

Biomechanics of Bimolecules and tissues

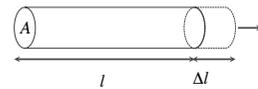
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Basics of tissue mechanics

Hooke's law



$$\frac{F}{A} = E \frac{\Delta l}{l}$$

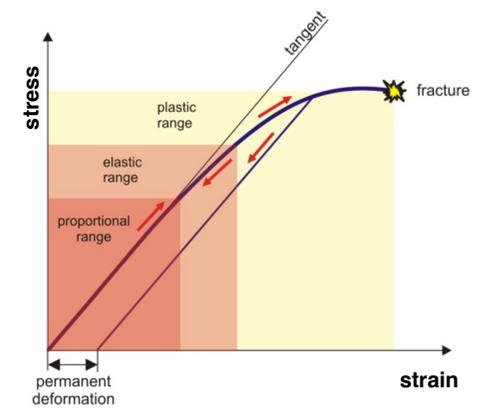
$$\sigma = E \varepsilon$$

F = force
A = cross sectional area
l = rest length
Δl = extension

$F/A = \sigma = \text{stress (N/m}^2 = \text{Pa)}$
 $\Delta l/l = \varepsilon = \text{strain (dimensionless)}$
 $E = \sigma / \varepsilon \text{ Young's modulus (Pa)}$

(elastic modulus - the name is misleading! it describes stiffness)

Stress-strain diagram

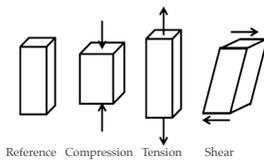


Biomechanics at the cellular level

Forces at work in tissues

Forces in tissues result from:

- cell generated tension
- fluid flow
- movement (stretch)
- hydrostatic/osmotic pressure



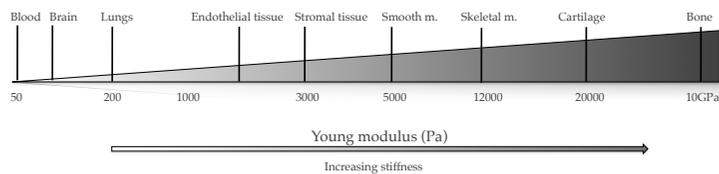
Forces as mechanical signals

- highly directional
- decay: $1/r$
- convey complex spatial information
- communication over long range
- rapid regulation
- no diffusible intermediate

Soluble (chemical) signals:

- diffuse rapidly (not directional)
- decay: $1/r^2$
- shorter range of communication
- need of diffusible intermediates

Cellular dimensions:
Length: μm Force: pN
 $1\text{Pa} = 1\text{pN}/\mu\text{m}^2$



Flashback: What did you learn about ultrasound propagation.... ?

How much is the speed of sound in different tissues?
Acoustic properties of various tissues are determined by their mechanical properties.

	E (GPa)	K (GPa ⁻¹)	c _{sound} (m/s)
Bone	18	0.05	3600
Muscle	7x10 ⁻⁵	0.38	1568

$$c_{\text{sound}} = \frac{1}{\sqrt{\rho \cdot \kappa}}$$

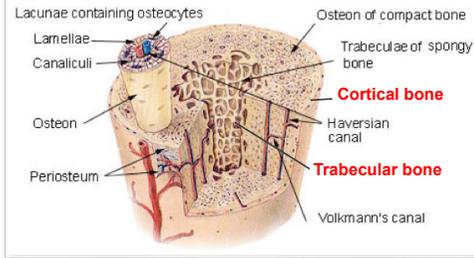
$\kappa = \frac{-\Delta V/V}{\Delta p}$
 strain (top), stress (bottom), compressibility (left)

Greater Young-modulus, faster sound speed

Bone

Due to the different structure of bone tissue along the cross section of long bones, the Young's modulus distribution is anisotropic. Denser cortical bone has greater Young's modulus vs. the trabecular bone..

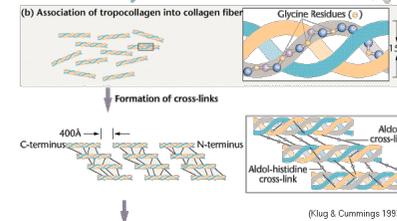
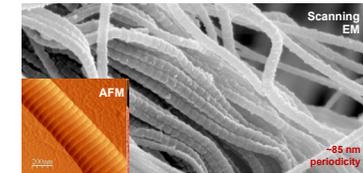
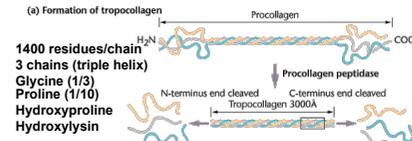
Young's modulus: 5-20 GPa
 Decalcified bone (acid treatment): flexible
 Removal of organic compounds (heating): brittle



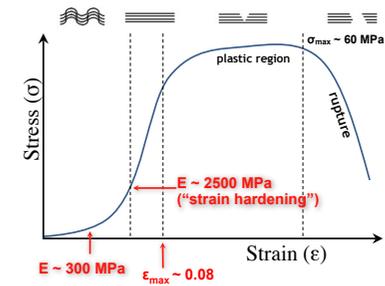
Calculation:

Bone has a Young's modulus of about 18 GPa. Under compression, it can withstand a stress of about 1.60×10^8 Pa before breaking. Assume that a femur (thigh-bone) is 46 cm long, and calculate the amount of compression this bone can withstand before breaking.

