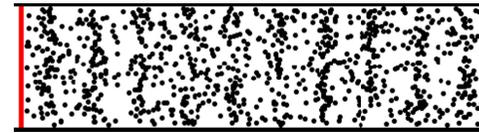
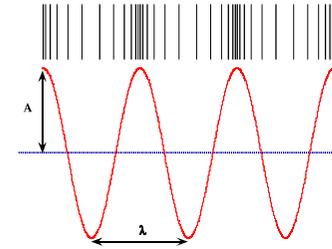


# SOUND, ULTRASOUND

MIKLÓS KELLERMAYER

## SOUND

Longitudinal  
mechanical wave  
(pressure wave)



Longitudinal wave

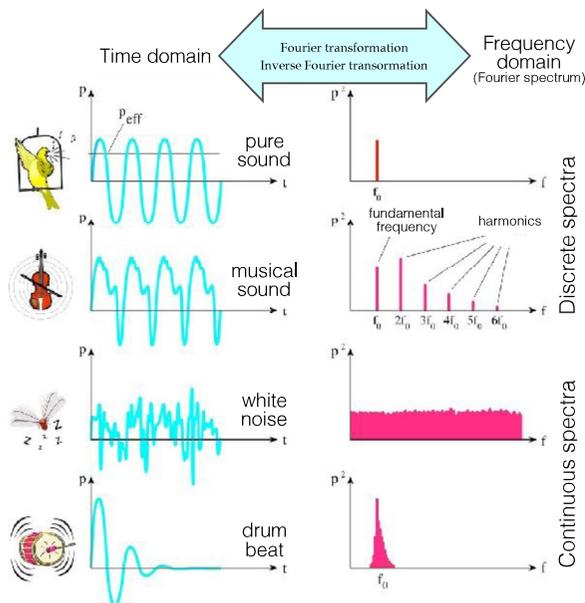


Transverse wave

Harmonic oscillation:  $y(t) = A \sin(ft + \varphi)$

$y$ =actual pressure;  $t$ =time  
 $f$ =frequency (Hz);  $A$ =amplitude  
 $\varphi$ =phase shift

## SOUNDS AND THEIR SPECTRA



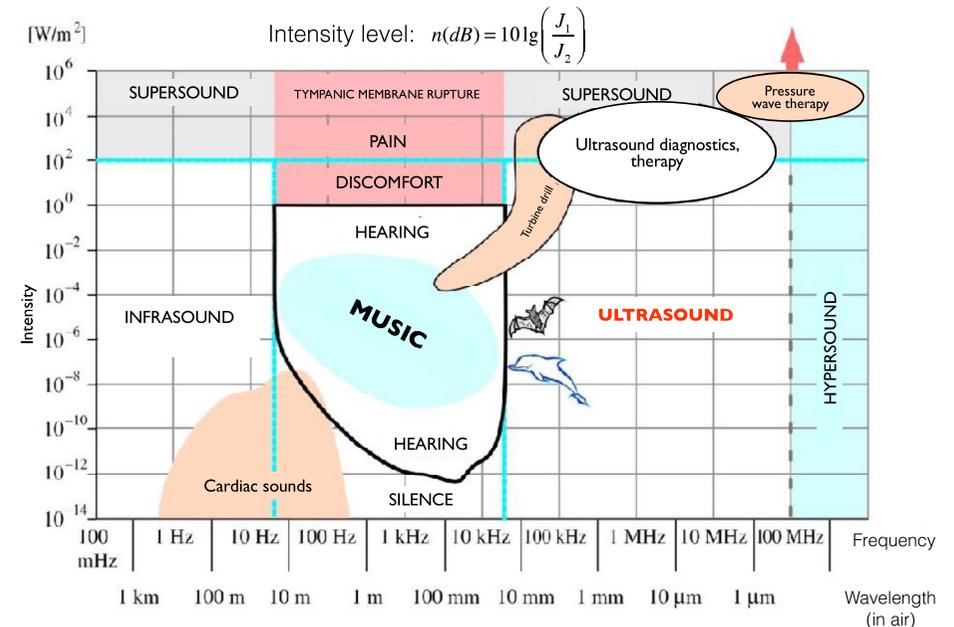
Fourier theorem:  
any function can be  
expressed as the sum of a  
fundamental sine wave and  
its harmonics

Steps of Fourier  
transformation:



