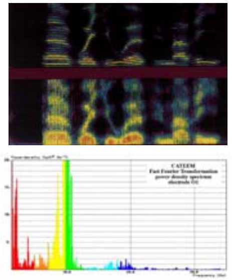
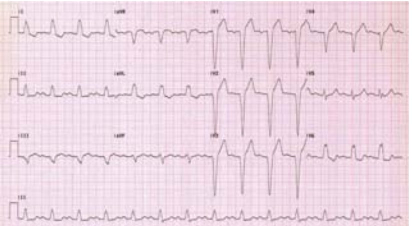
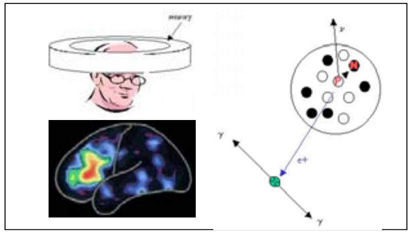


Medical signal processing





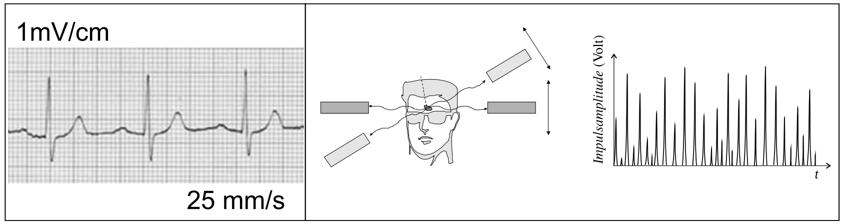
KAD 2014.02.06

A **signal** is any kind of physical quantity that conveys/ transmits/stores information

e.g. (1)
electrical voltage, that can be measured on the surface of the skin/head as a result of the heart-/muscle-/brain activities (ECG/EMG/EEG)

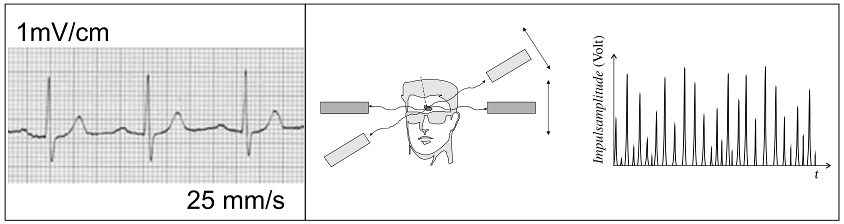
e.g. (2)
gamma photon detection in radioisotope diagnostics

(1) (2)



Classification of signals

static	–	time-dependent
periodic	–	non-periodic
random	–	deterministic
pulsed	–	continuous
electric	–	non-electric
analog	–	digital



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in a very special role

electric signals

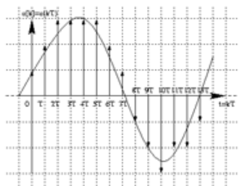
non-electric signals are transferred to electric ones

advantages of **electric** signals: they are easy to transform, amplify, transmit

digital signals

analog signals are transferred to digital ones

advantages of **digital** signals: they are easy to store, the noise can be engineered and influence can be reduced



quantity that compares the magnitudes of two signals:

Signal level or **Bel**-number (or **Decibel**-number): n

(named after A. Bell)

unit of n : Bel (B) or decibel (dB)

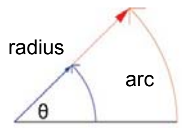
$$n = \lg\frac{P_2}{P_1}\,\mathrm{B} = \lg\frac{J_2}{J_1}\,\mathrm{B} = \lg\frac{E_2}{E_1}\,\mathrm{B}$$

decimal logarithm of ratio of two powers (intensities, energies)

cf. **radian**

$$\Theta = \frac{\text{arc}}{\text{radius}}$$

$$[\Theta] = \frac{\mathrm{m}}{\mathrm{m}} = \mathrm{rad} = 1$$



cf. **pH** (power of Hydrogen)

$$\mathrm{pH} = -\lg\frac{[\mathrm{H}^+]}{1\mathrm{M}}$$

$$e.g.: \; [\mathrm{H}^+] = 10^{-7}\mathrm{M}$$

$$\Rightarrow \mathrm{pH} = -\lg 10^{-7} = -1\cdot(-7) = 7$$

---

instead of Bel number we are using **decibel-number**

$$\boxed{n = 10\cdot\lg\frac{P_2}{P_1}\,\mathrm{dB}} \qquad (10\mathrm{d} = 1)$$

the **characteristic** unit: **power** (or intensity/energy),
the **practical** unit: (electric) **voltage**

the relation between power and voltage:

$$P = U\cdot I = \frac{U^2}{R} \quad (\mathrm{Ohm}: \; U = R\cdot I)$$

signal level with voltages:

$$n = 10\cdot\lg\frac{P_2}{P_1}\,\mathrm{dB} = 10\cdot\lg\frac{\frac{U_2^{\,2}}{R_2}}{\frac{U_1^{\,2}}{R_1}}\,\mathrm{dB} \overset{R_2 \approx R_1}{=}$$

