

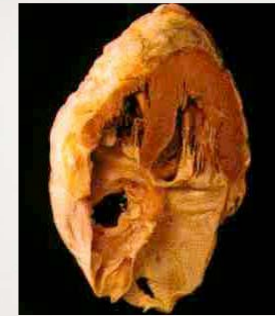
FLUID FLOW AND CIRCULATORY SYSTEM

MIKLÓS KELLERMAYER

Importance of the physics of fluids

I. Hemodynamics

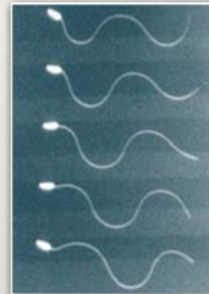
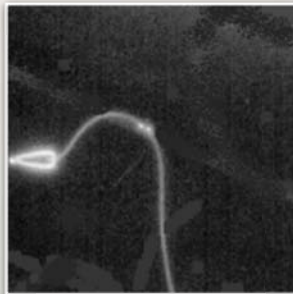
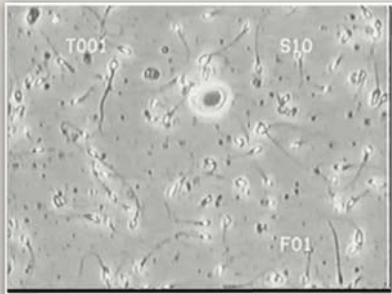
Characteristics of blood flow along the circulatory system.



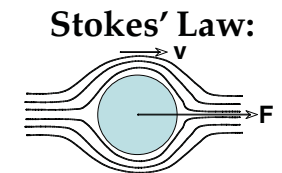
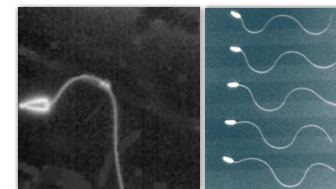
Significance of the physics of fluids

II. Motion in fluids

Force exerted by a single spermatozoa during its motion.



Drag coefficient of the spermatozoa



$$\gamma = 6r\pi\eta = 6 \cdot 1.6 \times 10^{-6} (m) \cdot \pi \cdot 10^{-3} (Pas) = 3 \times 10^{-8} Ns/m$$

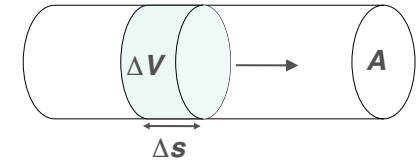
$$F = \gamma v = 3 \times 10^{-8} Ns/m \cdot 5 \times 10^{-5} m/s = 1.5 \times 10^{-12} N = 1.5 pN$$

Biophysics of fluids

- Basic principles
- Types of fluids
- Types of fluid flow
- Laws of fluid flow
- Biomedical importance

Basic principles I.

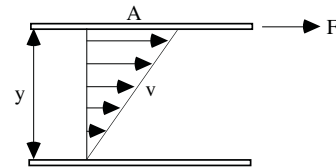
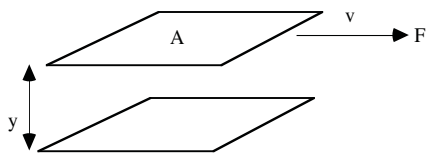
Volumetric flow rate (Q):



$$Q = \frac{\Delta V}{\Delta t} = A \frac{\Delta s}{\Delta t} = A \bar{v}$$

Average velocity: $\bar{v} = \frac{Q}{A}$

Basic principles II. Viscosity (internal friction)



F = shear force
A = area of fluid layer
 η = viscosity
v = flow velocity
y = distance between fluid layers

$$\frac{F}{A} = \eta \frac{\Delta v}{\Delta y}$$

$$\eta = \frac{\tau}{D}$$

F/A = shear stress (τ)
 $\Delta v / \Delta y$ = velocity gradient (D)

Units of viscosity: $1 \text{ Pas} = 1 \frac{\text{Ns}}{\text{m}^2} = 10 \text{ P (poise)}$

Types of fluids I.