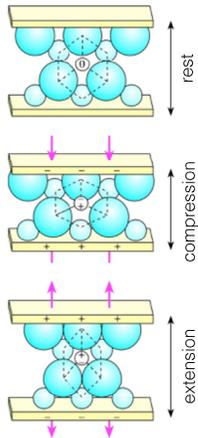
Octave - frequency  
difference with a  
2:1 ratio

## FREQUENCY AND INTENSITY OF SOUNDS



# GENERATION AND DETECTION OF ULTRASOUND: PIEZOELECTRIC EFFECT

Piezoelectricity (Pierre and Jacques Curie, 1880): "pressure electricity"



1. Direct piezoelectric effect: electrical polarization ( $P$ ) that occurs in certain crystals upon mechanical deformation:

$$P = d \times \frac{F}{A}$$

$d$ =piezoelectric coefficient (m/V)  
 $F/A$ =stress

Application: detection of ultrasound, piezoelectric lighter



2. Inverse piezoelectric effect: deformation in a crystal placed in electric field:

$$\frac{\Delta l}{l} = E \times d$$

$\Delta l/l$ =strain  
 $E$ =electric field  
 $d$ =piezoelectric coefficient (m/V)

Application: generation of ultrasound

Resonance: frequency of alternating voltage coincides with the Eigen (resonance) frequency of the crystal. Typical ultrasound frequencies > 1 MHz.

Electrical polarization upon mechanical deformation, Centers of + negative - charges are spatially separated.

Frequently used piezoelectric crystals: quartz ( $d=3 \times 10^{-12}$  m/V), ammonium-dihydrogen phosphate, lead-zirconium-titanate (PZT), etc.

# PROPERTIES OF ULTRASOUND: PROPAGATION

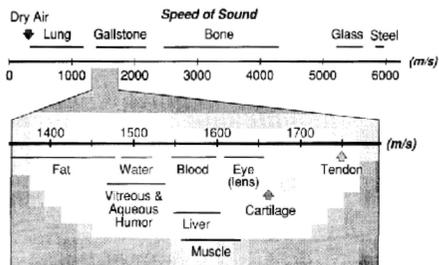
Speed of propagation ( $S, v, c$ ):  $S = f \lambda = \frac{\lambda}{T}$

US propagates solely as a longitudinal wave in gases and liquids; in solids it may also propagate as a transverse wave.

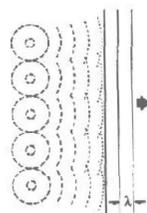
Speed depends on the properties of the medium:

$$S = \sqrt{\frac{Y}{\rho}} = \sqrt{\frac{1}{k\rho}}$$

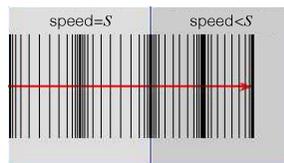
$Y$  = Young's modulus  
 $\rho$  = density of the medium  
 $k$  = compressibility of the medium



Speed of ultrasound in different media



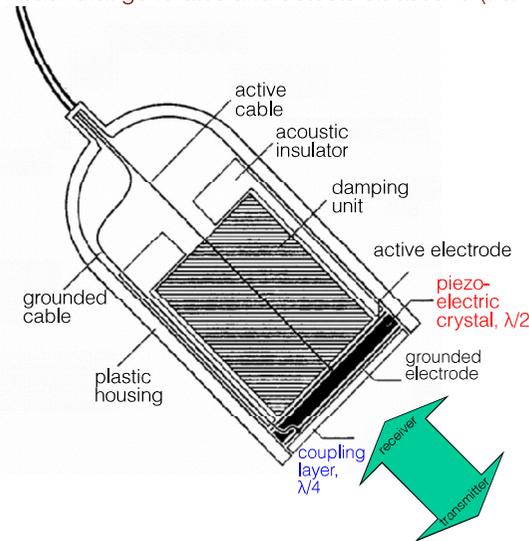
Formation of wavefront: based on Huygens-principle



During propagation frequency is unchanged. Wavelength varies with speed.

# THE ULTRASOUND TRANSDUCER

"Head" that generates and detects ultrasound (*transducere* ~ to lead across, to convert)



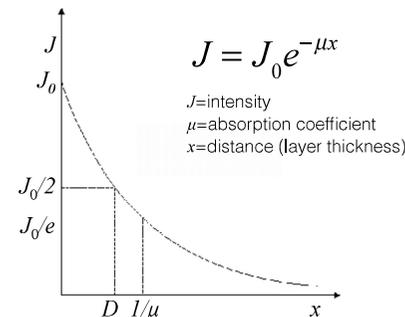
Shape and size of the ultrasound transducers vary with applications.