$$= 10\cdot\lg\frac{U_2^{\,2}}{U_1^{\,2}}\,\mathrm{dB} = \boxed{20\cdot\lg\frac{U_2}{U_1}}\,\mathrm{dB}$$

$$\frac{P_2}{P_1} = 2 \Leftrightarrow 10\lg 2\,\mathrm{dB} =$$
$$= 10\cdot 0{,}3\,\mathrm{dB} = 3\mathrm{dB}$$

$$\frac{P_2}{P_1} = \frac{1}{2} \Leftrightarrow -3\mathrm{dB}$$

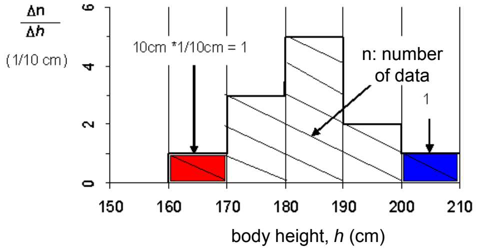
cf. half life,
half value thickness

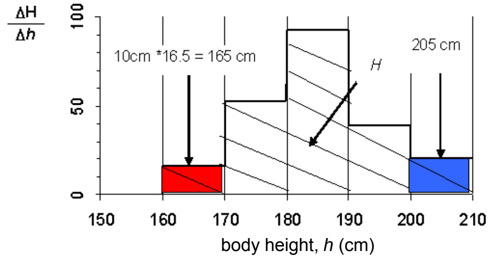
$$\frac{P_2}{P_1} = 10 \Leftrightarrow 10\cdot\lg 10\,\mathrm{dB} =$$
$$= 10\cdot 1\mathrm{dB} = 10\mathrm{dB}$$

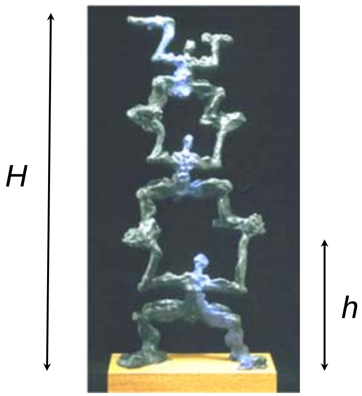
$$\frac{P_2}{P_1} = 100 \Leftrightarrow 10\lg 100\,\mathrm{dB} =$$
$$= 10\cdot 2\,\mathrm{dB} = 20\mathrm{dB}$$

U_2/U_1	P_2/P_1	dB
1,414	2	3
2	4	6
	8	9
3,16	10	10
	20	13
10	100	20
	$1000=10^3$	30
$100=10^2$	$10000=10^4$	40
$1000=10^3$	10^6	60

empirical density function

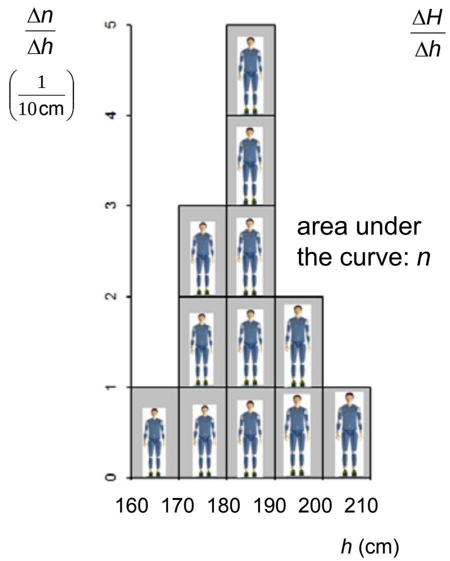


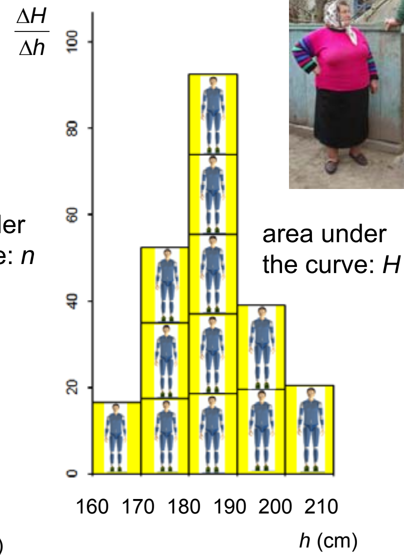




spectrum, as a special density function

Density function **Spectrum**





Fourier's theorem for periodic functions (signals)

all (usual) periodic functions can be expressed as a sum of sine (and cosine) functions from the fundamental frequency and the overtones

