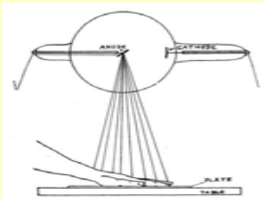
X-ray

production and properties

Glass tube with two electrodes in vacuum
or in low pressure gas

Experiments and observations of Wilhelm Conrad Roentgen

- cathode ray generates radiation in the wall of the tube
- the radiation induces fluorescence in barium platinocyanide
- it has much higher penetration than UV



This unknown radiation has high penetration distance

Roentgen's X-ray picture of the hand of his wife, taken December 22, 1895.

Age of Wilhelm Conrad Roentgen

1895 – the year

Roentgen discovers X-ray

On November 27, 1895, in Paris, Alfred Bernhard Nobel signed his will.

The cinématographe (Auguste and Louis Lumière) was patented on 13 February 1895

U.S. patent for an automobile by George B. Selden

Jungle Book was written by Rudyard Kipling

Discoveries of „Golden Years" in physics

1896: Becquerel – radioactivity

1897: Thomson – electront

1898: Pierre és Marie Curie – polonium and radium

X-ray

Discovery – November 1895

Publication – December 1895

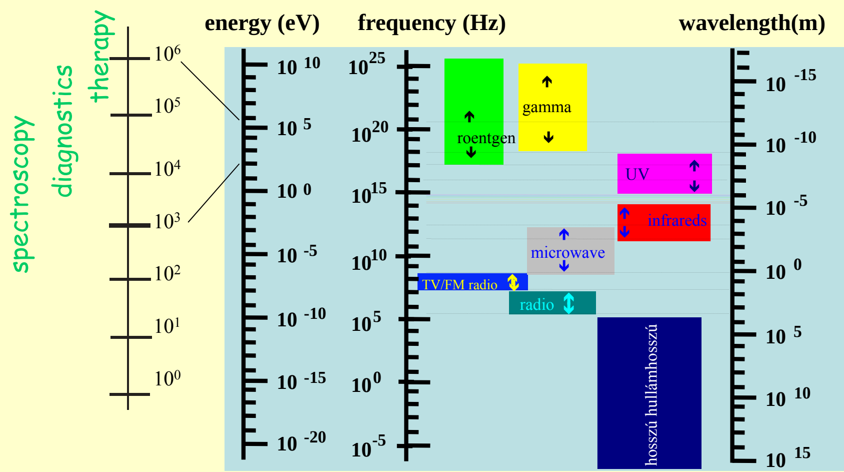
Medical application – January1896

Wilhelm Conrad Roentgen

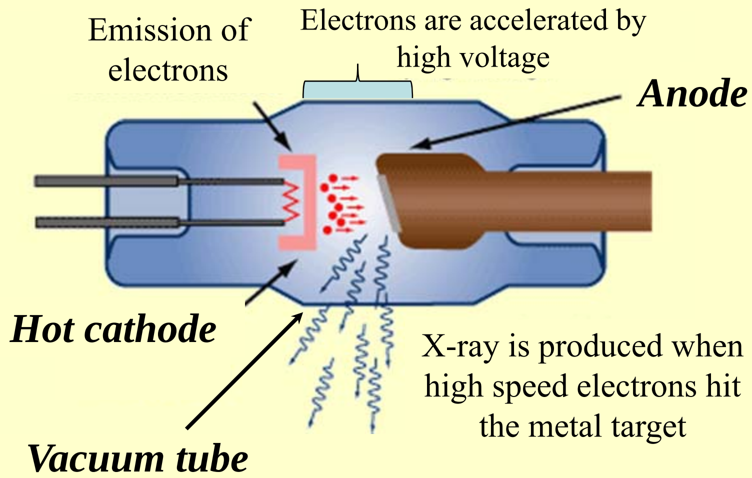
Nobel Prize in Physics 1901
in recognition the discovery of the remarkable rays subsequently named after him

