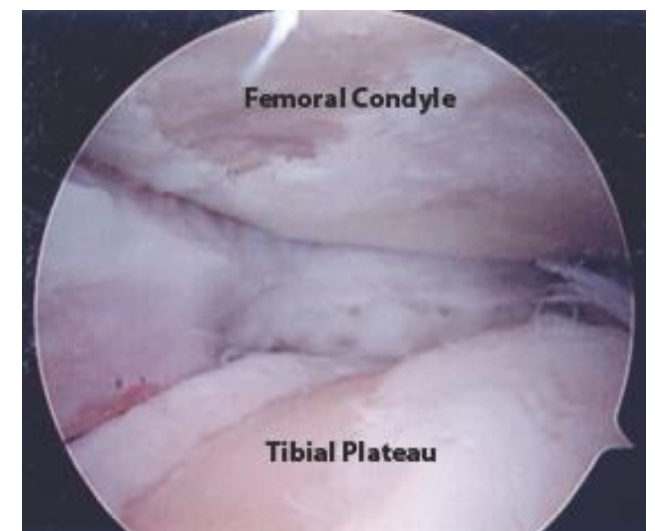
## Endoscopy

### OBJECTIVES

1. Diagnostics: visual inspection, biopsy, contrast agent delivery
2. Therapy: surgery, cauterization, removal of foreign objects