# PROPERTIES OF ULTRASOUND: ATTENUATION

Attenuation: decrease of intensity, "weakening"

1.  $1/r^2$  law ("inverse square law"): intensity decreases with the inverse of the square of propagation distance (sound power is distributed across a spherical surface).

2. Absorption: Mechanisms: a. incoherent molecular motion (heat), b. viscosity of the medium



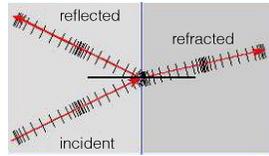
Material	$D$ ( $f=1$ MHz)
Air	~ 1 cm
Water	few m

# PROPERTIES OF ULTRASOUND: REFRACTION AND REFLECTION

## Refraction

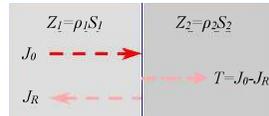
Change in the direction of propagation at surfaces bounded by media in which the speed of US propagation is different. Refraction increases with increasing angle of incidence. Snell's Law applies:

$$\frac{\sin \alpha}{\sin \beta} = \frac{S_1}{S_2}$$



## Reflection

Part of the acoustic intensity is reflected from surfaces bounded by media with different acoustic impedances. Reflected intensity increases with increasing difference in the acoustic impedance of the media. At certain surfaces (e.g., soft tissue/bone), total reflection may occur.



$Z = \rho S$   
 $Z_1 = \rho_1 S_1$      $Z_2 = \rho_2 S_2$   
 $\rho$  = density  
 $S$  = speed of propagation

Reflectivity (reflection coefficient):

$$R = \frac{J_R}{J_0} = \left( \frac{Z_1 - Z_2}{Z_1 + Z_2} \right)^2$$

$$Z = \rho S$$

"Total" reflection:  
 $Z_1 \ll Z_2, R \approx 1$

Optimal coupling:  
 $Z_{coupling} \approx \sqrt{Z_{source} Z_{skin}}$

boundary surface	R
muscle/blood	0,001
fat/liver	0,006
fat/muscle	0,01
bone/muscle	0,41
bone/fat	0,48
soft tissue/air	0,99



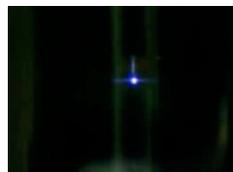
# EFFECTS OF ULTRASOUND

## Primary effects

1. Cavitation: (formation of cavities; cavum = cavity): short-lived cavities generated upon the breakdown of cohesion forces between participating molecules.

Sonoluminescence: photon emission upon the collapse of the cavity. Mechanism:

- In the expansive phase of the pressure wave, bubbles are formed (5-70  $\mu\text{m}$ ).
- In the compressive phase, the bubbles contract.
- The temperature inside the bubble may reach levels up to 20.000-30.000 °K.
- The excited noble gas (Ar, Xe) atoms remaining in the bubbles emit photons.



Light-emitting bubble in liquid irradiated with US (several MHz)

2. Sound pressure: Pressure exerted on the object standing in the path of US wave. Directly proportional to US intensity.

3. Absorption: Absorption of radiation energy by the medium, leading to increased temperatures (increases with frequency and layer thickness).

## Secondary effects

1. Mechanical: resonance of particles suspended in the medium (dispersion, cleaning, dentistry, etc.)
2. Chemical: energy absorption may initiate chemical reactions (oxidation, e.g.,... condensation of iodine from KI solution).
3. Biological: Complex mechanisms - bactericidal, fungicidal, virucidal, etc., effects.

# PROPERTIES OF ULTRASOUND: DOPPLER EFFECT

In case of a moving US source, the detected frequency is changed:

- If the source is approaching, then the detected frequency increases.
- If the source is departing, then the detected frequency decreases.



Christian Andreas Doppler (1803 - 1853)

Frequency shift: Doppler shift

$$\text{Doppler shift: } f_o = f_s \frac{S + v_o}{S - v_s}$$

$f_o$ : detected frequency  
 $f_s$ : frequency of source  
 $S$ : speed of propagation of US  
 $v_o$ : speed of the observer  
 $v_s$ : speed of the US source



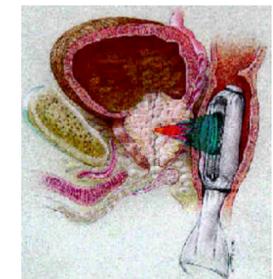
# THERAPEUTIC APPLICATIONS OF ULTRASOUND

