Physical bases of dental material science

Biomechanics
Biomolecular and dental tissue mechanics

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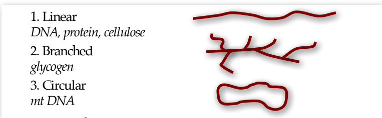
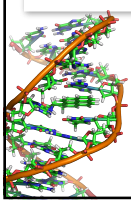
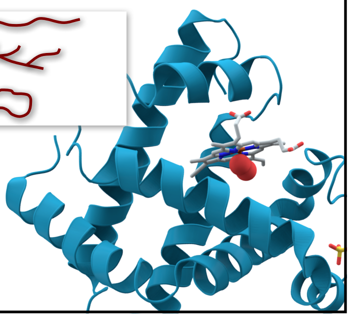
Biomolecules are polymers

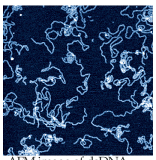
Common feature: **Linear primary structure (protein, DNA)**
Strong bonds between monomers (covalent)
Weaker interactions between distant region of polymer chain



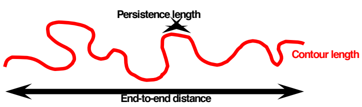




What is the shape of biopolymers?


AFM image of dsDNA

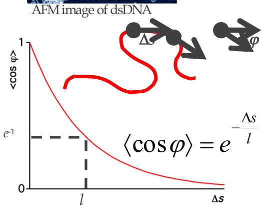
Parameters to describe the shape of polymer



Contour length (L): Full length of the chain

End-to-end distance (R): Distance between chain termini.

Persistence length (*l*) : describe the persistence of chain orientation.



$$\langle \cos\varphi \rangle = e^{-\frac{\Delta s}{l}}$$

Shorter persistence length polymers are more flexible.

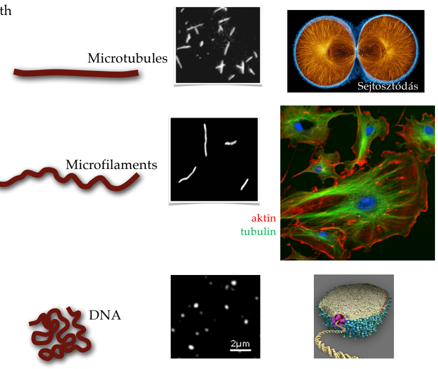
Biopolymer classification based on flexibility

l = persistence length
L = contour length

RIGID
$l >> L$

SEMIFLEXIBLE
$l \approx L$

FLEXIBLE
$l << L$



Are biopolymers elastic?

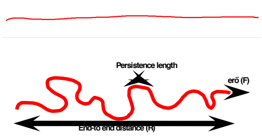
Yes, but Hooke's law is not valid! Non-linear elasticity.

Entropic elasticity

Thermal energy (k_BT) excites bending movements in the chain

The chain's disorder (entropy) increases

The chain shortens

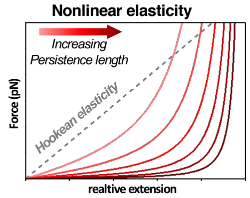


Force is needed to stretch an entropic chain

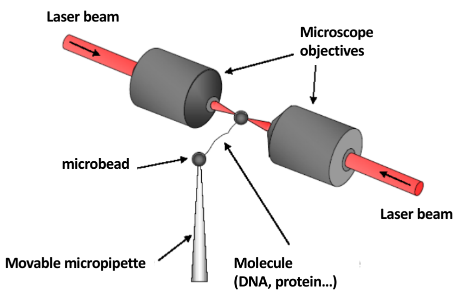
$$F \sim \frac{k_B T}{l} \cdot \frac{R}{L} + \left(\frac{R}{L}\right)^a$$

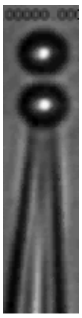
F = force
l = **persistence length**
k_B = Boltzmann constant
T = absolute temperature
L = contour length
R = end-to-end distance
R/L = relative extension

Nonlinear elasticity



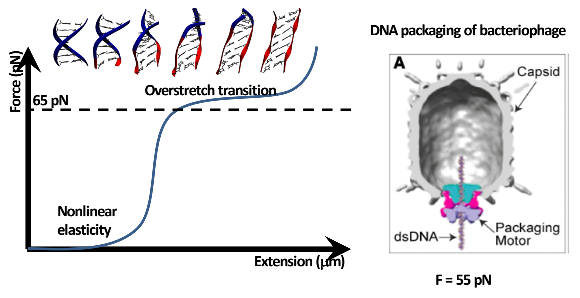
How to stretch single molecules?
Optical tweezers