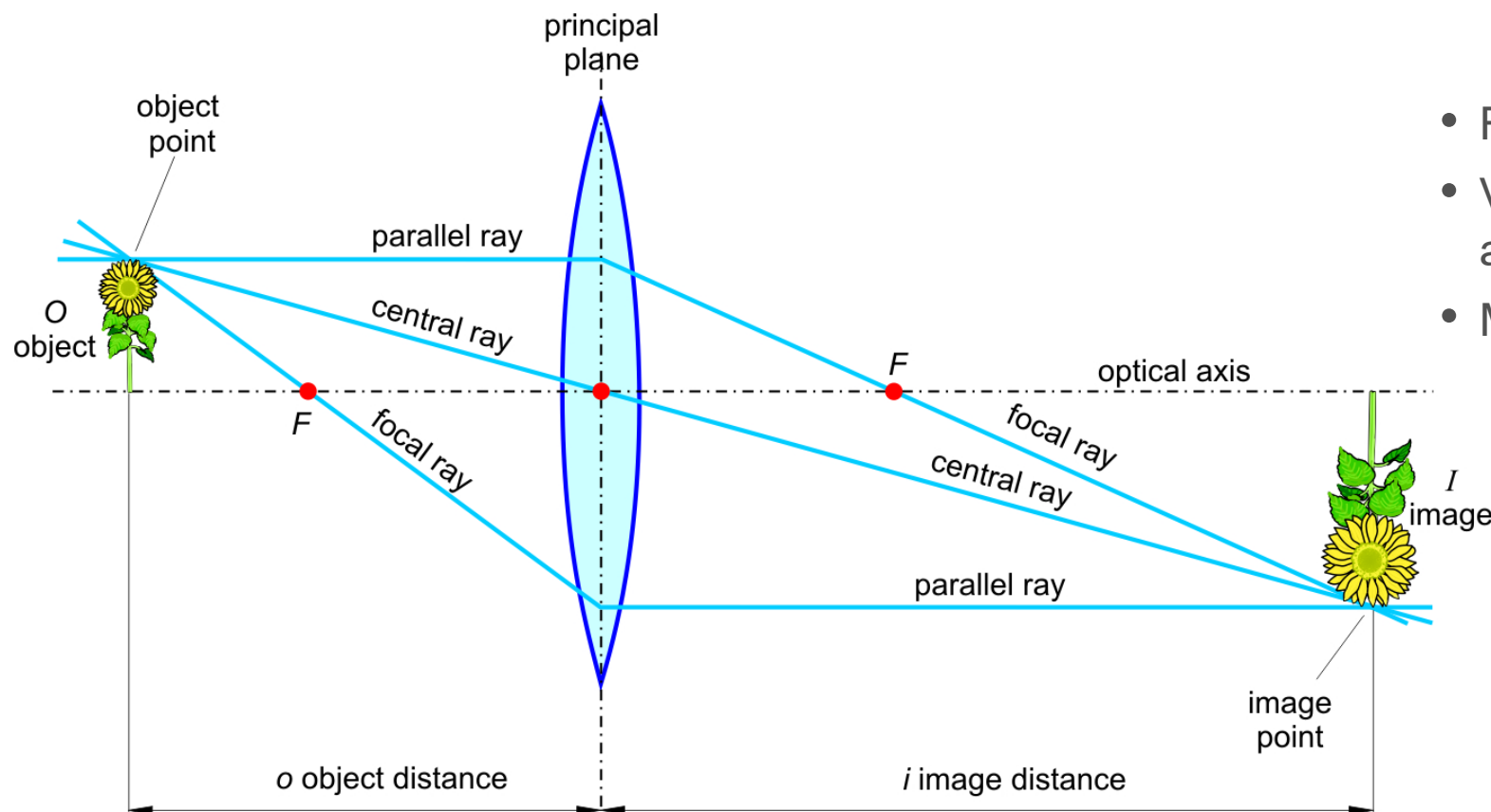
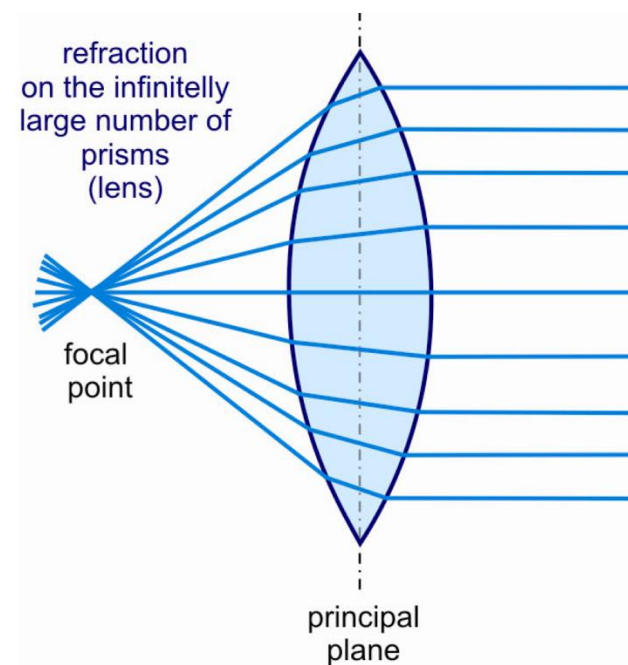
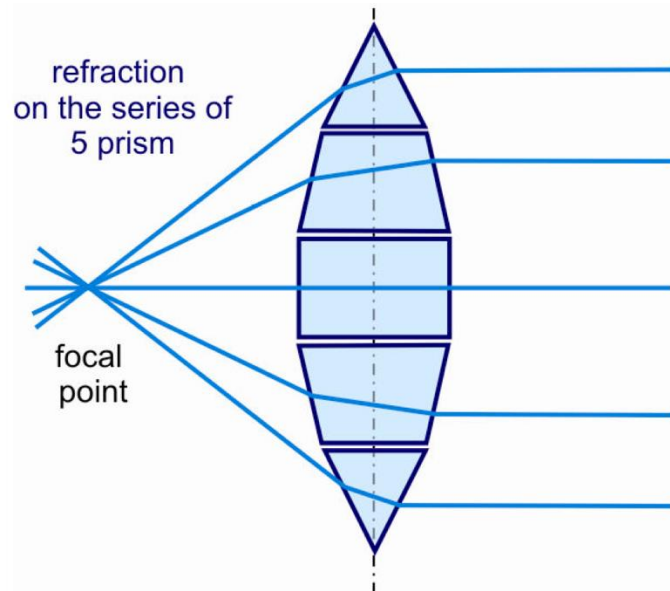
### TYPES

*Arthroscopy* (joints); *Bronchoscopy* (trachea and bronchi); *Colonoscopy* (colon); *Colposcopy* (vagina and cervix); *Cystoscopy* (urinary bladder, urethra uterus, prostate via urethra); *ERCP* (endoscopic retrograde cholangio-pancreatography, delivery of X-ray contrast agent into biliary tract and pancreatic duct); *EGD* (Esophago-gastroduodenoscopy, upper GI tract); *Laparoscopy* (stomach, liver, female gonads via abdominal wall); *Laryngoscopy* (larynx); *Proctoscopy* (rectum, sigmoidal colon); *Thoracoscopy* (pleura, mediastinum and pericardium via chest wall)