periodic function:
there is a period, T

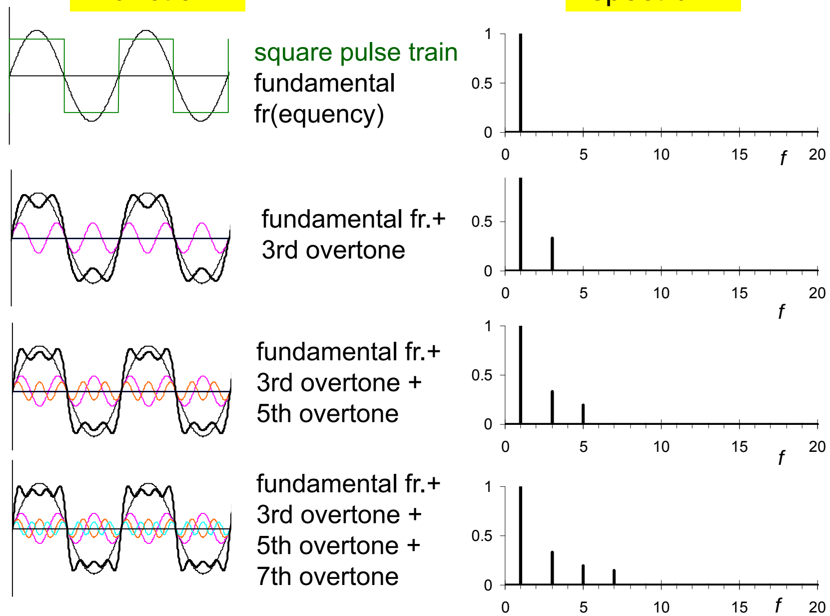
$\frac{1}{T} = f$, where f is the frequency

the sine function, which has the same frequency as the periodic function:
fundamental frequency

$2f$, $3f$, $4f$, ... : **overtones**

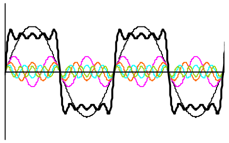
(line spectrum)

function spectrum

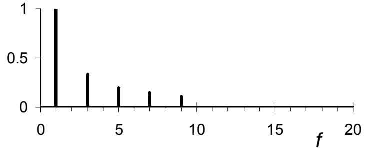


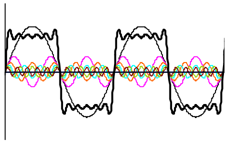
function

spectrum

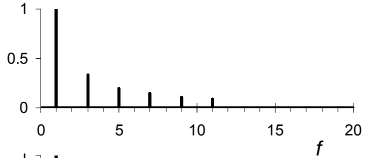


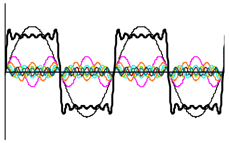
fundamental fr.+
3rd overtone +
+ ... +
9th overtone



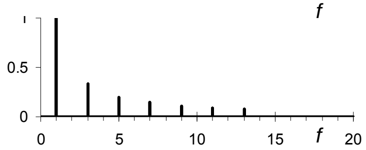


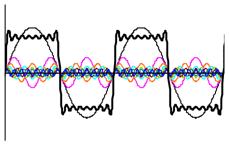
fundamental fr.+
3rd overtone +
+ ... +
11th overtone



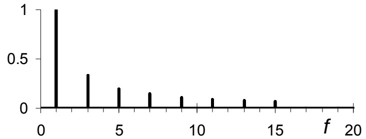


fundamental fr.+
3rd overtone +
+ ... +
13th overtone



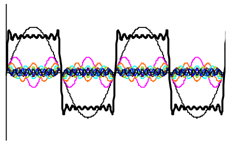


fundamental fr.+
3rd overtone +
+ ... +
15th overtone

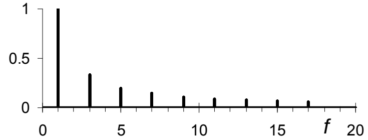


function

spectrum



fundamental fr.+
3rd overtone +
+ ... +
17th overtone



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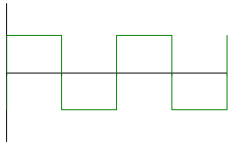
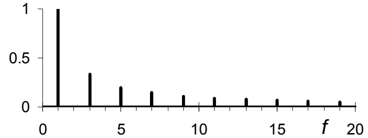
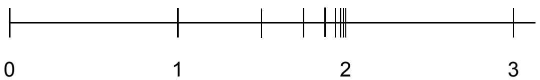


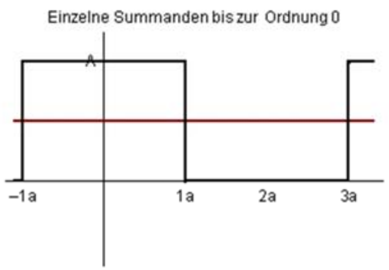
fundamental fr.+
3rd overtone +
+ ... +
17th overtone +
+ ...