The therapeutic applications of US depend on its physical effects

1. Local heating

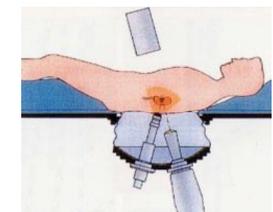
2. Micromassage

3. High Intensity Focused Ultrasound (HIFU):  
 Crushing of prostate tumors



HIFU

Shock wave therapy (not really US!)  
 ESWL (Extracorporeal Shockwave Lithotripsy)  
 Crushing of kidney stones



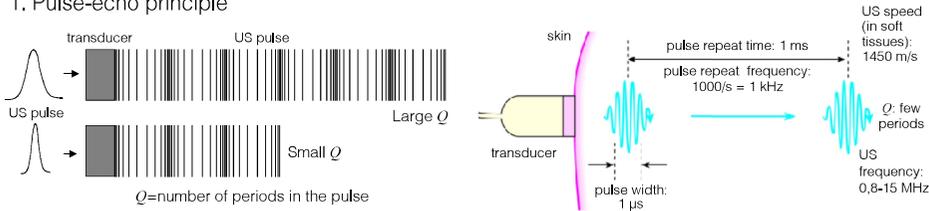
ESWL

4. Physical therapy

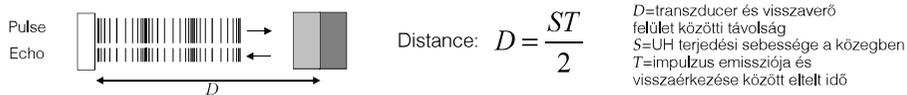
# DIAGNOSTIC APPLICATIONS OF ULTRASOUND

Imaging method. Its basis is differential absorption and reflection by the bounding media. The acoustic impedance of the bounding media are different.

## 1. Pulse-echo principle



## 2. Distance measurement with ultrasound

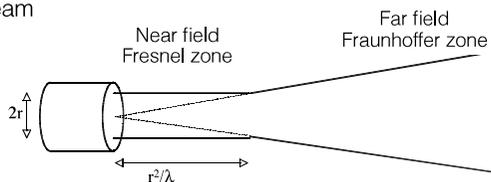


# DIAGNOSTIC APPLICATIONS OF ULTRASOUND

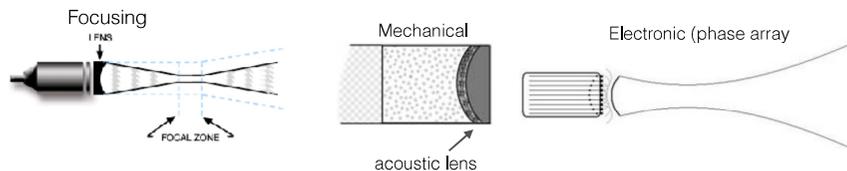
## 4. Time-gain compensation

Intensity decreases with increasing distance (attenuation). Acoustic attenuation can be partially compensated for by amplification of the detected signal. After pulse emission, gain is constantly increased as a function of time.

## 5. Ultrasound beam

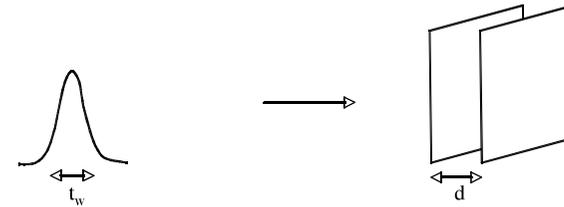


Upon increasing frequency, the length of the Fresnel zone increases, divergence decreases: the beam may be better focused.



# DIAGNOSTIC APPLICATIONS OF ULTRASOUND

## 3. Axial resolving power



Condition of resolving smallest axial distance ( $d$ ):

$$St_w < 2d$$

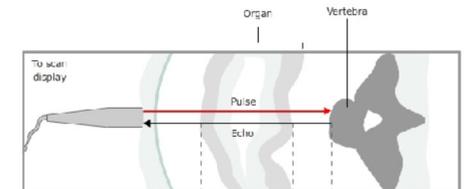
At a given frequency, axial resolution increases with decreasing  $Q$  value.  
At a given  $Q$  value the axial resolution increases with increasing frequency.