X-ray

Elektromagnetic radiation

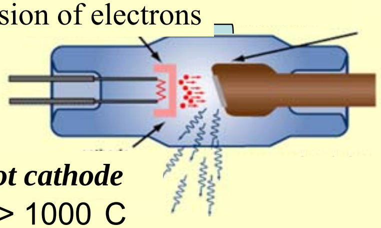


X-ray tube



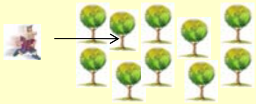
Steps of producing X-ray

Emission of electrons



Hot cathode
T > 1000 C

vacuum ~ 10^{-4} Pa
free pass length ~ 10 cm



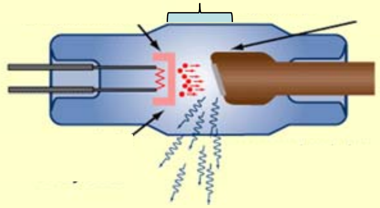
In the air, under atmospheric pressure
free pass length ~ 70 nm

Current density ~ T^2

$$I_{anod} = \frac{Q}{t} = \frac{n*e}{t}$$

$$P_{electric} = UI$$

Steps of producing X-ray



Acceleration of electrons

Pl. U = 60 kV
$m_e = 9{,}1.10^{-31}$ kg
$e = 1{,}6.10^{-19}$ C

$$eU = \frac{1}{2} m_e v^2$$

$$v = \sqrt{\frac{2eU}{m_e}} = 1.5*10^8 [\frac{m}{s}]$$

Work of electric field

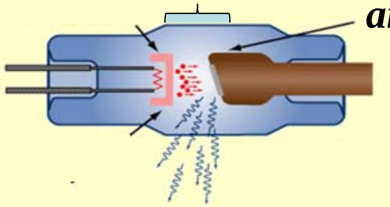
$$W = \Sigma F \Delta s = Q \Sigma E \Delta s$$

$$W = QU$$

$$\downarrow$$

$$W = \frac{1}{2} m_e v^2$$

Steps of producing X-ray



anode

Anode ***material***: - high atomic number (e.g. ^{29}Cu, ^{42}Mo, ^{74}W
- high melting poin

Anode ***position***: - standing – lower possible power (few W/ mm^2)
It is enough in dentisry
- rotating – heat distribution is better, higher possible power (10000 W/ mm2)

Steps of X-ray production

Generation of charged particles

e$^-$, *H^+, light ions*

Acceleration

X-ray tube, accelerators

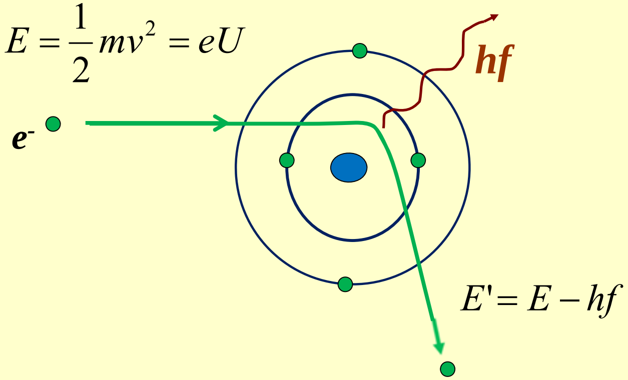
Deceleration

^{29}Cu, ^{42}Mo, ^{74}W, ^{78}Pt

Mechanism of X-ray production

1. Bremsstrahlung or "braking radiation "

$$E = \frac{1}{2}mv^2 = eU$$



The electron is deflected from its original path and decelerated.

The electron's kinetic energy is reduced

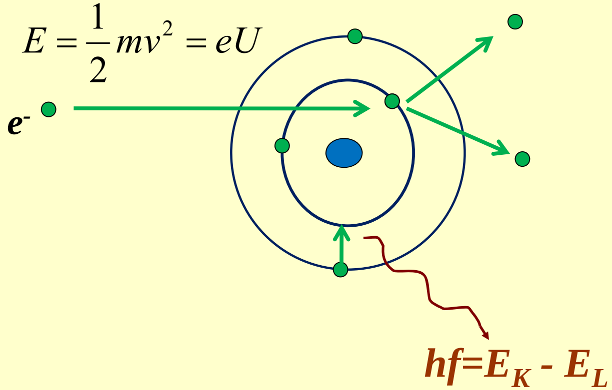
The energy lost by the electron takes the form of a Bremsstrahlung photon.