1. Ideal

frictionless, incompressible
 $Q = \text{constant}$, $\eta = 0$

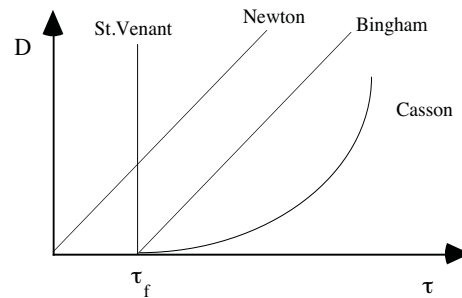
2. Non-ideal (real)

a. *Newtonian (viscous)*
 η independent of shear stress

b. *Non-newtonian (anomalous)*
 η varies with shear stress

Types of fluids II.

Relationship between velocity gradient and shear stress in real fluids



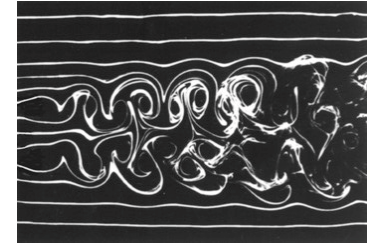
τ_f =flow threshold

Viscoelastic materials: combination of elastic and viscous properties (e.g., polymer solutions)
Stress-relaxation: decay of shear stress in viscoelastic material following sudden stretch.

NB: Blood is non-newtonian fluid!

Types of fluid flow

- 1. Stationary**
Flow intensity stays constant.
- 2. Laminar**
Fluid layers do not mix.
- 3. Turbulent**
Fluid layers mix.



Reynolds number: $R = \frac{vr\rho}{\eta}$

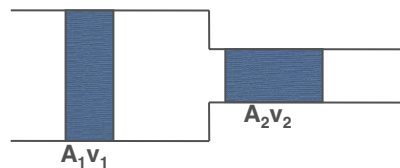
v =flow rate (m/s)
 r =tube radius (m)
 ρ =density of fluid (kg/m³)
 η =viscosity (Ns/m²)

laminar turbulent

100 1000 R

Laws of flow in ideal fluids I.

Continuity equation



$$A_1v_1 = A_2v_2 = \text{konst}$$

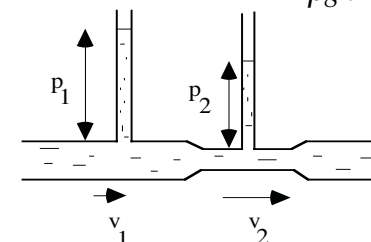
A =cross-sectional area
 v =flow rate

Laws of flow in ideal fluids II.

Bernoulli's law

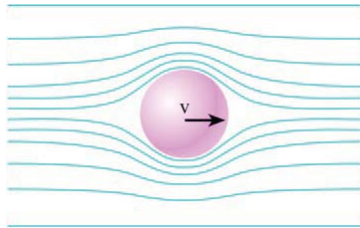
$$p + \frac{1}{2}\rho v^2 + \rho gh = \text{konst}$$

p =static pressure
 $\frac{1}{2}\rho v^2$ = dynamic pressure
 ρgh = hydrostatic pressure



Laws of flow in viscous fluids I.

Stokes' law



$$F = \gamma = 6r\pi\eta v$$

F = force

γ = drag coefficient (shape factor)

v = flow rate

r = radius of sphere

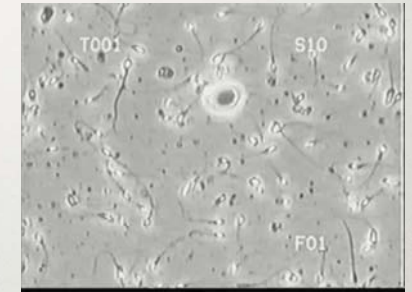
η = viscosity

Stokes Force

Hydrodynamic drag force (Stokes force): $F = \gamma = 6r\pi\eta v$



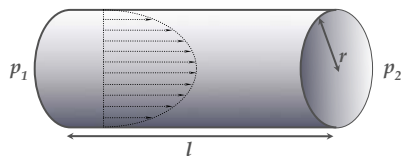
Affects stationary particles
in moving fluid



Affects moving particles in
stationary fluids

Laws of flow in viscous fluids II.

