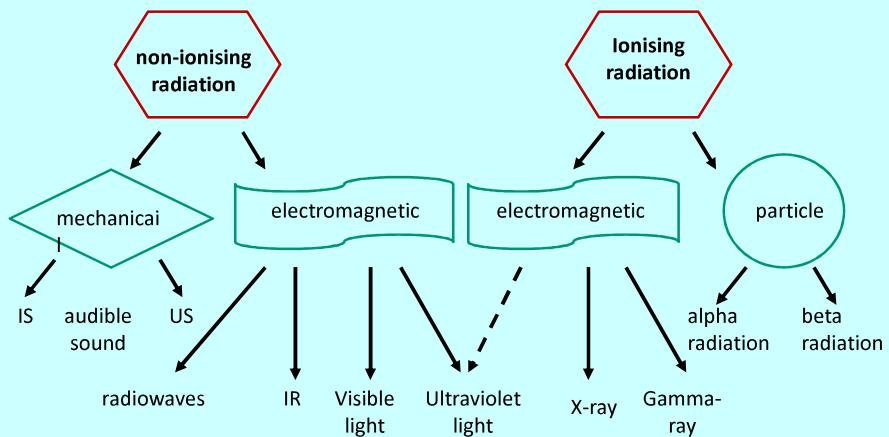


## Radiation



1

## Sound

and

ultrasound



2

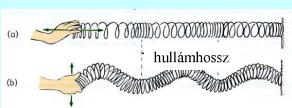
## Physics of sound

Longitudinal vs. Transverse wave



*longitudinal wave*

(in the interior of liquids and gases only this type)

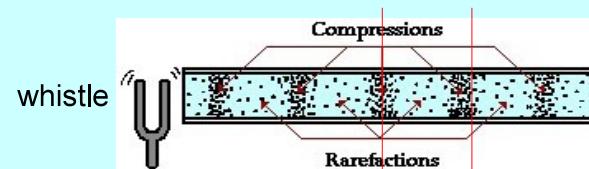


*transverse wave*

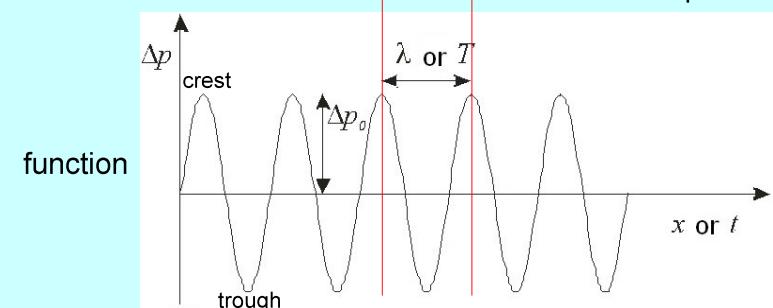
can generated in solid materials and at liquid surfaces

Sound: mechanical wave (model)

## Physics of sound



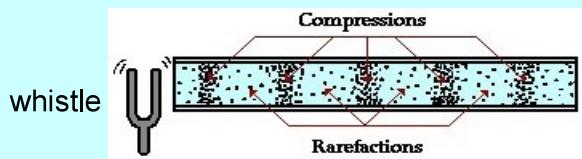
spring



spatial and temporal periodicity

3

4



hydrostatic pressure      pressure change, sound pressure

$$p_{\text{total}} = p_{\text{hydrostat}} + \Delta p$$

pressure DC + AC

amplitude

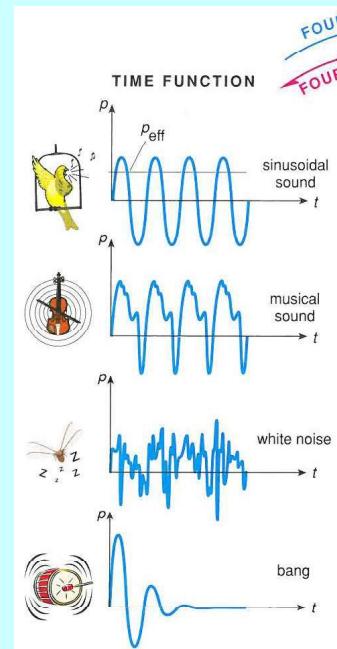
phase

$$\Delta p(t, x) = \Delta p_{\max} \sin\left[2\pi\left(\frac{t}{T} - \frac{x}{\lambda}\right)\right]$$