Arthroscopic surgery

# Refraction on curved surface



- Real image: may be projected onto a surface
- Virtual image: may be mapped by using an accessory lens
- Magnification  $> 1$ , if the object is within  $2f$  distance:

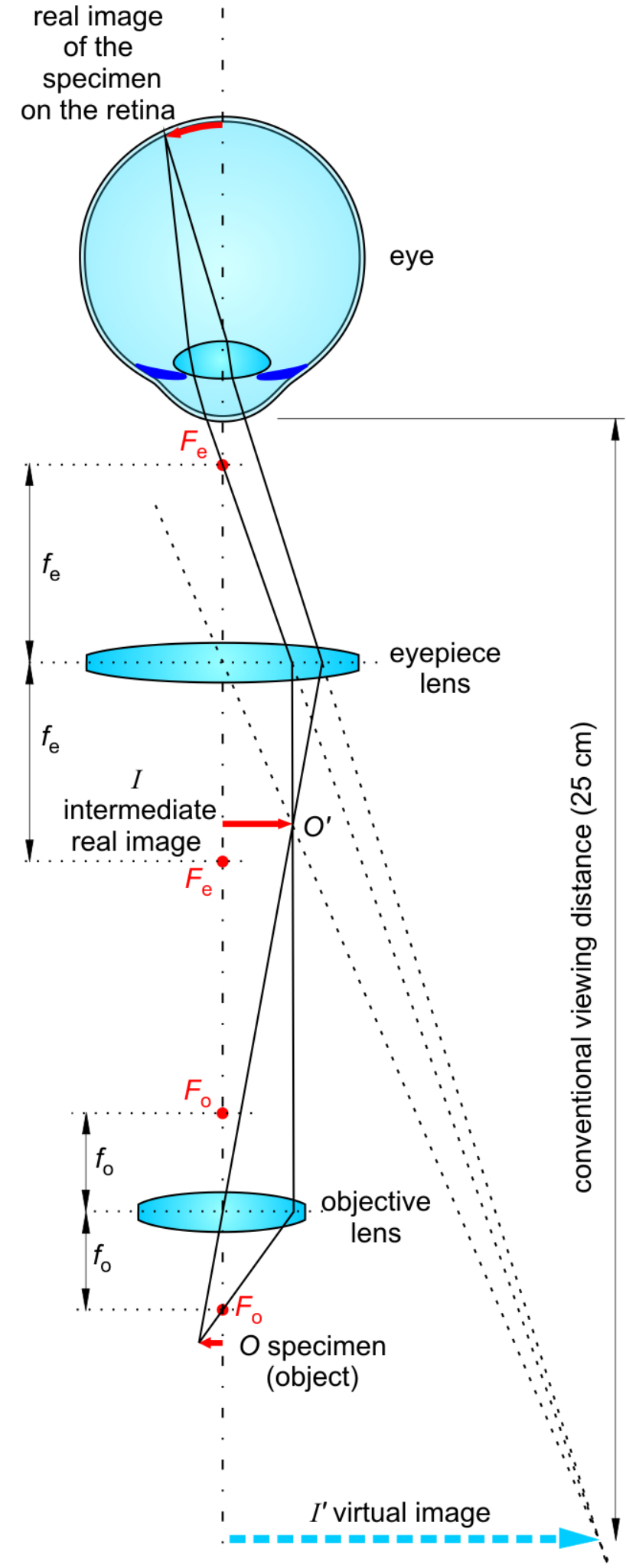
$$N = \frac{K}{T} = \frac{k}{t}$$

Lens equation: 
$$D = \frac{1}{f} = \frac{1}{t} + \frac{1}{k}$$

$D$ =optical power (diopter,  $m^{-1}$ )