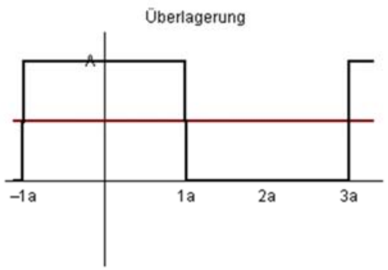


cf. infinite **series**

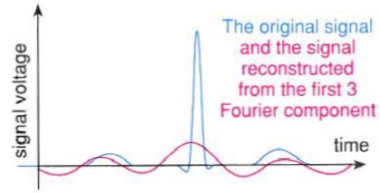
$$\sum_{k=0}^{\infty}\frac{1}{2^k}=\frac{1}{2^0}+\frac{1}{2^1}+\frac{1}{2^2}+\frac{1}{2^3}+\ldots=1+\frac{1}{2}+\frac{1}{4}+\frac{1}{8}+\ldots=2$$

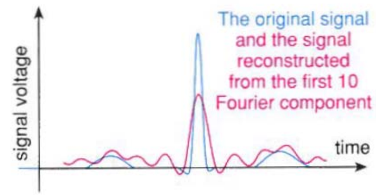


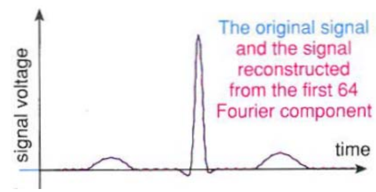




Creating an ECG signal from sine functions



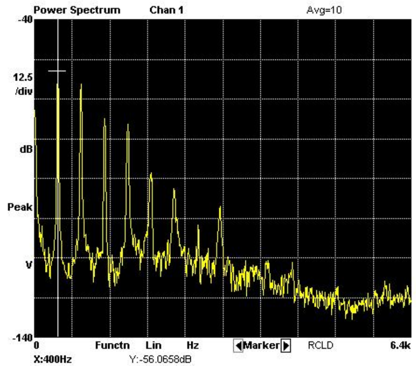




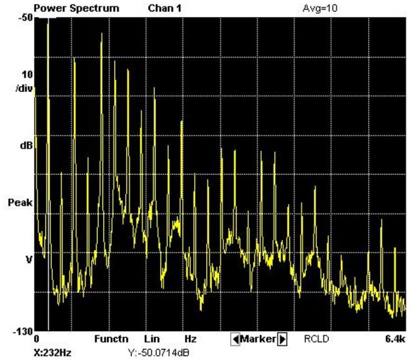
Textbook, Figure VII.3.

Measured spectra

flute



clarinet

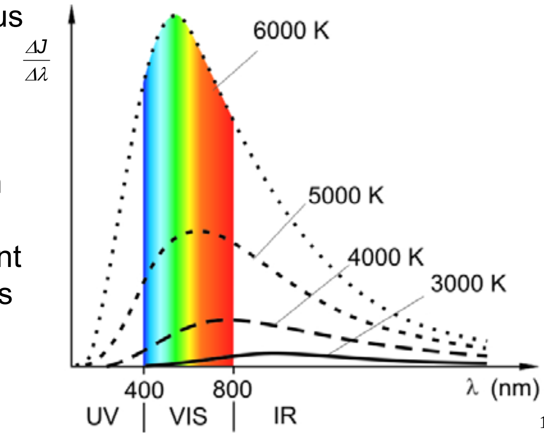


Fourier'theorem for non-periodic functions (signals)

all (usual) functions can be expressed as a sum of sine (and cosine) functions

spectrum: continuous

cf. emission spectra of incandescent light sources



function | spectrum

sine function — line spectrum (1 line)