The photon energy depends on
- the kinetic energy of incoming electron
- distance of closest approach to the nucleus
- atomic number of target material

Highest photon energy is equal to the kinetic energy of incoming electron.

2. Characteristic radiation

$$E = \frac{1}{2}mv^2 = eU$$

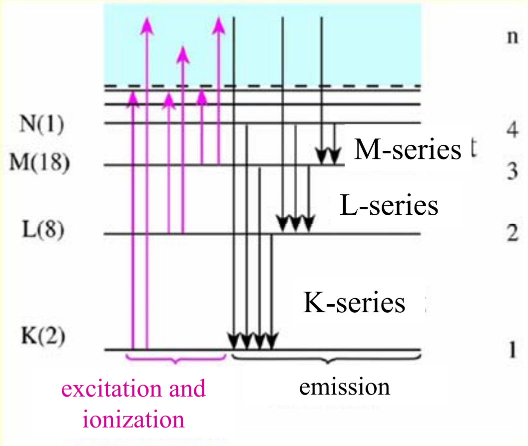


If the incident electron energy is high enough, it may interact with an (inner) orbital electron, ejecting it from its orbit (excitation/ionization).

The vacancy is occupied by an electron from a higher orbits

The discrete excess energy is emitted as a characteristic photon

Possible energy transitions of the Cu-atom with 29 electrons

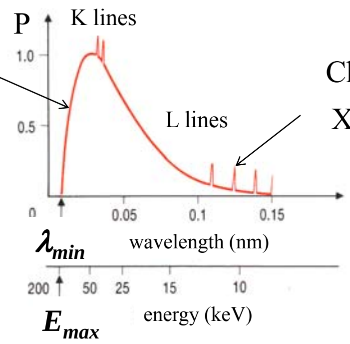


Photon energies veries with the energy differences between neighbouring elecronic states.

Spectral properties of X-ray

Continuous
Bremsstrahlung spectrum

Line
Characteristic
X Radiation



$$E_{\max} = \frac{1}{2}mv^2 = eU$$

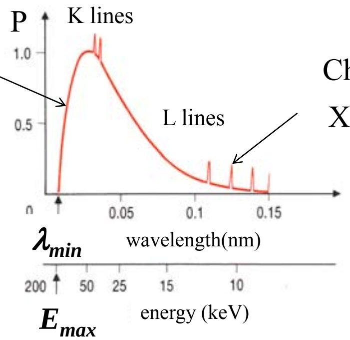
$$eU = h\frac{c}{\lambda_{\min}}$$

$$\lambda_{\min} = \frac{hc}{eU}$$

Spectral properties of X-ray

Continuous
Bremsstrahlung spectrum

Line
Characteristic
X Radiation



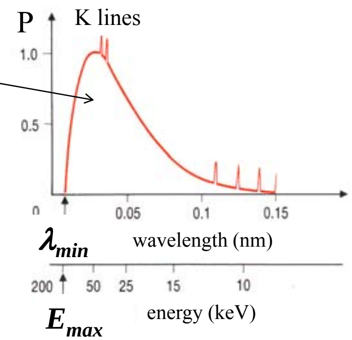
$$\lambda_{\min} = \frac{hc}{eU}$$

Duanne-Hunt law

Power and efficiency of X-ray tube

$$P = cIU^2Z$$

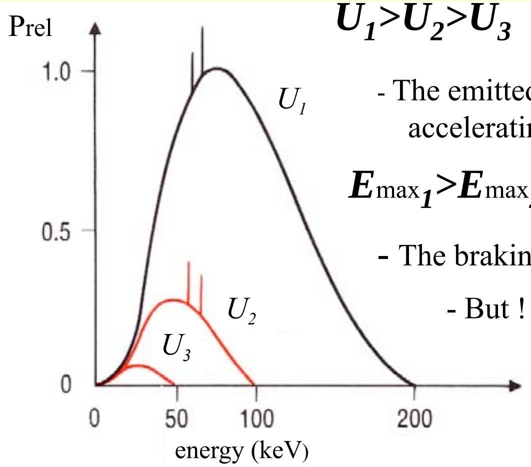
$c=1{,}1\times10^{-9}$ [1/V]



$$\eta = \frac{P}{P'} = cUZ$$

$\eta < 1\%$

Decrease of accelerating voltage :



$U_1 > U_2 > U_3 \qquad P_1 > P_2 > P_3$

- The emitted power decreases with the accelerating voltage.