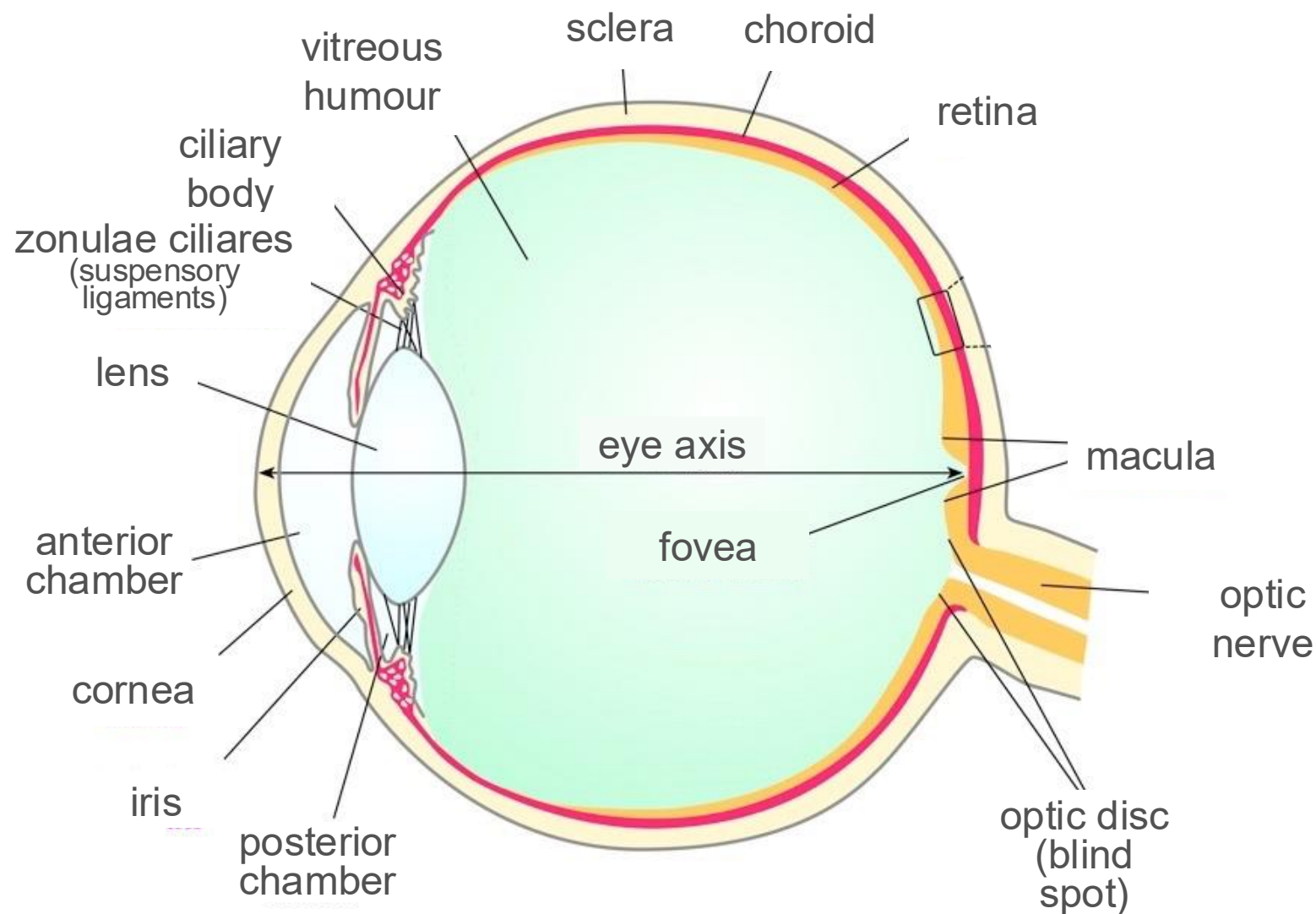
# Image formation in the compound microscope

- Magnified, up-side-down, virtual image
- Condition of the formation of projected image: an accessory lens (eye lens) needs to be positioned in the optical path.
- Projection screen: retina