Hagen-Poiseuille's law



$$\frac{V}{t} = \frac{\pi r^4}{8\eta} \frac{dp}{dl}$$

V=volume

t=time

(V/t=Q = flow intensity)

r=tube radius

η =viscosity

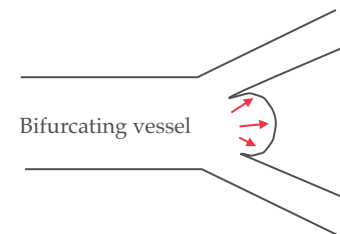
p=pressure

l=length of tube

(dp/dl=pressure gradient, maintained by p_1-p_2)

Biomedical significance

Bernoulli's law:



aneurysm:

- ➡ flow rate decreases (according to continuity equation)
- ➡ pressure increases
- ➡ aneurysm increases

Hagen-Poiseuille's law:

$$\frac{V}{t} = \frac{\pi r^4}{8\eta} \frac{dp}{dl}$$

Flow intensity may be **drastically reduced** in certain pathological conditions:

-constriction of blood vessels
(e.g., diabetes, Bürger's disease)

-change in blood viscosity
(e.g., fever, anaemia)

BIOPHYSICS OF BLOOD FLOW

1. Blood as fluid
2. Determinants of blood viscosity
3. The vascular system
4. Blood vessels as elastic tubes
5. Auxiliary forces of circulation

BLOOD AS FLUID

55-60% of body mass is water
42 kg (70 kg body mass)

2/3 intracellular 28 kg	1/3 extracellular 14 kg
	1/3 plasma 4-5 kg
	2/3 interstitium 9-10 kg

Blood

Average volume: 5 l
Average viscosity: 5 mPas
Average density: 1.05 g/cm³
Composition: 40-45 % corpuscular, 55-60 % plasma

Determinants of blood viscosity I.

1. Hematocrit (htc , ϕ):

$$htc = \frac{V_{cells}}{V_{total}}$$

Normal range: 0.4-0.5.

Viscosity of blood as suspension
(in the physiologically relevant htc range):

$$\lg \eta_s = A + B\phi$$

η_s =suspension viscosity
A, B=empirical constants

Determinants of blood viscosity II.

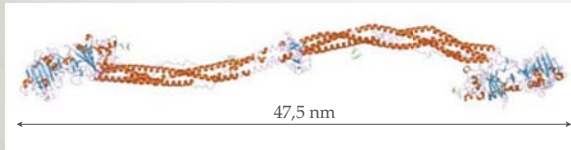
2. Plasma viscosity

Depends on plasma proteins.

In paraproteinaemias (e.g. myeloma multiplex or plasmocytoma) the concentration of immunoglobulins is high, leading to increased viscosity.

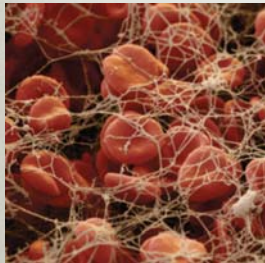
Plasma protein	Normal concentration	% ratio	Function
Albumin	35-50 g/l	55%	maintenance of colloind osmotic pressure, transport
Globulins	20-25 g/l	38%	Part of the immune system
Fibrinogen	2-4.5 g/l	7%	Blood coagulation

Fibrinogen, fibrin

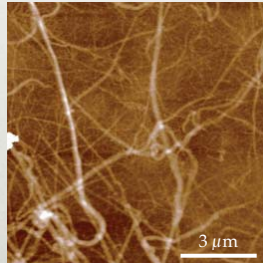


Fibrinogen:

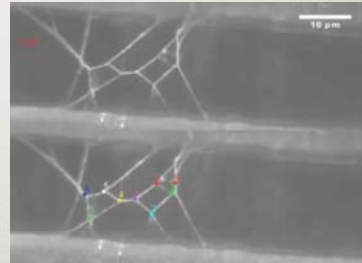
MW = 340.000 Da
In plasma: 2-4 g/l \approx 10 μ M
Average nearest-neighbor distance \approx 55 nm