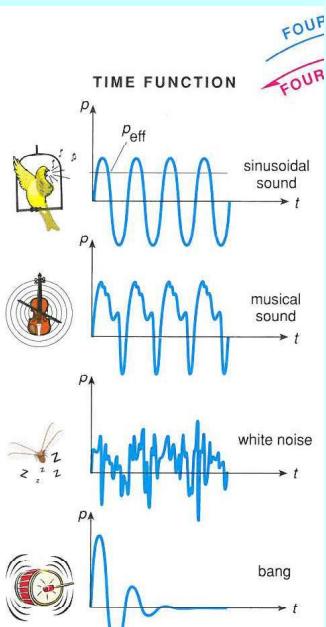


$$c \cdot T = \lambda, \quad c = f \cdot \lambda$$

5



$$p(t) = p_1 \sin(\omega t) + p_2 \sin(2\omega t) + p_3 \sin(3\omega t) + \dots$$



**pitch**  
frequency of the fundamental

height

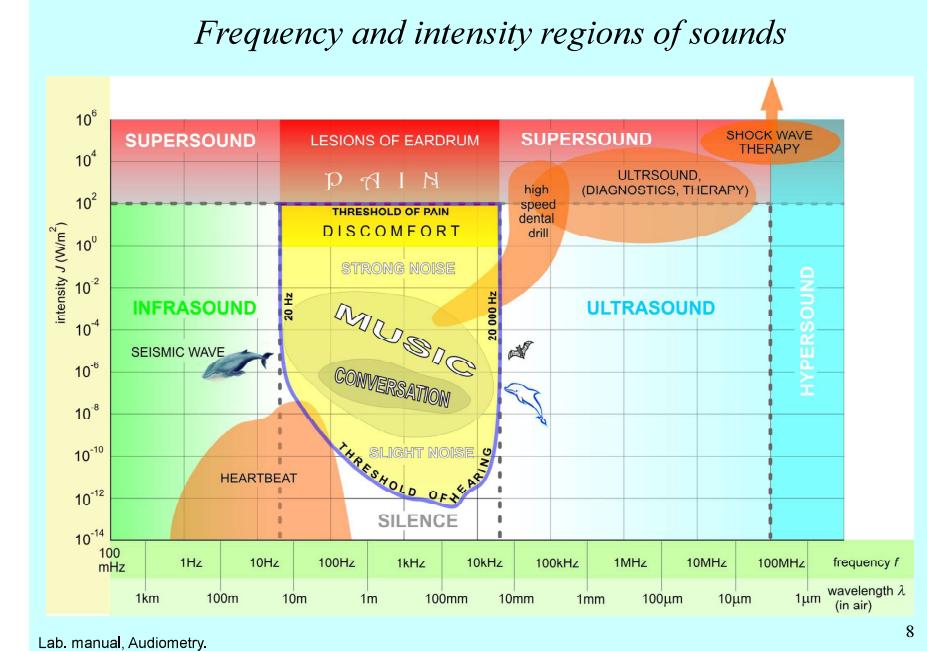
**timbre**  
relative strengths of overtones/harmonics (spectrum)