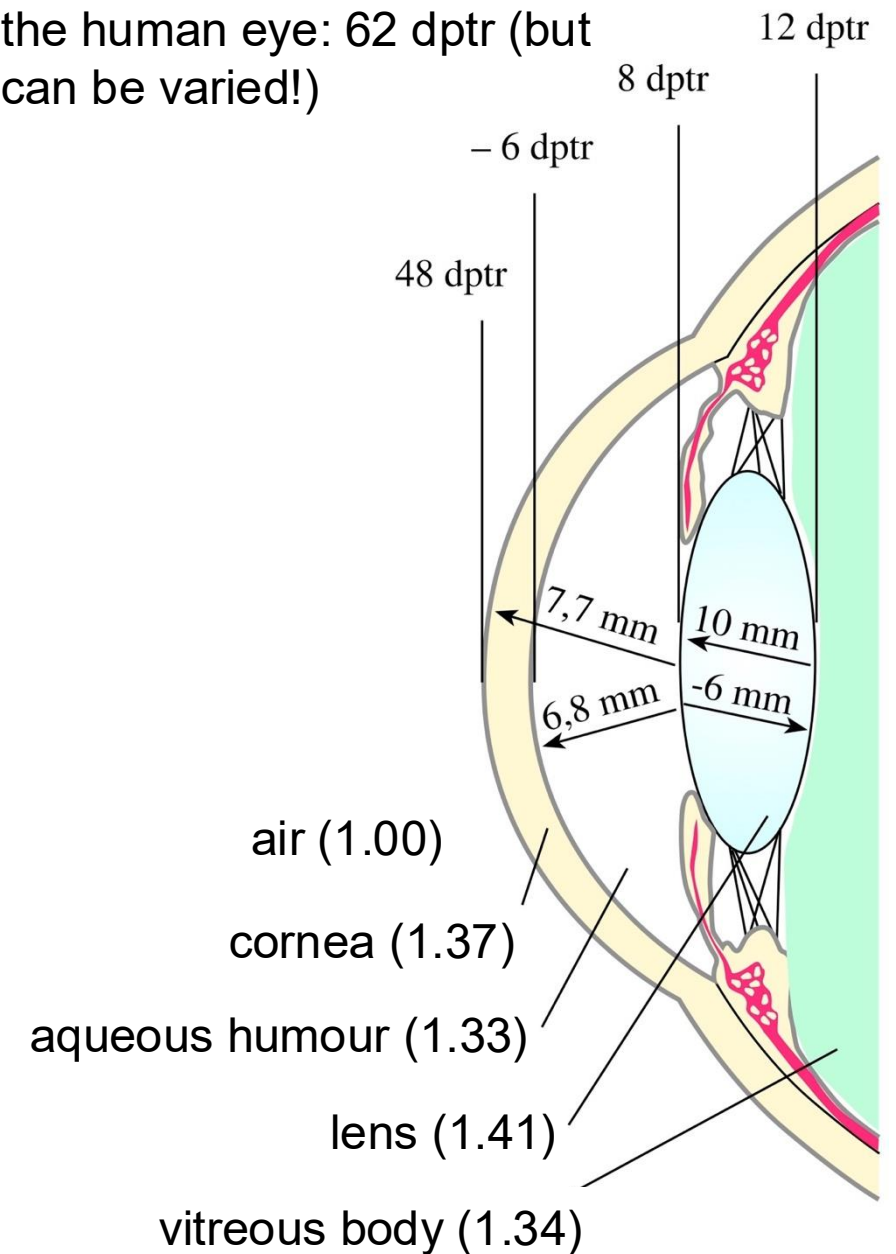
# Optics of the human eye

Demagnified, up-side-down, real image is formed on the retina.



Horizontal section of the human eye

Total refractive power of the human eye: 62 dptr (but can be varied!)