Red blood cells in fibrin meshwork



Fibrin polymerized in vitro (AFM)



Extensibility of fibrin fibrils

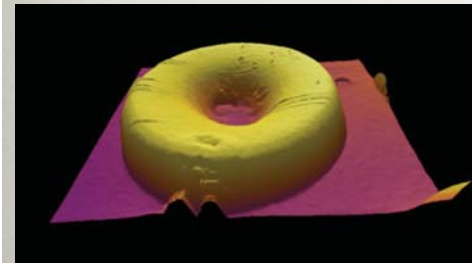
Determinants of blood viscosity III.

3. Plasticity of red blood cells

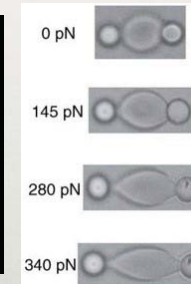
65% suspension of blood-cell-size particles is rock hard.

By contrast, a 95% blood suspension is fluid, with viscosity of \sim 20 mPas!

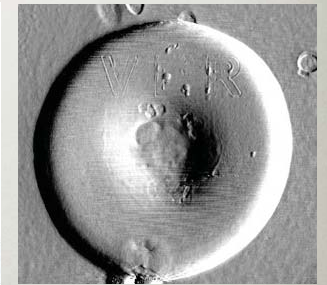
Deformation of red blood cells: droplet, parachute, arrowhead shapes.



Disc-shaped cell with 7-11 μ m diameter



Deformation of a RBC with optical tweezers



Fixed RBC maintaining impression (AFM)

Determinants of blood viscosity III.

4. Aggregation of red blood cells

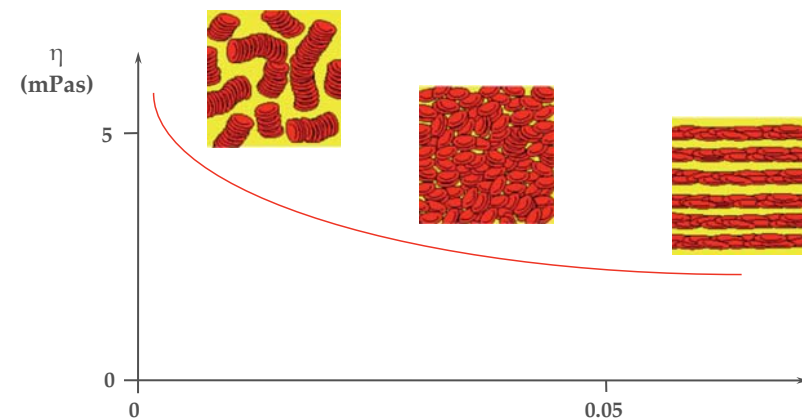
Stack or rouleaux formation.

More pronounced at low flow rates.



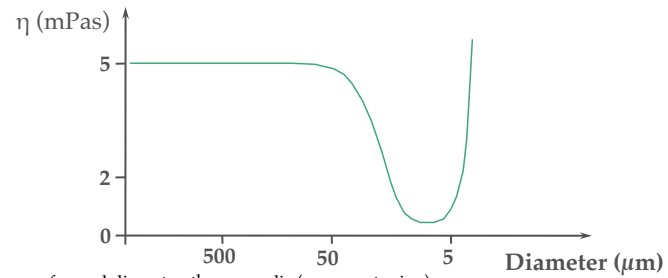
Determinants of blood viscosity IV.

5. Flow rate, velocity gradient



Determinants of blood viscosity V.

6. Blood vessel diameter



N.B.:

-With a decrease of vessel diameter, the anomalic (non-newtonian) behavior of blood becomes more pronounced.

-*Axial migration:*

the red blood cells line up in the axis of the vessel.

In the axis the velocity gradient decreases,

and near the vessel wall it increases.

Increase in velocity gradient decreases apparent viscosity (Fåhræus-Lindqvist effect).