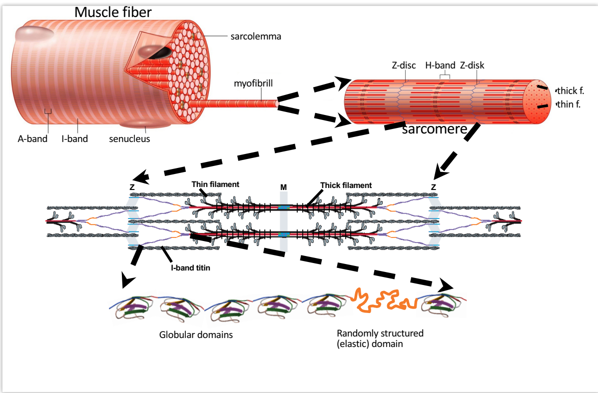


http://glass.phys.uniroma1.it/dileonardo/Applet.php?applet=TrapForcesApplet

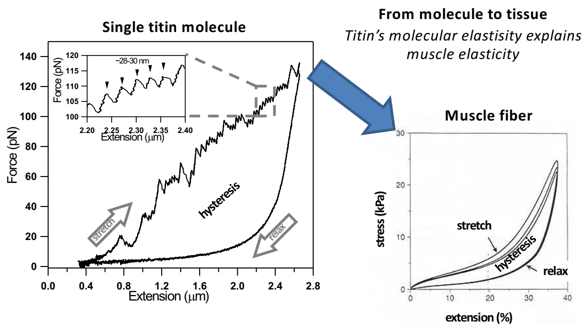
Stretching dsDNA with optical tweezers



Titin: elastic filament of the sarcomere



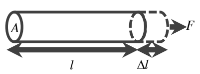
Titin is the main determinant of muscle elasticity



Dental tissue mechanics

Basics of tissue mechanics

Hookean elasticity

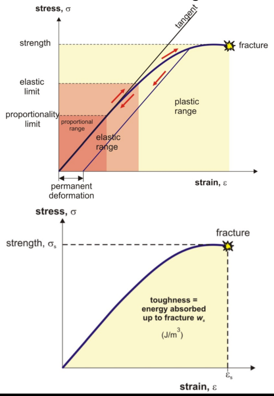


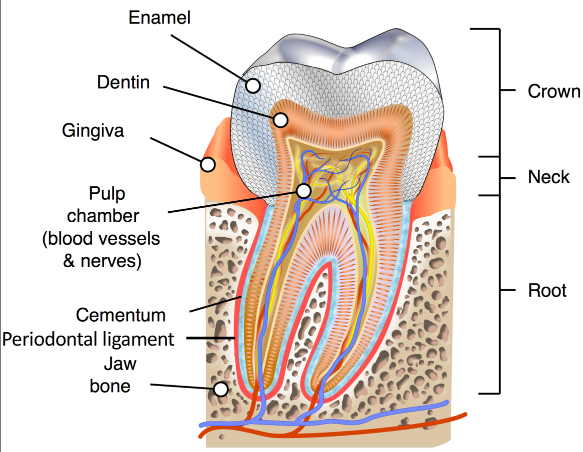
$$\frac{F}{A} = E\frac{\Delta l}{l}$$

F = force
A = cross sectional area
l = rest length
Δl = extension

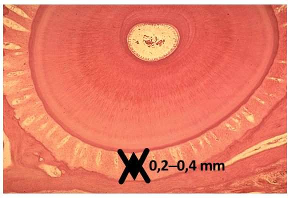
F/A = σ = stress (N/m² = Pa)
$\Delta l/l$ = ε = strain (dimensionless)
E= σ / ε Young's modulus (Pa)

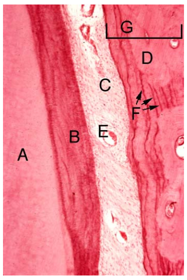
Stress-strain diagram





Periodontal ligament





≈ collagen

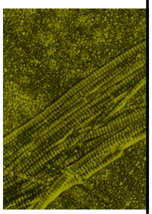
polimer

Collagen

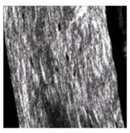
Structural protein, main component of connective tissues, in mammals about 25% of the total protein is collagen. Has an important role in:

- tendons, ligaments,
- skin,
- cartilage,
- bone,
- tooth,
- blood vessels
- vitreous humor,
- cornea,
- etc.