tone colour

**Intensity\***  
from pressure amplitude

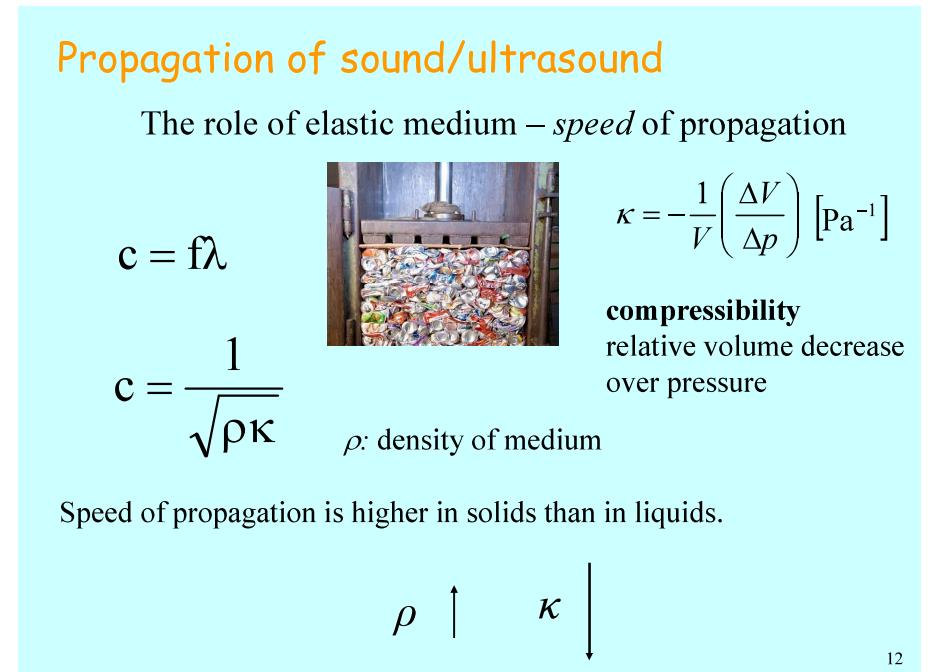
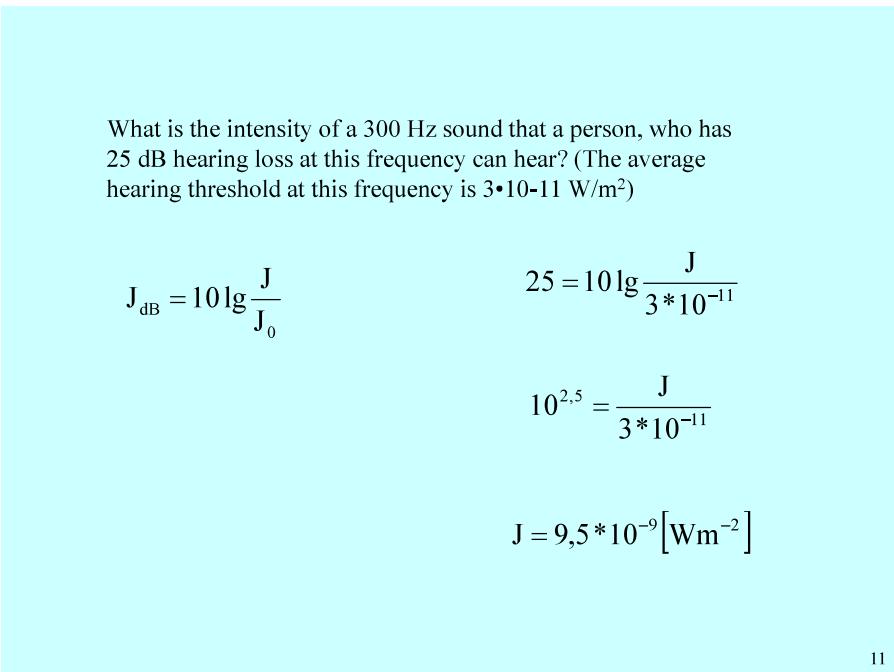
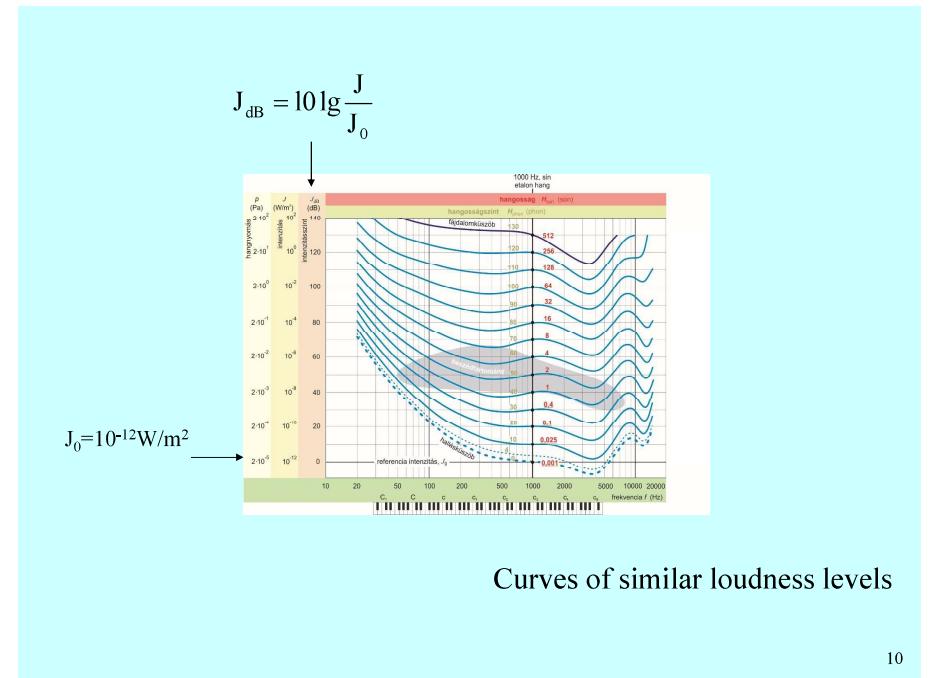
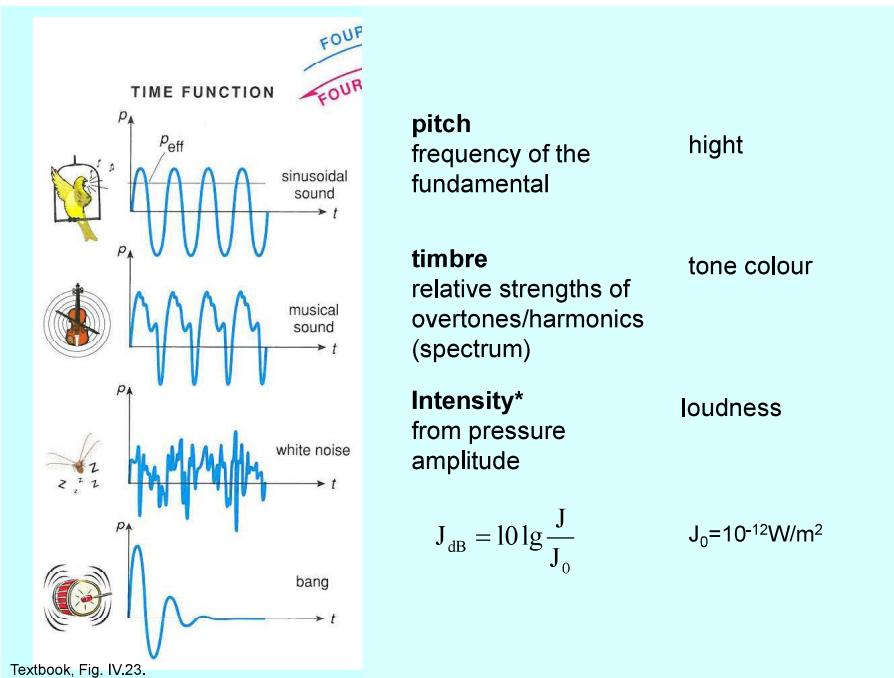
loudness