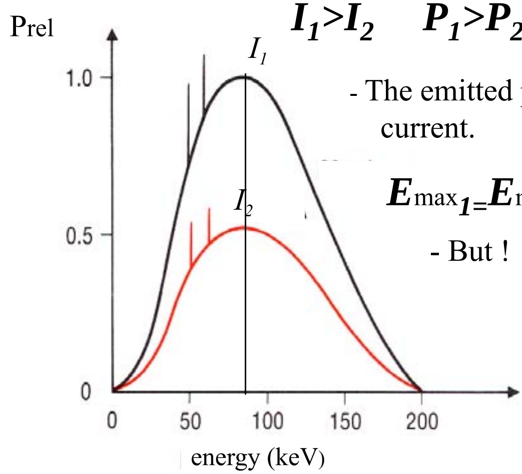
$E_{max_1} > E_{max_2} > E_{max_3}$

- The braking radiation becomes softer.

- But !

The position of characteristic lines remains the same.

Decrease of current:



$I_1 > I_2 \qquad P_1 > P_2$

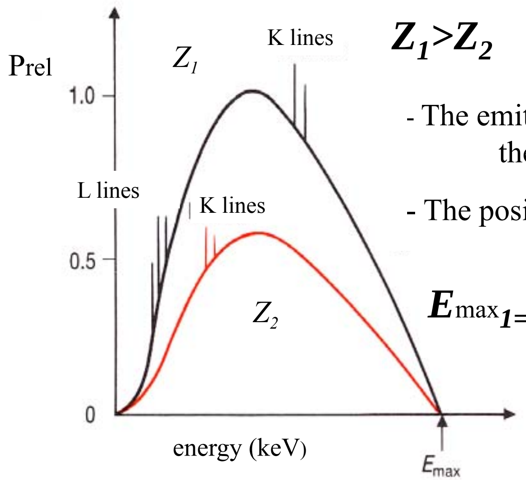
- The emitted power decreases with the current.

$E_{max_1} = E_{max_2}$

- But !

Spectral distribution and the position of characteristic lines remains the same.

Effect of target (anode) material



$Z_1 > Z_2 \qquad P_1 > P_2$

- The emitted power decreases with the atomic number of target.

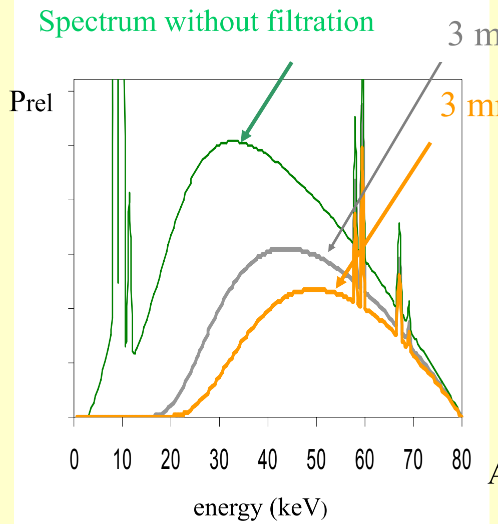
- The position of characteristic lines is altered.

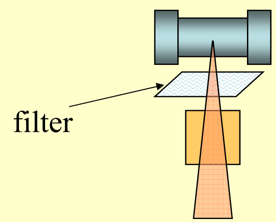
$E_{max_1} = E_{max_2}$

- But !

Spectral distribution of breaking radiation remains the same.

Application of radiation filters





Preferential absorption of lower photon energies

Average photon energy increases

No change in E_{max}

Application of radiation filters

Modification oft he properties (spectrum, special distribution) of radiation

Inherent filter elements.

e.g., anode material, wall of the tube, diaphragm etc.