Collagen



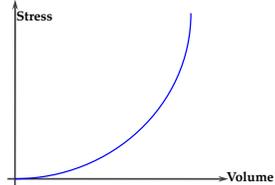
Post translational modification is necessary for tropocollagen polymerization
 Hydroxylation of lysin and praline residues requires vitamin-C as cofactor!



Elastic arteries

Non-linear elasticity

Strain is not linearly proportional to stress.

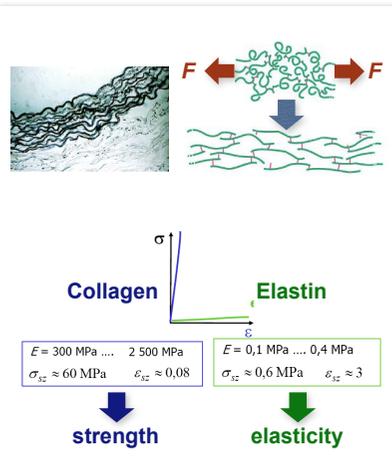


Determinants of vascular elasticity:

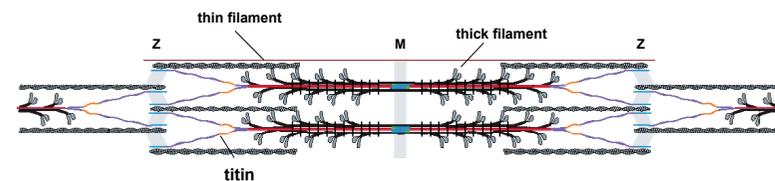
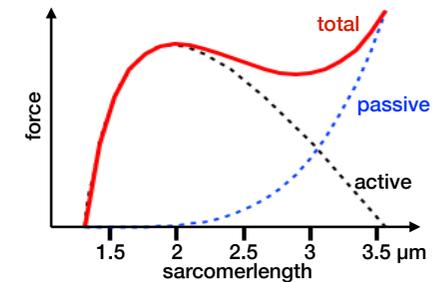
- Elastin
- Collagen
- Smooth muscle

Implications of vascular elasticity:

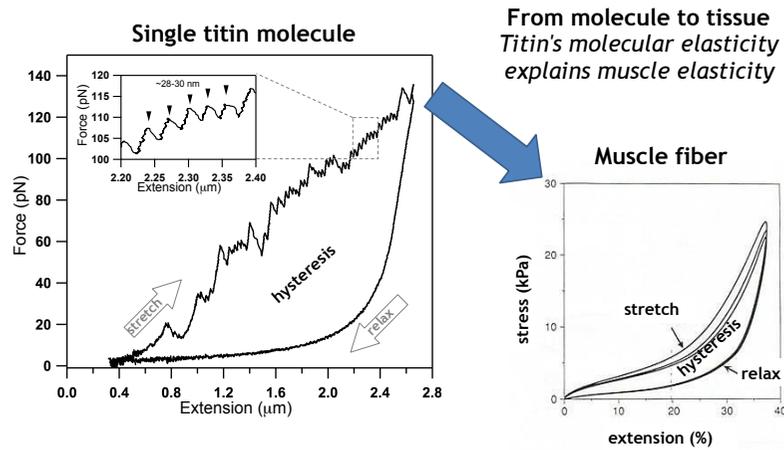
- Storage of potential (elastic) energy
- Dampening of pressure pulses
- Constant flow rate



Titin: the elastic filament of the sarcomere



Titin is the main determinant of muscle elasticity

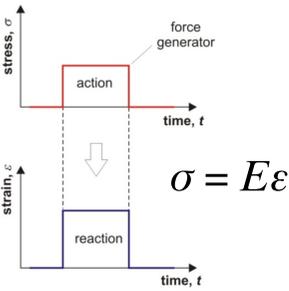
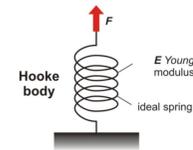


13

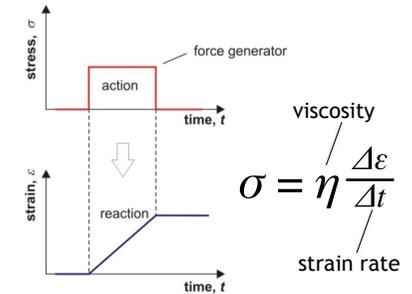
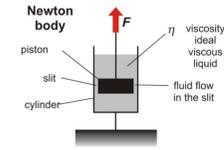
Viscoelasticity

(mechanical model)