Textbook, Fig. IV.23.



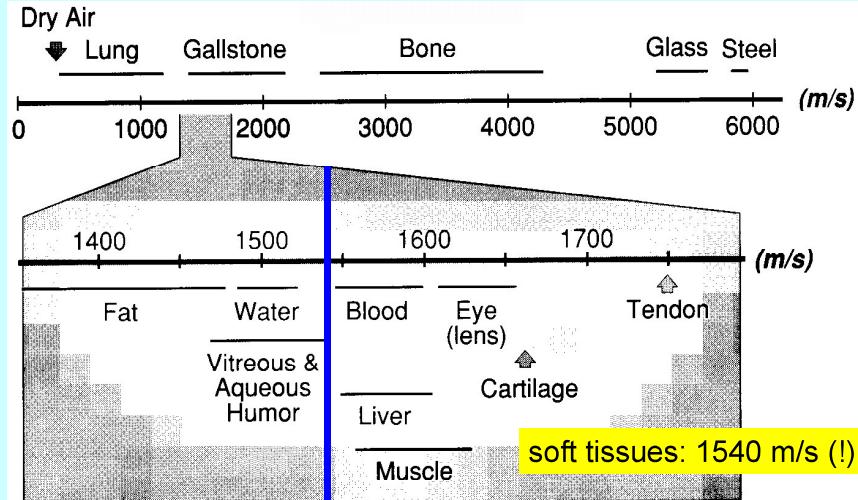
Lab. manual, Audiometry.

8





### Speed of sound/US in various media



### Propagation of sound/ultrasound

$$c = \frac{1}{\sqrt{\rho \kappa}}$$



$$\kappa = \frac{-\Delta V/V}{\Delta p} \quad [\text{Pa}^{-1}]$$

$$Z = \frac{p}{v} = \frac{p_{\max}}{v_{\max}}$$

acoustic impedance  
(definition)

$$Z = c\rho = \sqrt{\frac{\rho}{\kappa}}$$

acoustic impedance  
(useful form)

$$Z_{\text{el}} = \frac{U}{I}$$

$$[\text{kg/m}^2 \text{s}]$$

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### Propagation of sound/ultrasound

$$c = \frac{1}{\sqrt{\rho \kappa}}$$

$$\kappa = \frac{-\Delta V/V}{\Delta p}$$

$$Z = c\rho = \sqrt{\frac{\rho}{\kappa}}$$

material	$\rho$ [kg/m <sup>3</sup> ]	$\kappa$ [1/GPa]	$c$ [m/s]	$Z$ [kg/(m <sup>2</sup> s)]
air	1,3	7650	331	0,00043 · 10 <sup>6</sup>
water 20°C	998	0,45	1492	1,49 · 10 <sup>6</sup>
aluminum	2700	0,009	6400	17,28 · 10 <sup>6</sup>
quartz	2650	0,011	5736	15,2 · 10 <sup>6</sup>