External filters, typically Al or Cu plates.

Disadvantage: reduces the intensity
increases the exposition time

Advantage: reduces – approximately 80% – the exposure of the patient

Typical conditions for diagnostic X-ray production

Accelerating voltage: 25 – 200 kV

Current: 1 – 1000 mA

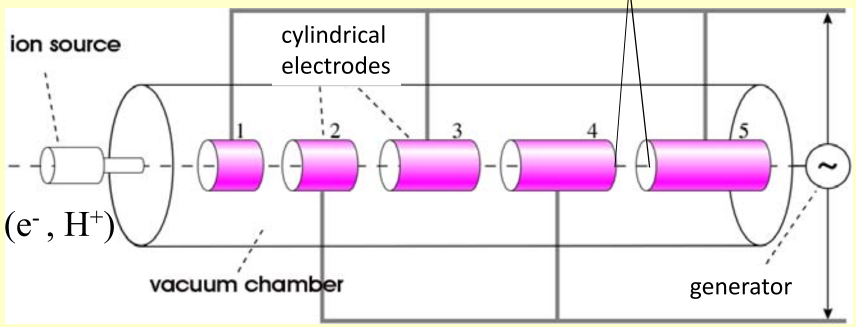
Anode material: W, in mammography Mo

Special conditions

Particle accelerators

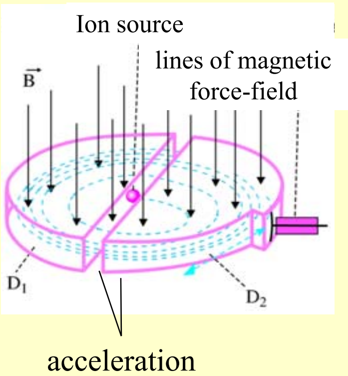
Linear Accelerator

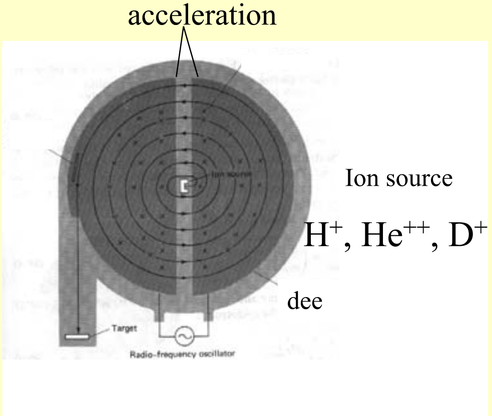
The particles are accelerated when passing through the gaps.



Linear accelerator (LINAC) is used in **Radiotherapy**

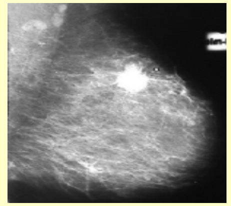
Cyklotron – acceleration on a circular path





Magnetic field (Lorenz-force) → circular path
Electric field → acceleration; increased radius of circle

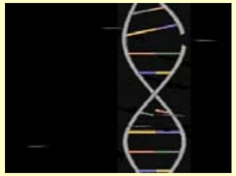
Medical applications of X-rays



X-ray diagnostics

Radiotherapy

Fertilization



Interaction of X-ray with matter

Law of radiation attenuation $$J = J_0 e^{-\mu x}$$

μ (linear attenuation (absorption) coefficient) depends on
photon energy
quality (atomic number) of absorber
density of absorber