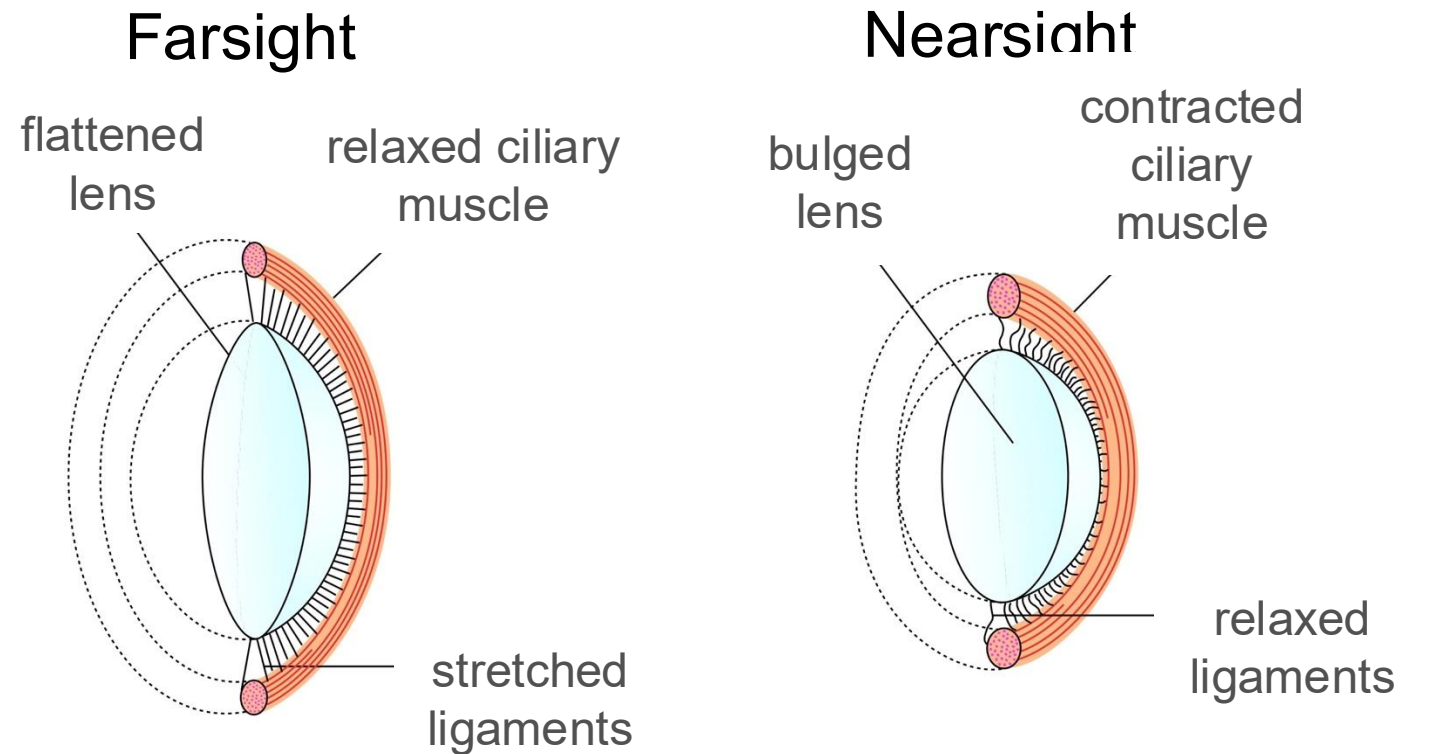
$$D = \frac{n - n'}{r}$$

$n - n'$  = refractive index difference of bounding media (air, cornea, etc.)  
 $r$  = radius of curvature of refractive surface

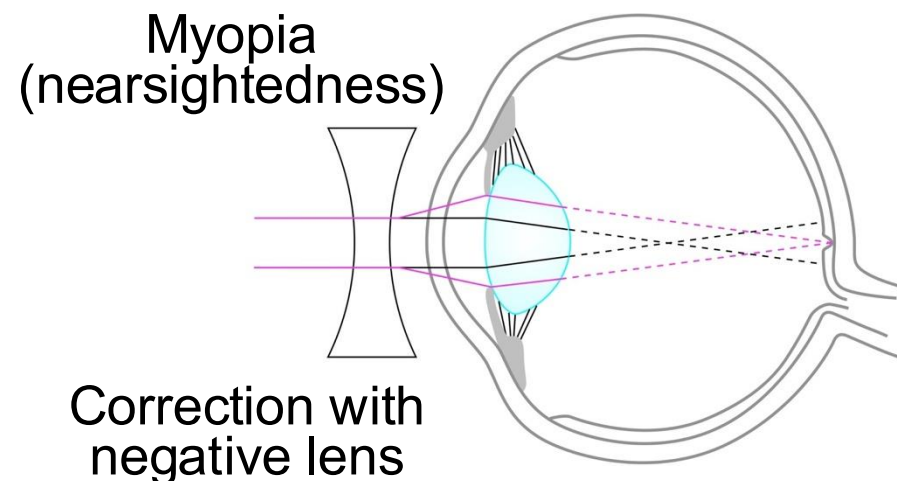
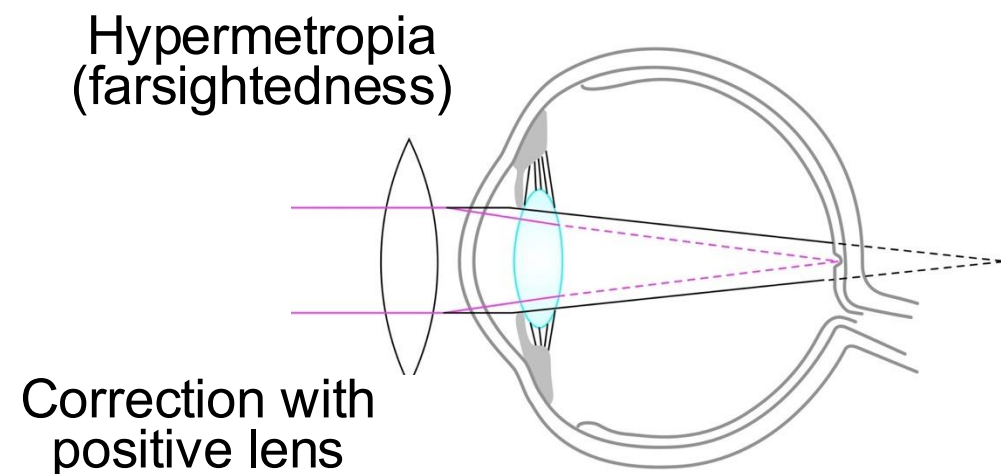
N.B.: 1)  $n - n'$  is greatest at the air-cornea surface.  
 2) There are two possible mechanisms for controlling refractive power (variation of  $n'$  or  $r$ )!