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#### Problem:

A sound beam of 3 MHz frequency and 50 mW/cm<sup>2</sup> intensity propagates in blood.

What is the pressure? What is the maximal displacement and velocity of particles in this beam?

$$Z_{\text{blood}} = 1,66 \times 10^6 \text{ kg/m}^2 \text{ s}$$

#### Solution:

Intensity:

$$J = \frac{p_{\max}^2}{2Z}$$

$$p = \sqrt{2JZ} = 40.74 \text{ kPa}$$

Velocity:

$$v = \frac{p}{Z} = \frac{40,74 \cdot 10^3}{1,66 \cdot 10^6} = 0,0245 \text{ m/s} = 24,5 \text{ mm/s}$$

Displacement:

$$A = \frac{v}{\omega} = \frac{24,5}{2 \cdot \pi \cdot 3 \cdot 10^6} = 1,3 \cdot 10^{-6} \text{ mm} = 1,3 \text{ nm}$$

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## Intensity of US

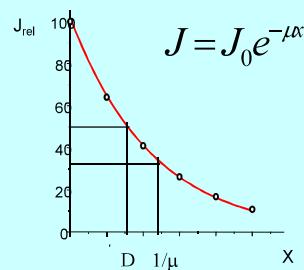
$$J = \frac{1}{Z} \Delta p_{\text{eff}}^2$$

intensity = energy/current density

$$P_{\text{el}} = \frac{1}{Z_{\text{el}}} U_{\text{eff}}^2$$

electric analogy

## Loss of energy during propagation (absorption)



$$\text{attenuation: } \alpha = 10 \cdot \lg \frac{J_0}{J} \text{ dB}$$

$$\alpha = 10 \cdot \mu \cdot x \cdot \lg e \text{ dB}$$

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$\mu$  is proportional to frequency in the diagnostic range

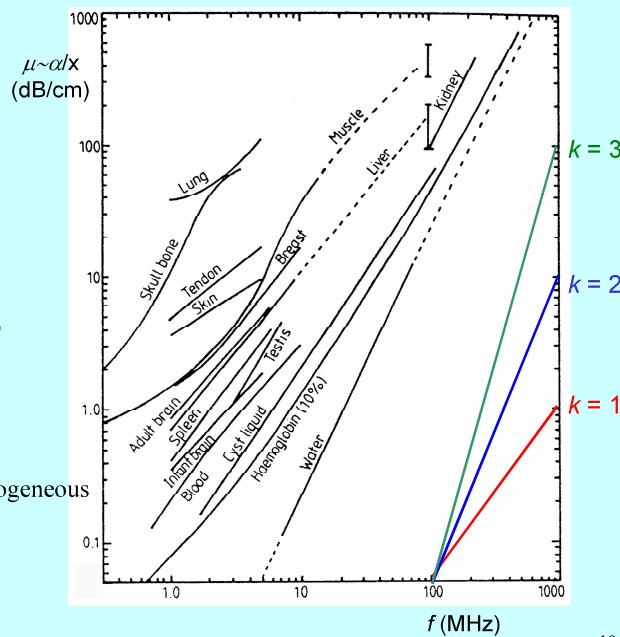
$$\mu \sim f^k, \quad k \sim 1 (?)$$

$$\log \mu \sim k \log f$$

if the graph is a linear, the power function approximation is valid

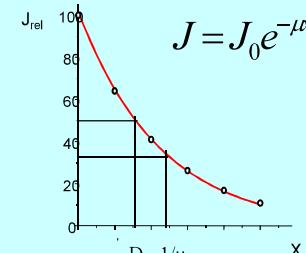
specific attenuation for soft tissues (homogeneous tissue model):

$$\frac{\alpha}{f x} \sim 1 \frac{\text{dB}}{\text{cm MHz}}$$



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## Loss of energy during propagation (absorption)