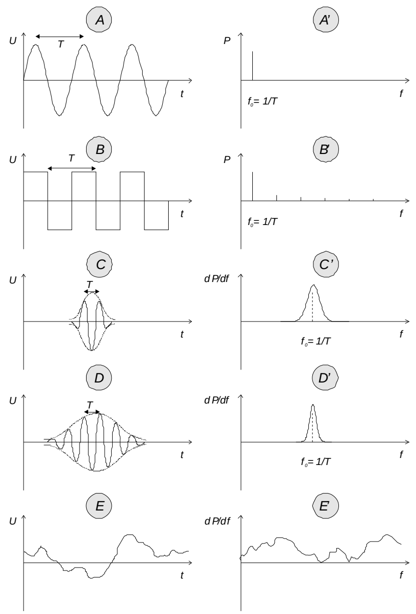
periodic function — line spectrum

a few periods — band spectrum

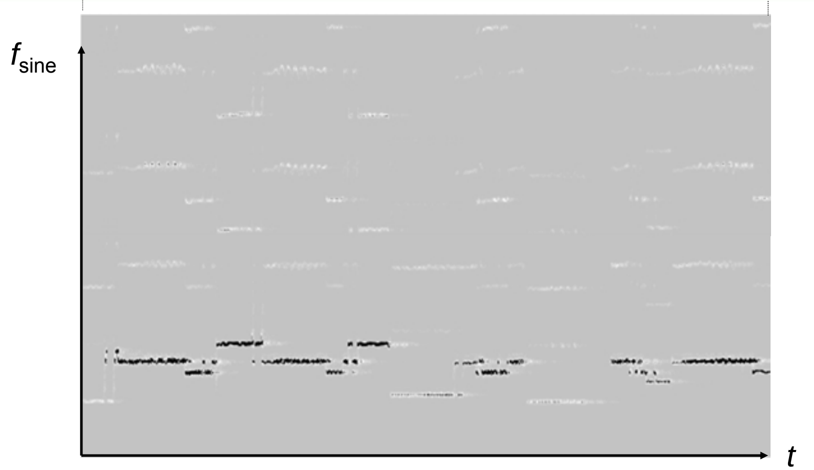
eg. pulsed ultrasound

more periods — band spectrum

non-periodic function — continuous spectrum



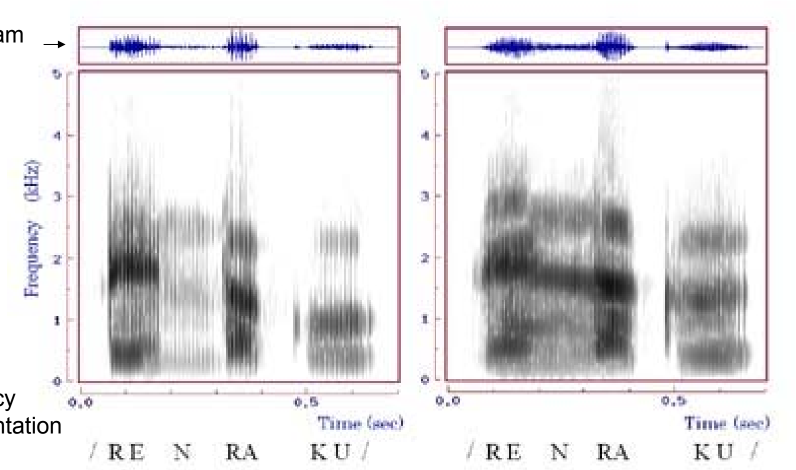
Music in time-frequency representation



Voiceprint

oscillogram (sound intensity vs. time)

time – frequency representation

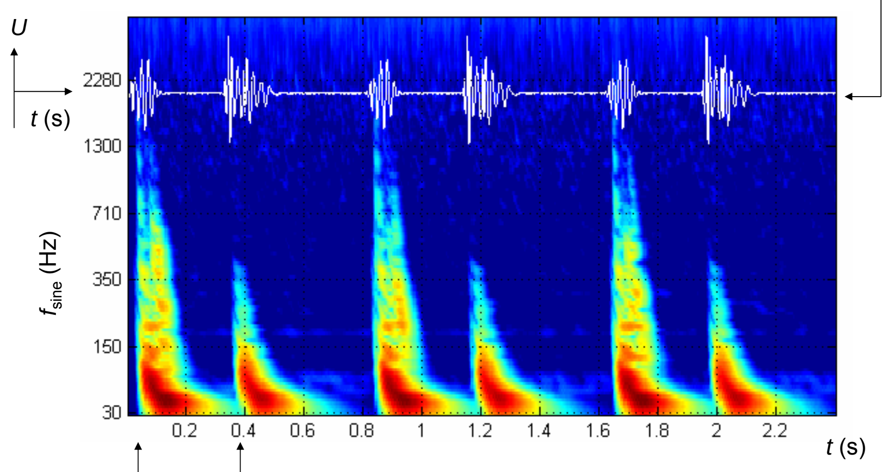


pronounced consonants and vowels

http://www.nrips.go.jp/org/fourth/info3/index-e.html

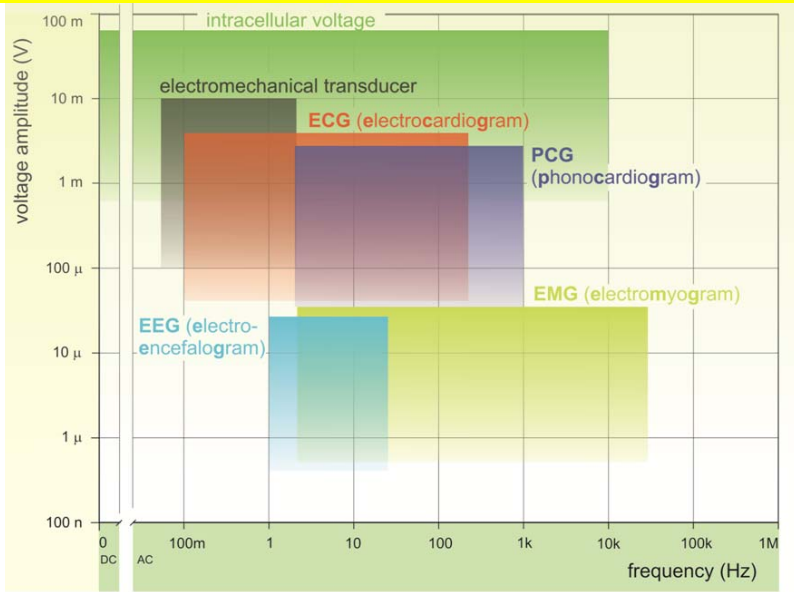
Heart beats in time-frequency representation