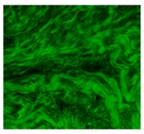
eye



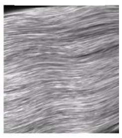
bone



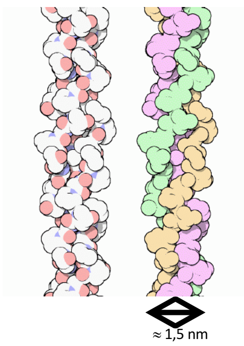
skin



tendon

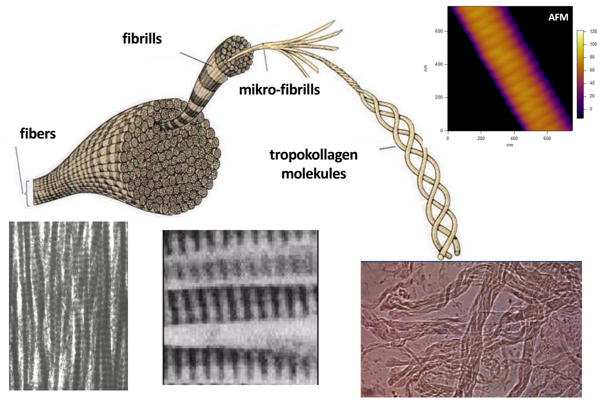


The collagen molecule



- 1400 aminoacids/chain
- glicin (1/3),
  prolin (1/10),
  hidroxiprolin, ...
- 3 chains → triple helix

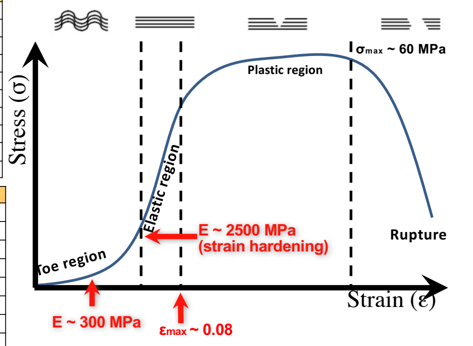
The structure of collagen



Stretch diagram of collagen

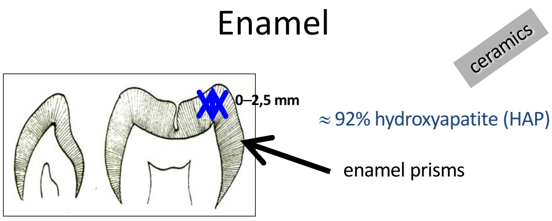
material	E (GPa)
enamel	≈ 100
dentin	≈ 15
steel	200-230
amalgam	50-60
gold	79
glass	60-90
ceramics	60-130
porcelain	60-110
PMMA	2,4-3,8
silicon	≈ 0,0003

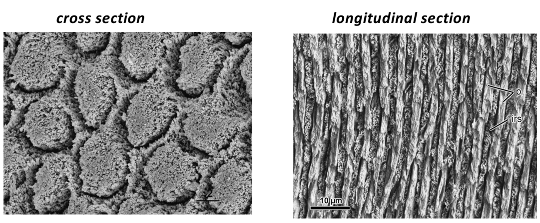
material	$\sigma_{sz, szakító}$ (MPa)
enamel	≈ 10
dentin	≈ 110
amalgam	30-55
gold	108
Ni-Cr alloys	400-900
glass	≈ 70
ceramics	5-400
porcelain	≈ 25
PMMA	≈ 50



Moderately elastic and tough, but soft

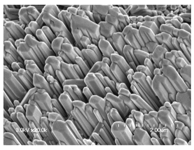
Enamel



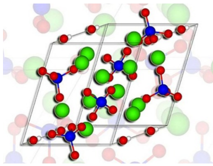


Hydroxyapatite

$Ca_{10}(PO_4)_6(OH)_2$



hexagonal ionic cristal



in dentin and bone

20-60 nm x 6 nm crystals

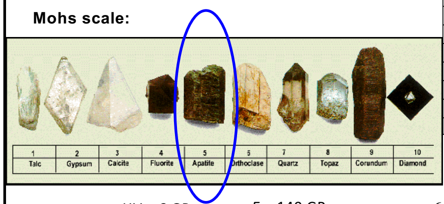
in enamel:

500-1000 nm x 30 nm crystals

Properties of hydroxyapatite

material	*HV* (MPa)
enamel	≈ 3400
dentin	≈ 600
amalgam	≈ 1000
gold	
gold alloys	600-250
Pd-Ag alloys	1400-1900
Co-Cr alloys	≈ 4000
Ni-Cr alloys	3000-4000
glass	
porceelain	4500-7000
akrylate	≈ 200

Mohs scale:



HAP: $HV \approx 6$ GPa $E \approx 140$ GPa $\sigma_S \approx 60$ MPa (bending)

≈ 500 MPa (compression)

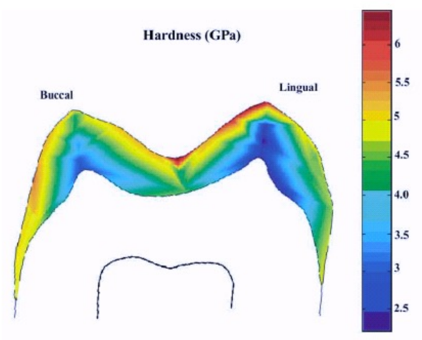
enamel: $HV \approx 3\text{-}6$ GPa $E \approx 90\text{-}100$ GPa $\sigma_S \approx 50$ MPa (tension)

≈ 400 MPa (compression)

Rigid, hard, strong but brittle!