$$\text{attenuation: } \alpha = 10 \cdot \lg \frac{J_0}{J} \text{ dB}$$

$$\alpha = 10 \cdot \mu \cdot x \cdot \lg e \text{ dB}$$

$\mu$  is proportional to frequency in the diagnostic range

$$\text{Specific attenuation: } \frac{\alpha}{f \cdot x}$$

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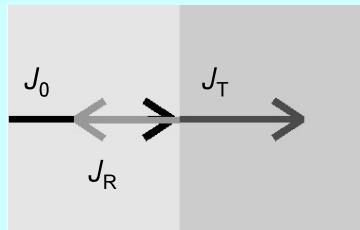
$$\frac{\alpha}{f x} \sim 1 \frac{\text{dB}}{\text{cm MHz}}$$

tissue	Specific attenuation
liver	0,6 – 0,9
kidney	0,8 – 1,0
fat	1,0 – 2,0
blood	0,17 – 0,24
bones	16 – 23

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## Phenomena at the boundary of different media

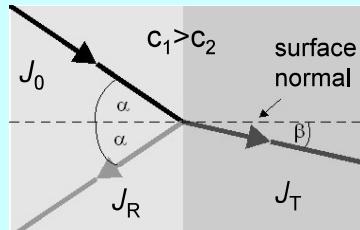
normal/perpendicular incidence



$$J_0 = J_R + J_T$$

reflection and transmission (penetration)

skew incidence

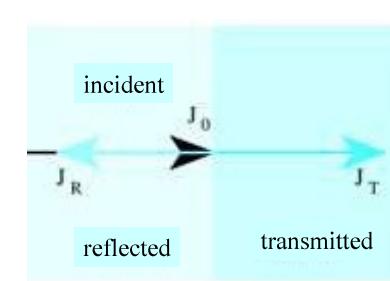


$$\frac{\sin \alpha}{\sin \beta} = \frac{c_1}{c_2}$$

Snellius-Descartes

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## Reflection of ultrasound



$$J_0 = J_R + J_T$$

$$R = \frac{J_R}{J_0}$$

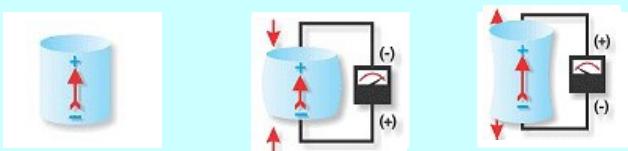
If  $R \approx 1$  Total reflection

$$R = \left( \frac{Z_1 - Z_2}{Z_1 + Z_2} \right)^2$$

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## Detection/Generation of US

### Piezoelectric effect

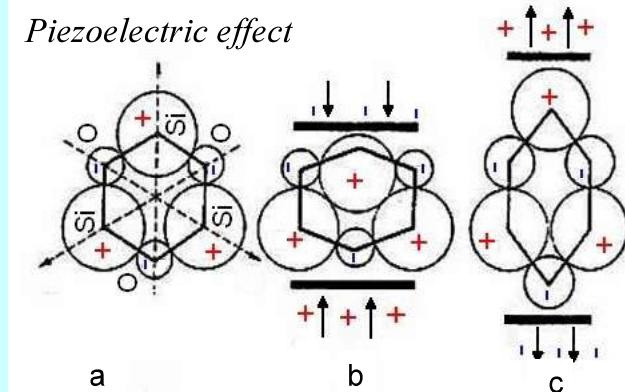


Pressure change

Mechanical deformation of crystal  
Electric potential difference

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### Piezoelectric effect



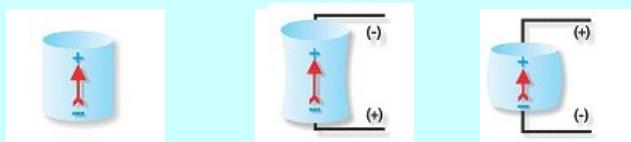
(a) Center of charge of positive and negative charges coincides.