(+ oscillogram)



systole diastole

Frequency and amplitude ranges of biological signals



Practical manual, titel page of meas. 17

Frequency dependent unit: Electronic amplifier

(1) $P_{in} < P_{out}$

(2) P_{in} and P_{out} : same functions

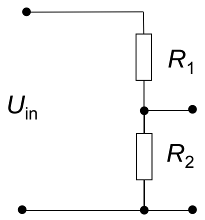
same: „fundamentalist“ requirement
similar: realistic requirement

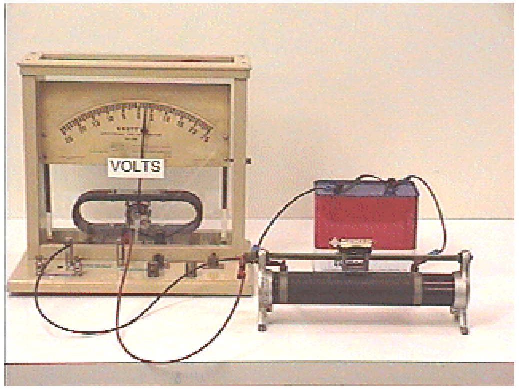
$$(1)+(2) \quad A_P \cdot P_{in}(t) \equiv P_{out}(t), \text{ where } A_P > 1$$

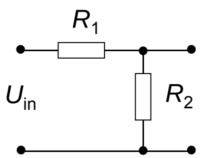
$\boxed{A_P = \dfrac{P_{out}}{P_{in}},}$ **power gain** (amplification)

$\boxed{A_U = \dfrac{U_{out}}{U_{in}},}$ **voltage gain** (amplification)

(frequency independent) voltage-divider







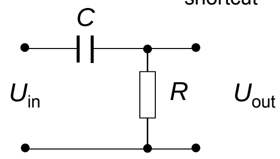
$$U_{out} = \frac{R_2}{R_1 + R_2} U_{in}$$

frequency dependent voltage-divider: with capacitor

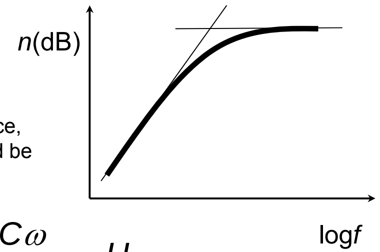
High-pass/low-cut **filter**

$R_C = \dfrac{1}{C\omega}$

at high frequencies the capacitor is a shortcut



because of the phase difference, the sum should be calculated as vectors



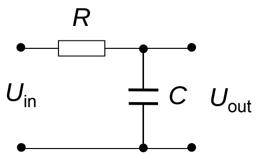
$$U_{out} = \frac{R}{\sqrt{\frac{1}{C^2\omega^2} + R^2}} U_{in} = \frac{RC\omega}{\sqrt{1 + R^2C^2\omega^2}} U_{in}$$

at very low frequencies: if $\omega << \omega_0$ $(\omega \approx 0), U_{out} = 0$

at low frequencies: if $\omega << \omega_0, U_{out} = RC\omega\, U_{in}$ ↔ 6 dB/octave

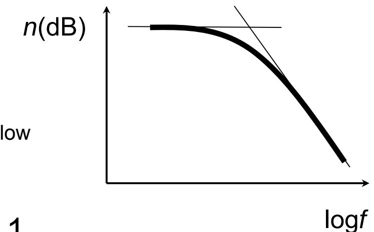
at high frequencies : if $\omega \approx \infty, U_{out} = U_{in}$

Low-pass/high-cut **filter**



$R_C = \dfrac{1}{C\omega}$

the capacitor at low frequencies is a discontinuity



$$U_{out} = \frac{\frac{1}{C\omega}}{\sqrt{R^2 + \frac{1}{C^2\omega^2}}} U_{in} = \frac{1}{\sqrt{R^2C^2\omega^2 + 1}} U_{in}$$

at low frequencies: if $\omega << \omega_0$ $(\omega \approx 0), U_{out} = U_{in}$

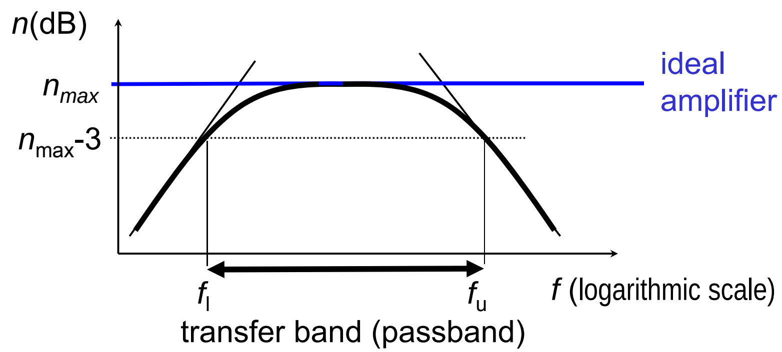
at high frequencies: if $\omega >> \omega_0, U_{out} = \dfrac{1}{RC\omega} U_{in}$ ↔ -6 dB/octave

at very high frequencies : if $\omega >> \omega_0$ $(\omega \approx \infty), U_{out} = 0$