# Accommodation

- Adaptation of the eye's refractive power to the object distance.
- Mechanism: radius of curvature of the lens is modified.
- Accommodation power: difference, in diopter, between the far and near points of the eye.

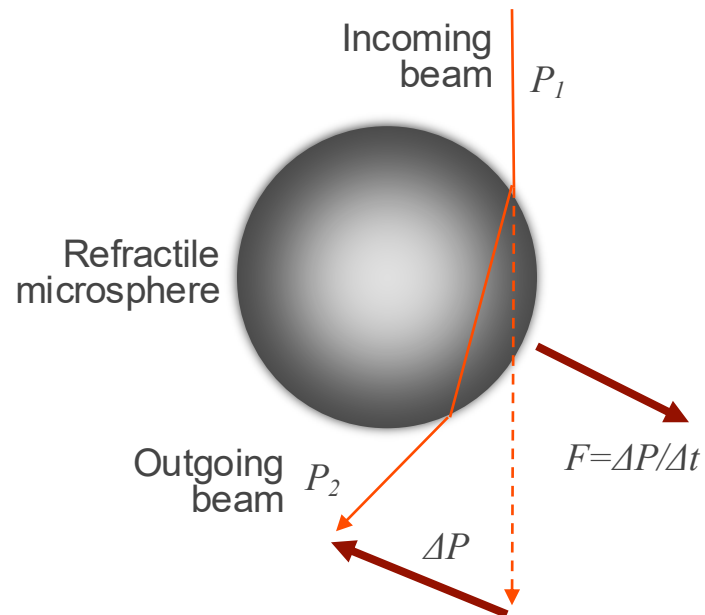


# Refraction problems

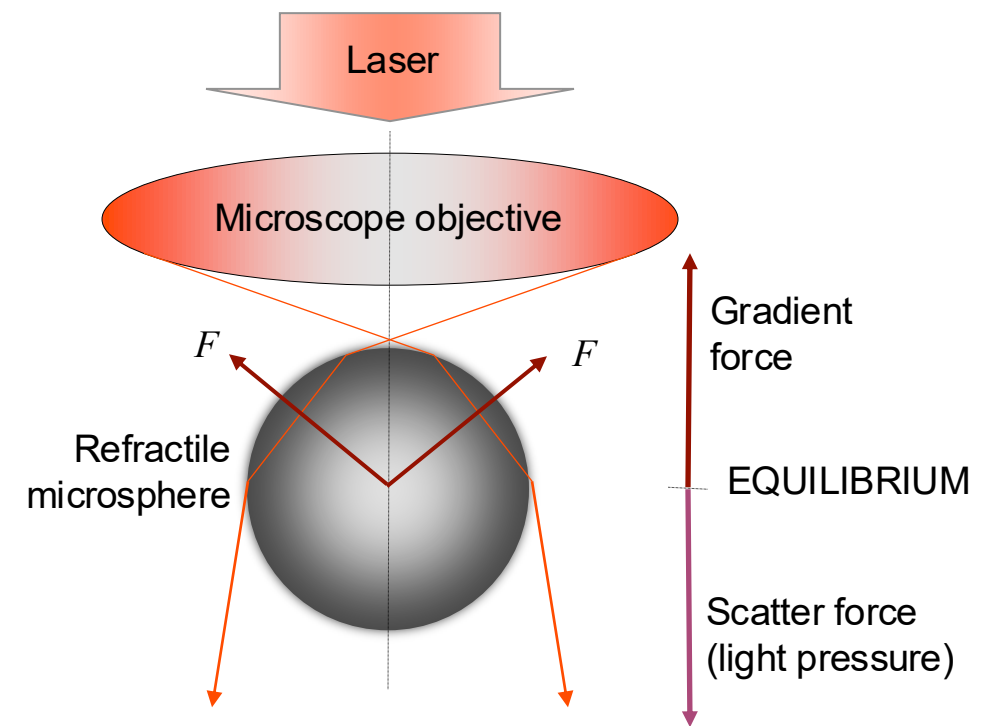


# Manipulating objects with refraction

Refraction is accompanied by photonic momentum change ( $\Delta P$ )  
(Theory later):