(b) and (c) As a result of pressure, the charge centers are separated, i.e. a potential difference arises

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## Detection/Generation of US

Inverse piezoelectric effect



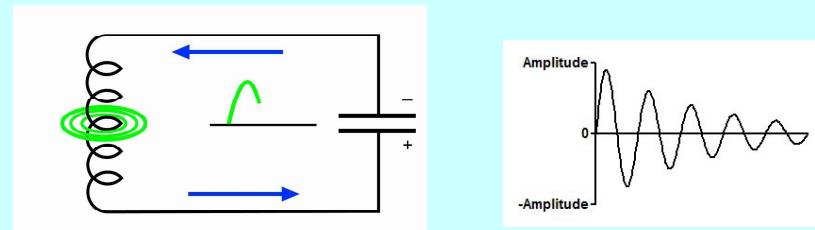
Periodic electric potential difference

The crystal is deformed when voltage is applied

**Mechanical vibration**

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## Oscillator circuit – LC circuit



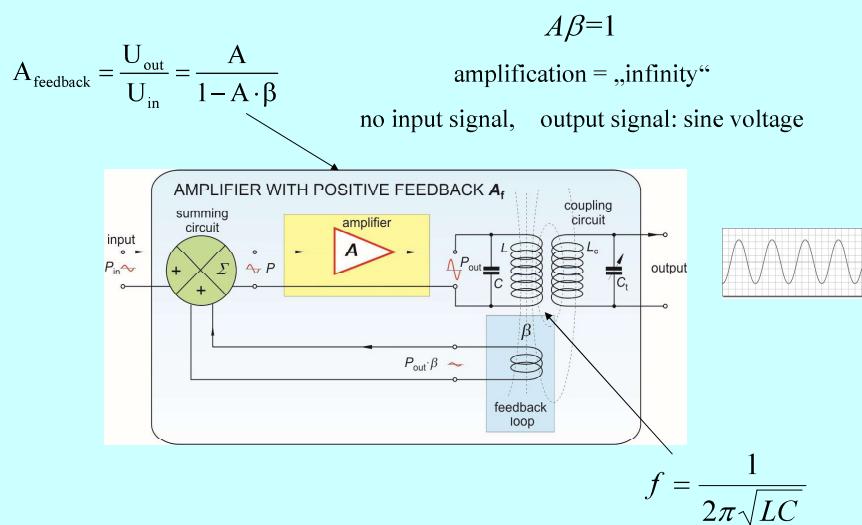
$$f = \frac{1}{2\pi\sqrt{LC}}$$

L : self inductance [ $\text{s} \cdot \Omega^{-1}$ ]

$$L \sim A N^2$$

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## Source of electric signal: sine wave oscillator

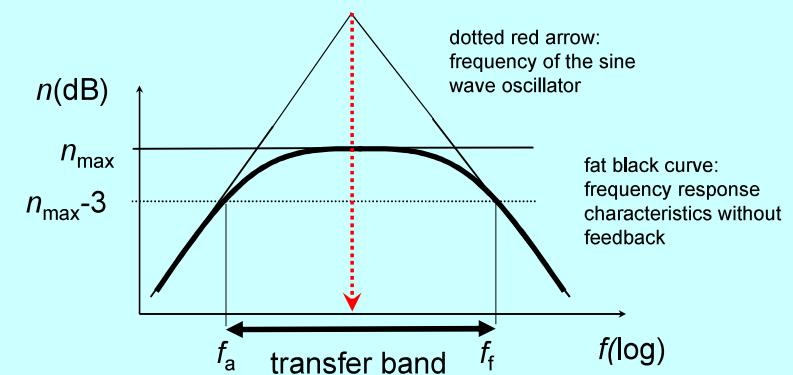


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## Source of electric signal: sine wave oscillator

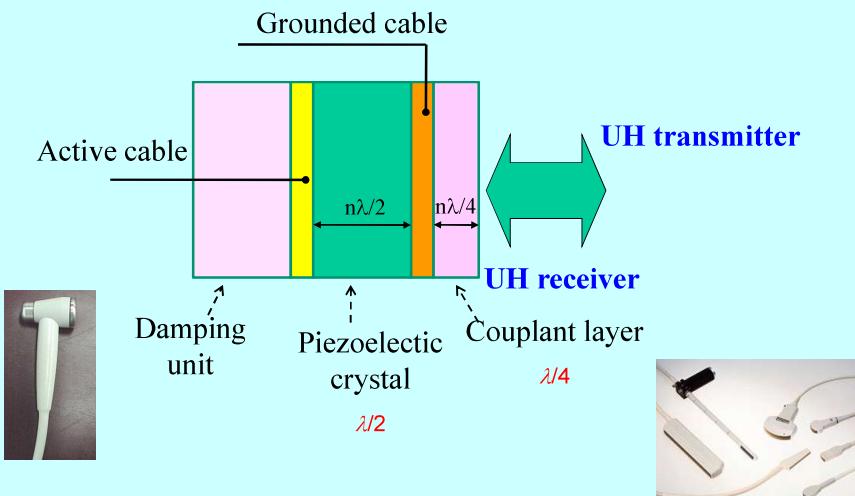
amplifier with positive feedback

$$A_{U, \text{feedback}} = \frac{A_U}{1 - \beta A_U}$$



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## Detection/Generation of US - Ultrasound transducer