for (1): A_P>1,

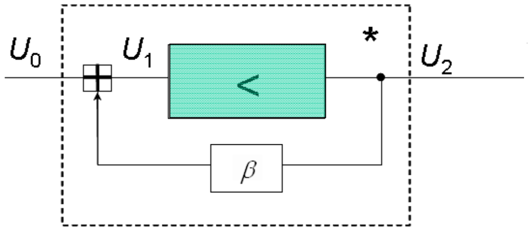
n=10 lg A_P = 20 lg A_U > 0 dB

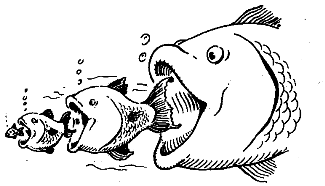
for (2): **frequency characteristics**



f_l : lower frequency limit f_u : upper frequency limit

Amplifier with feedback





Without appropriate perspective we may not recognize our real position.

$(a)\quad U_1 = U_0 + \beta U_2 \qquad (b)\quad A_U = \frac{U_2}{U_1}$

$(c)\quad A_U^* = \frac{U_2}{U_0} = \frac{U_1 A_U}{U_0} = \frac{(U_0 + \beta U_2) A_U}{U_0} = A_U + \beta \frac{U_2}{U_0} A_U = A_U + \beta A_U^* A_U$

$A_U^* - \beta A_U^* A_U = A_U \qquad \boxed{A_U^* = \frac{A_U}{1 - \beta A_U}}$

$\boxed{A_U^* = \frac{A_U}{1 - \beta A_U},}$ A_U^*: voltage gain with feedback

A_U: voltage gain without feedback

$\beta > 0$, **positiv feedback** (same phase), $A_U^* > A_U$ (advantage)

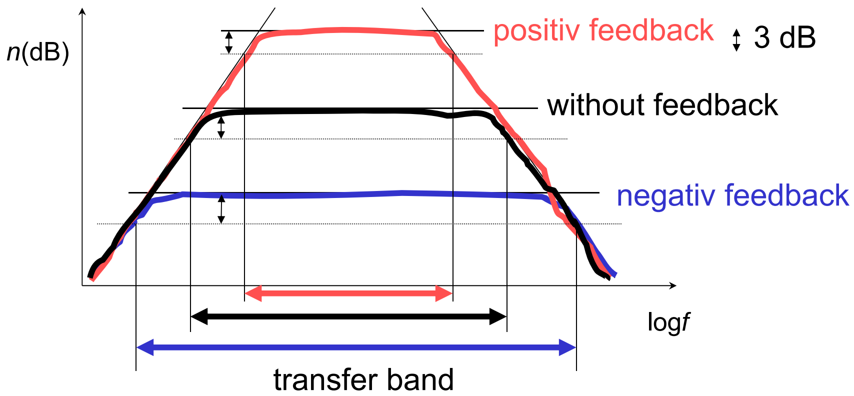
$\beta < 0$, **negativ feedback** (in opposite phase), $A_U^* < A_U$ (disadv.)

positiv feedback:

(a) $\beta A_U = 1$, amplification: „infinite“
– sine wave oscillator
e.g.: ultrasound generator, heat theraphy

(b) $\beta A_U \leq 1$, amplification: very big
– regenerative amplifier
e.g.: hearing, outer haircells

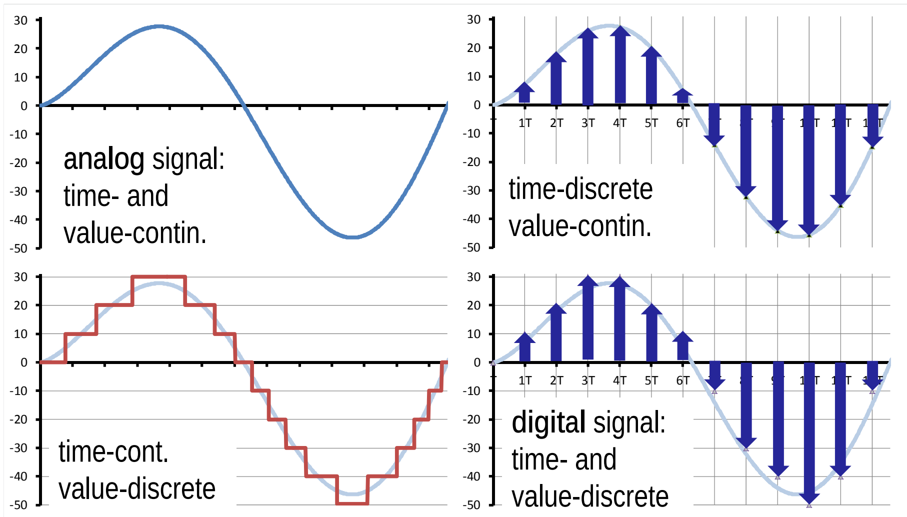
negativ feedback: „all“ amplifier



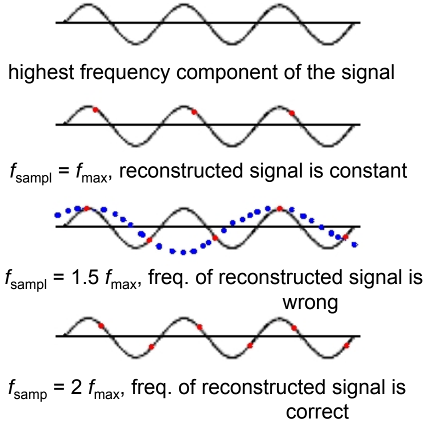
positiv feedback: transfer band – narrrower (big disadvantage)
higher gain (advantage)

negativ feedback: transfer band – broader (advantage)
less gain (small disadvantage)