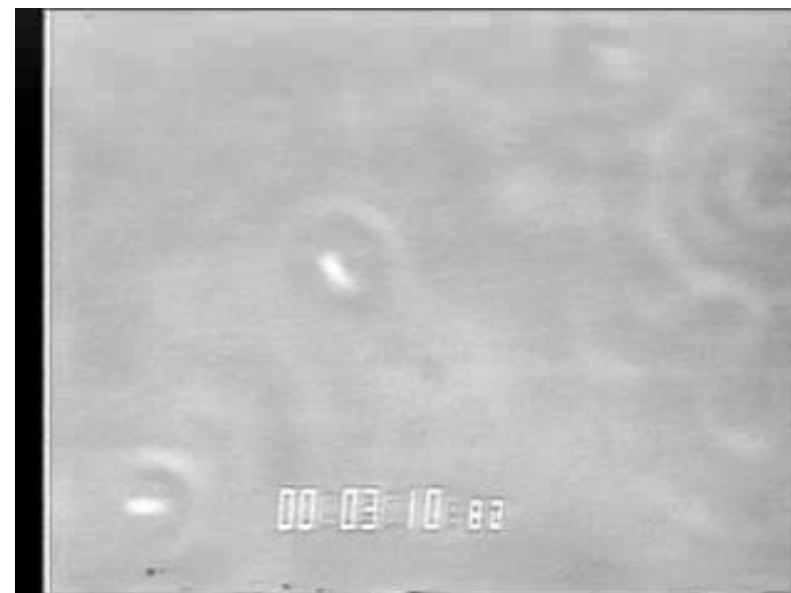
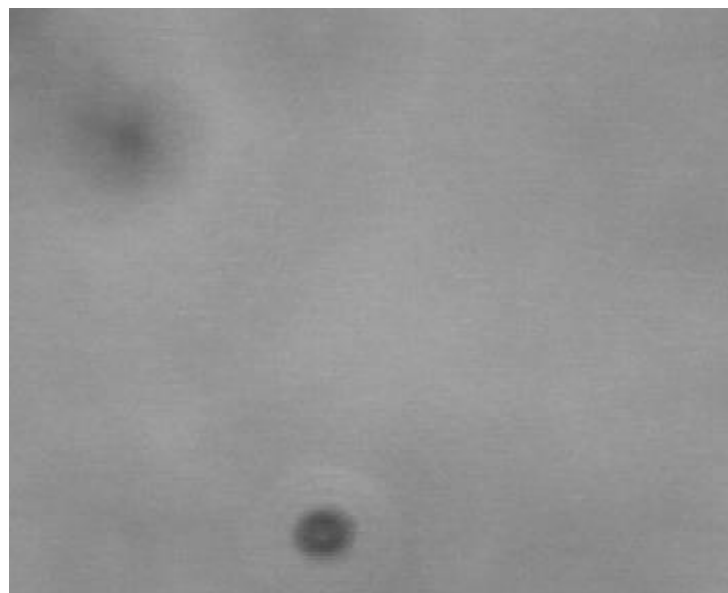


Refractile particles may be **captured** with photonic forces:



In the **optical trap** a momentum change occurs between the photons and the trapped particle:

3  $\mu\text{m}$  latex (polystyrene) microspheres in the optical trap



Optical trapping of bacterial (E.coli) cells

# Feedback:



<https://feedback.semmelweis.hu/feedback/index.php?feedback-qr=Z8JYKZ10V0N3CT7S>