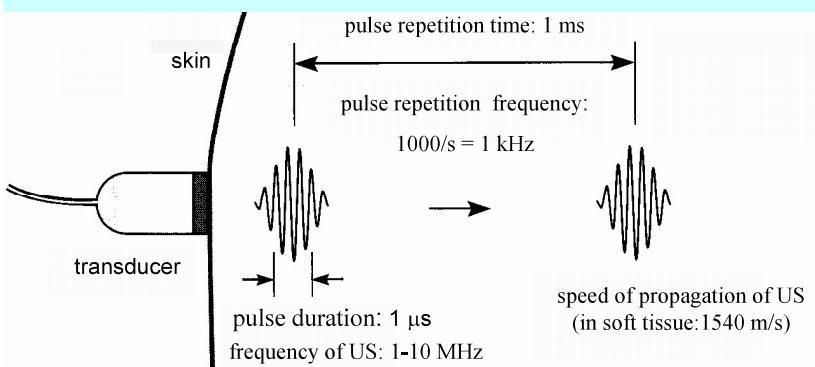
Question of the week

Why is the speed of propagation of US higher in bones than in soft tissues?

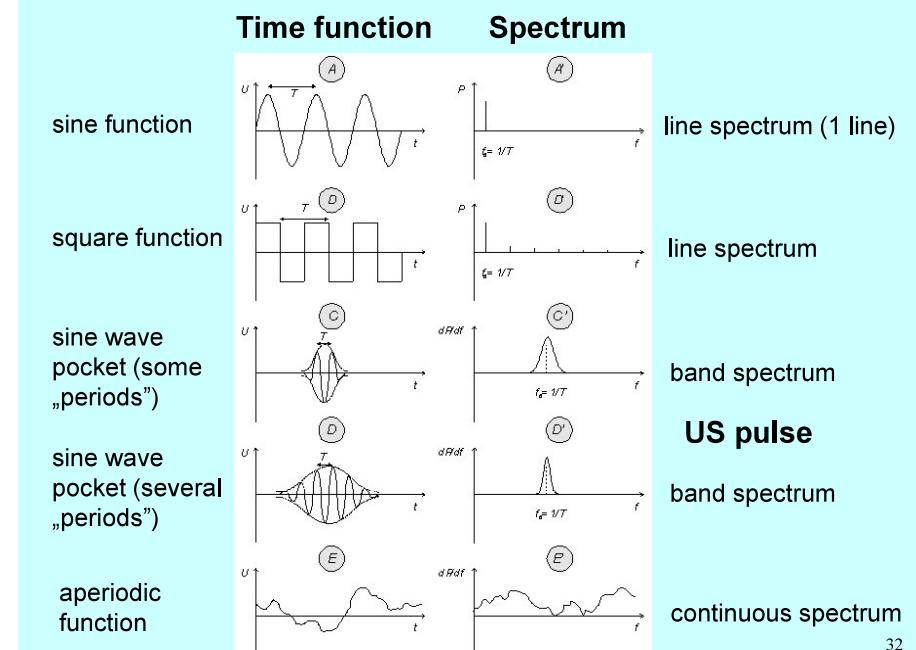
## Characteristic of US pulses

transducer: transmitter and receiver is the same unit

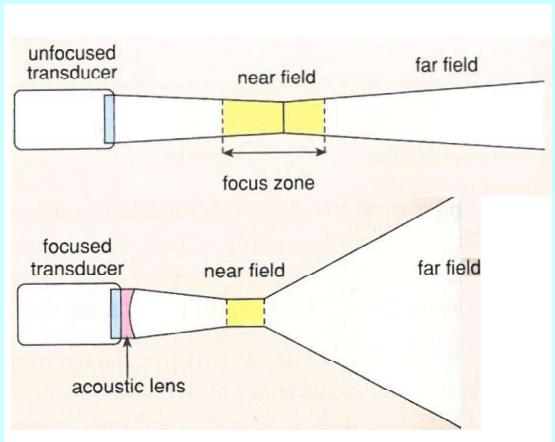
**time sharing mode:** pulses instead of continuous wave US



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## *Focusing of the beam*



Focusing increases the divergence of the beam in the far field regime and reduces the depth sharpness.