20

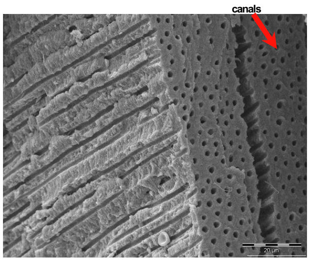
Hardness distribution of enamel crown



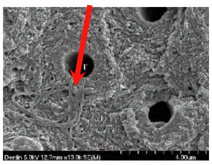
Dentin

composite

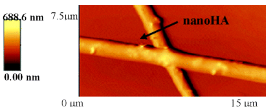
moderately hard, very strong and tough



about 1/3 organic + water
(collagen fibers)

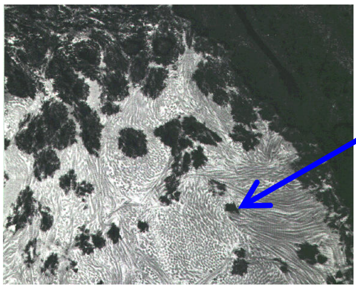


about 2/3 inorganic
(HAP crystals on collagen fibers)



Cementum

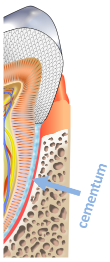
composite



≈ 50% organic + water (collagen!)

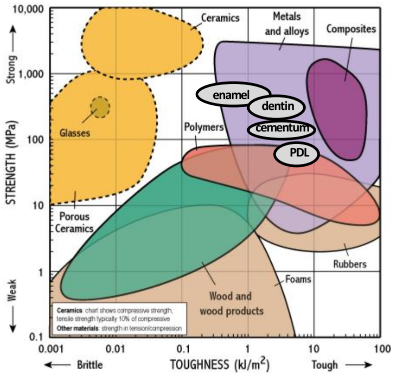
≈ 50% HAP

HAP crystals



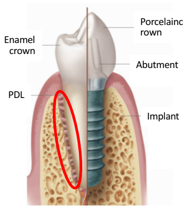
Summary

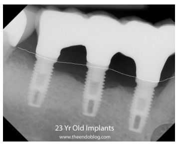
	PDL (≈ collagen)	dentin (≈1/3 collagen, 2/3 apatite)	enamel (≈ apatite)
stiffness (E) (GPa)	0,3–2,5	10–20	90–100
strength (σ_{max}) (MPa)	60	110 (tensile) 300 (compress)	50 (tensile) 400 (compress)
toughness (kJ/m^3)	1–10	0,5–5	0,1–1
hardness HV (GPa)		0,5–1	3–6



Example: Implants vs nastural tooth

PDL makes the difference!





Absence of PDL result in :

- **loss of masticatory force perception**
- **loss of visco-elastic (damper) effect**
- **loss of force sensory mechanisms**
- **No implant movement**

Implant is in direct contact with bone tissue

⬇

Increased compressive stress

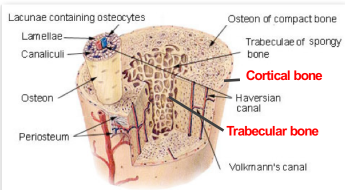
⬇

Bone loss (0.2 mm / year)
Loss of gingival height

Implants ⬄ Root Canal Treatment

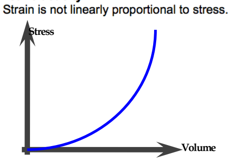
Bone

Due to the different structure of bone tissue along the cross section of long bones, the **Young's modulus distribution is anisotropic**. Denser cortical bone has greater Young's modulus vs. the trabecular bone..
Young's-modulus: 5-20 GPa
Decalcified bone (acid treatment): flexible
Removal of organic compounds (heating): brittle



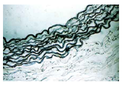
Biomechanics of elastic arteries

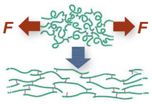
Non-liear elasticity
Strain is not linearly proportional to stress.



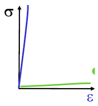
Determinants of vascular elasticity:
- Elastin
- Collagen
- Smooth muscle

Implications of vascular easticity:
- Storage of potential (elastic) energy
- Dampening of pressure pulses
- Constant flow rate





Collagen



Elastin

Collagen	Elastin
E = 300 MPa .... 2 500 MPa	E = 0,1 MPa .... 0,4 MPa
$\sigma_{sz} \approx 60$ MPa $\varepsilon_{sz} \approx 0{,}08$	$\sigma_{sz} \approx 0{,}6$ MPa $\varepsilon_{sz} \approx 3$

strength

elasticity