Analog signal – digital signal



time-discrete: the value of the signal is not known for all moments in time



Nyquist–Shannon sampling theorem:

for complete reconstruction the minimum sampling frequency should be twice the frequency of the highest overtone of the signal

e.g.: hifi, f_{max} = 20 kHz

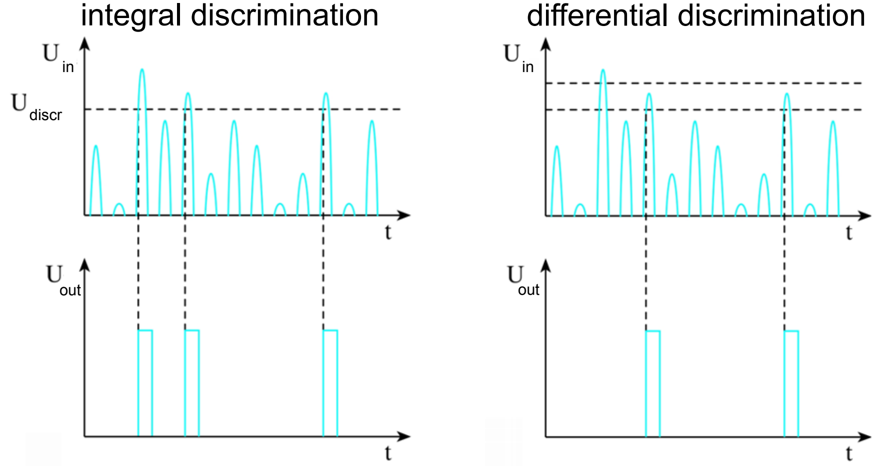
f_{sampl} = 44.1 kHz > 2*20 kHz

value discrete: the value of the signal can not be arbitrary

e.g.: hifi, 16 bit = 2^{16} = 65 536 (CD standard)

24 bit = 2^{24} = 16 777 216 (“best” audio card)

Pulse processing



to select only those pulses that are larger than a preset amplitude

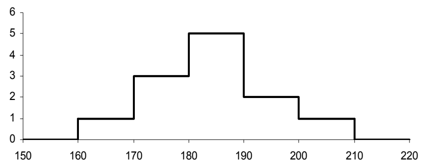
to select only those pulses whose amplitudes lie within a preset window

Textbook, Figure VII.32.

Distribution functions and ID/DD ”spectra”

$\frac{\Delta N}{\Delta h}\left(\frac{1}{10\,\mathrm{cm}}\right)$

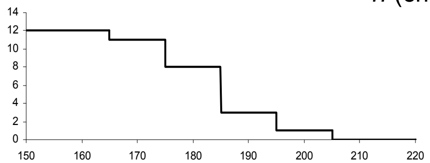
density function



DD-”spectrum”

$M=N_0-N$

”cumulative-distribution-function”

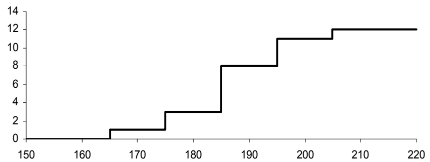


ID-”spectrum”

how many pulses are larger than *h*?

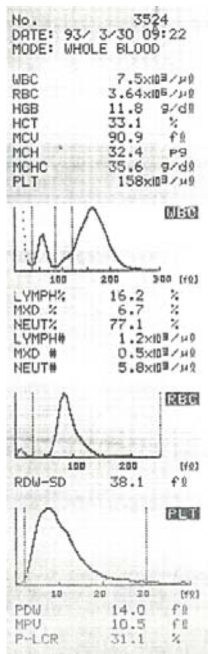
N

cumulative-distribution-function



how many pulses are smaller than *h*?

Concentration of white blood cells


No. 3524
DATE: 93/ 3/30 09:22
MODE: WHOLE BLOOD

WBC 7.5x10³/μl
RBC 3.64x10⁶/μl
HGB 11.8 g/dl
HCT 33.1 %
MCV 90.9 fl
MCH 32.4 pg
MCHC 35.6 g/dl
PLT 158x10³/μl

WBC
LYMPH% 16.2 %
MXD % 6.7 %
NEUT% 77.1 %
LYMPH# 1.2x10³/μl
MXD # 0.5x10³/μl
NEUT# 5.8x10³/μl

RBC
RDW-SD 38.1 fl

PLT
PDW 14.0 fl
MPV 10.5 fl
P-LCR 31.1 %

Coulter counter