Elastic body



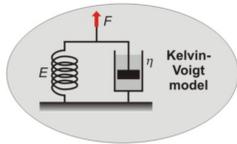
Viscous body



14

Viscoelasticity

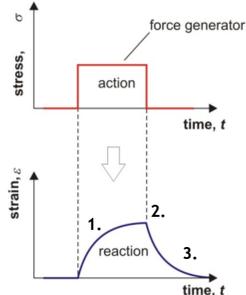
(mechanical model)



Viscoelasticity means to co-appearance of viscous and elastic behavior. A

model: parallel connection of spring and dashpot
(Kelvin-Voigt model)

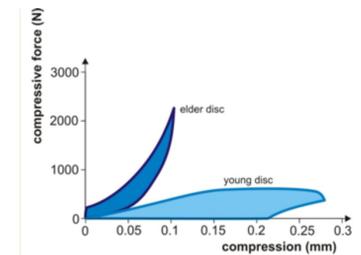
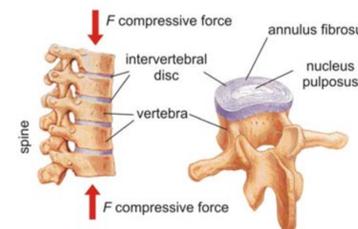
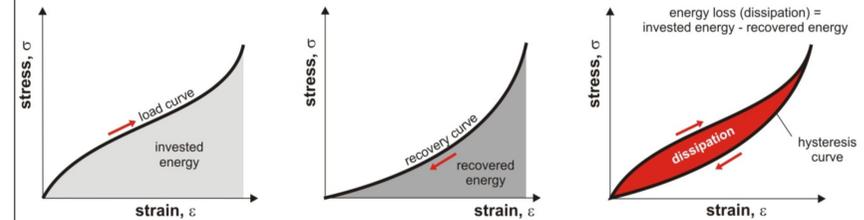
Spring: ideal elastic (Hooke) body
Dashpot: ideal viscous (Newton) body



1. Upon stretch, the extension of the spring is slowed down by the dashpot.
2. Extension stops when the elastic spring force equals the external force.
3. When the external force is quenched, the contraction of the spring is slowed down by the dashpot.

15

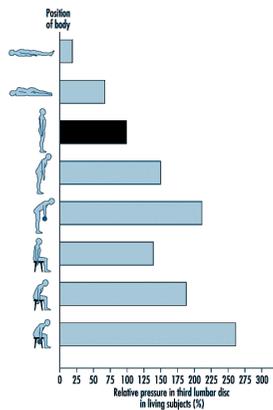
Energy dissipation in viscoelastic system



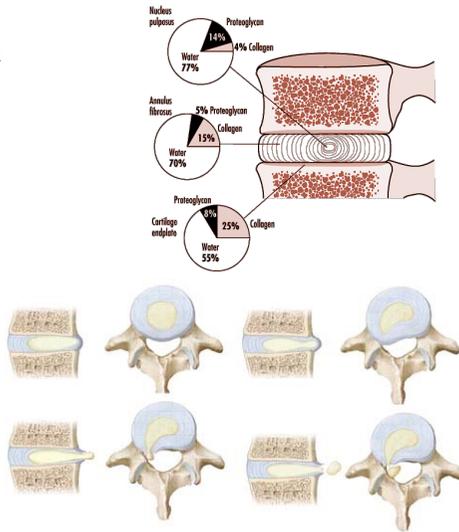
16

Example I. Consequences of increased mechanical stress on intervertebral discs (*discus hernia*)

Relative stress on L3 intervertebral disc at various positions



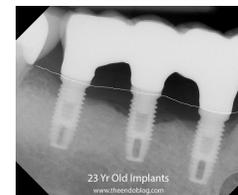
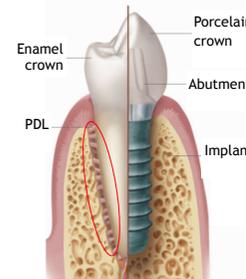
Source: Adapted from Nachemson 1992.



17

Example II: Implants vs natural tooth

PDL makes the difference!



Absence of PDL results in:

- loss of masticatory force perception
- loss of viscoelastic dampening
- loss of force sensory mechanism
- no implant movement

Implant is in direct contact with bone tissue



Increased compressive stress during mastication



Bone loss (0.2 mm /year)
Loss of gingival height

Implants ↔ Root canal treatment

18

Calculations

To stretch a relaxed biceps muscle 3 cm requires a force of 25 N. To do the same stretch of a contracted muscle at its maximal tension requires a force of 500 N. Find the Young's modulus for both relaxed and tense muscle tissue. Assume the biceps is a uniform cylinder of length 20 cm and diameter 6 cm. (59 kPa, 1.18 MPa)

Collagen fiber is stressed with 12 N force. The cross-sectional area of the fiber is 3 mm², its coefficient of elasticity is 500 MPa. Give the percentage of relative extension. (0.8 %)

The length of an elastic thread used in orthodontics is 6 cm, its cross-sectional area is 1 mm², its coefficient of elasticity is 5 MPa. We extend the thread with 40 %. How large is the retracting force and what is the amount of elastic energy stored in the thread?(F=2N,E=24mJ)

19