$$\mu_m = \frac{\mu}{\rho}$$

BUT! Ratio of μ and the density is constant

μ_m [cm²/g] : mass attenuation coefficient

Varies with – the photon energy
– atomic number of absorber

Law of radiation attenuation

$$J = J_0 e^{-\mu_m x_m}$$

x_m [g/cm²] : surface density $\quad x_m = \rho x$

$$\mu = \frac{0.693}{D}$$

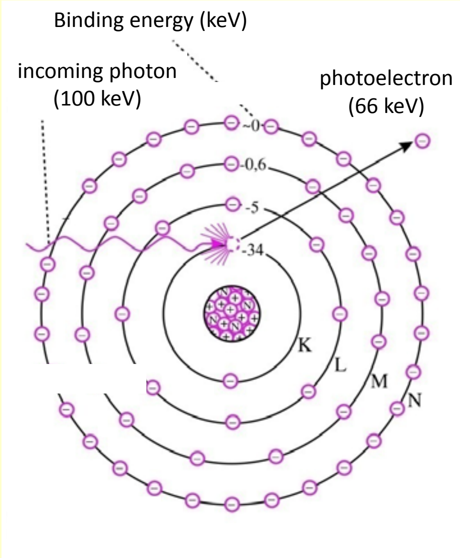
and

$$D_m = \rho D$$

$$\mu_m = \frac{0.693}{D_m}$$

Mechanism of interaction (1)

Photoeffect

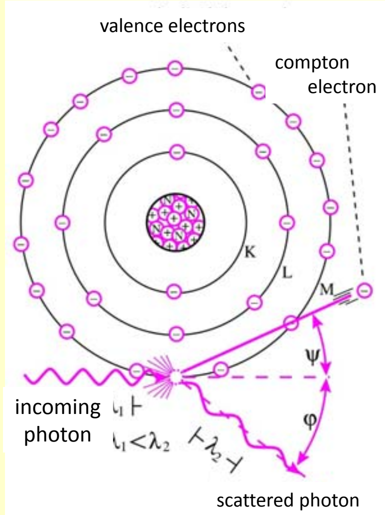


energy ballance:

$$hf = E_{binding} + \frac{1}{2} m_e v^2$$

Mechanism of interaction (2)

Compton scatter

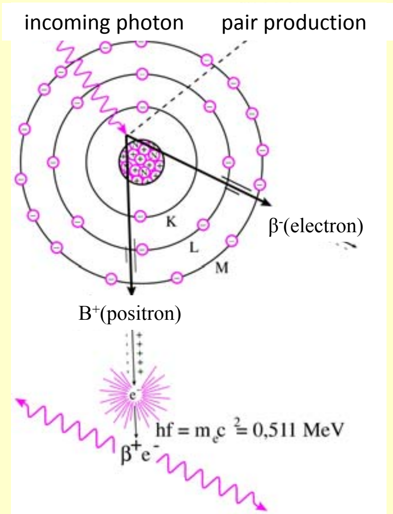


energy ballance:

$$hf = E_{binding} + \frac{1}{2} m_e v^2 + hf'_{scattered}$$

Mechanism of interaction (3)

Pair production



energy ballance:

$$hf = 2m_e c^2 + 2\frac{1}{2} m_e v^2$$

$$hf \geq 2m_e c^2$$

$$\boxed{hf \geq 1.02 MeV}$$

Probability of interaction (absolute and relative) depends on

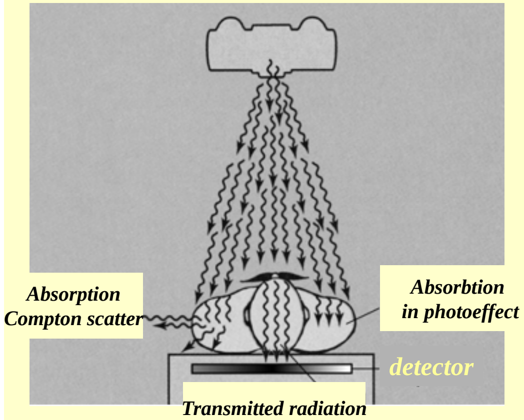
- the photon energy
- atomic number of absorber

$$\mu = \tau + \sigma + \kappa$$

photoeffect (τ), Compton scatter (σ), Pair production (κ)

$$\mu_m = \tau_m + \sigma_m + \kappa_m$$

Basic principle of X-ray diagnostic is the absorption of radiation



Possible interactions:

Compton scatter

photoeffect

no interaction

Damjanovich, Fidy, Szöllősi: Medical Biophysics

II. 3.1
- 3.1.1
- 3.1.2
- 3.1.3
- 3.1.4
- 3.1.5
- 3.1.6