# DIAGNOSTIC APPLICATIONS OF ULTRASOUND

## 6. Ultrasound imaging modes:

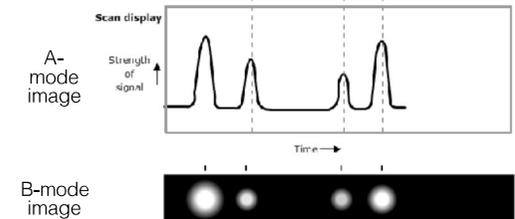
### A-mode (Amplitude-modulated):

Single transducer; beam propagates along a single line. The echo is detected as a voltage pulse on an oscilloscope.



### B-mode (Brightness):

Voltage pulses are displayed as points of varying gray level. Grayscale density is proportional to voltage amplitude: the greater the voltage the brighter the point and vice versa.

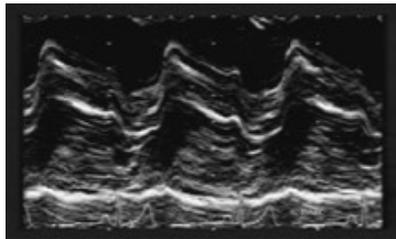


# DIAGNOSTIC APPLICATIONS OF ULTRASOUND

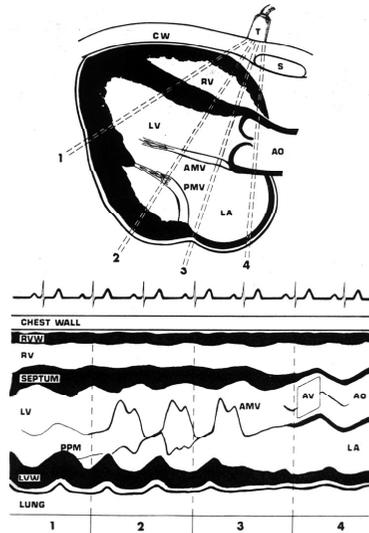
M-mode (time Motion)

Displays periodic motions as a function of time (e.g., echocardiography)

X-axis: time  
Y-axis: 1-dimensional B-mode image (line)

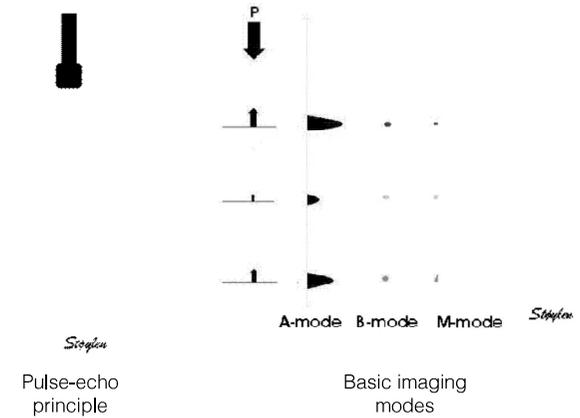


Mitral stenosis



# DIAGNOSTIC APPLICATIONS OF ULTRASOUND

One-dimensional imaging modes - comparison



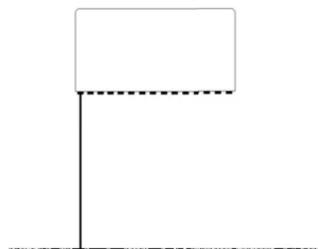
Pulse-echo principle

Basic imaging modes

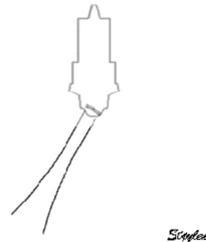
# DIAGNOSTIC APPLICATIONS OF ULTRASOUND

2-dimensional B-mode (Brightness)

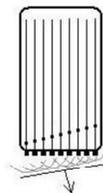
Scanning is carried out in two dimensions



"Linear array"  
(hundreds of small piezo crystals arranged linearly)



Mechanical scanning  
(single piezo crystal is scanned along a line)

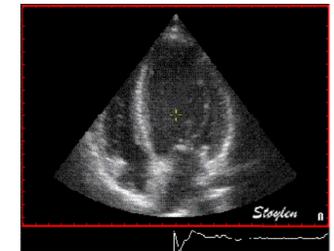
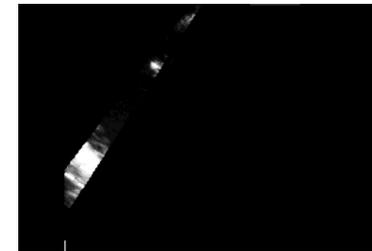


Electronic scanning  
(phase array)

# DIAGNOSTIC APPLICATIONS OF ULTRASOUND

2-dimensional B-mode (Brightness)

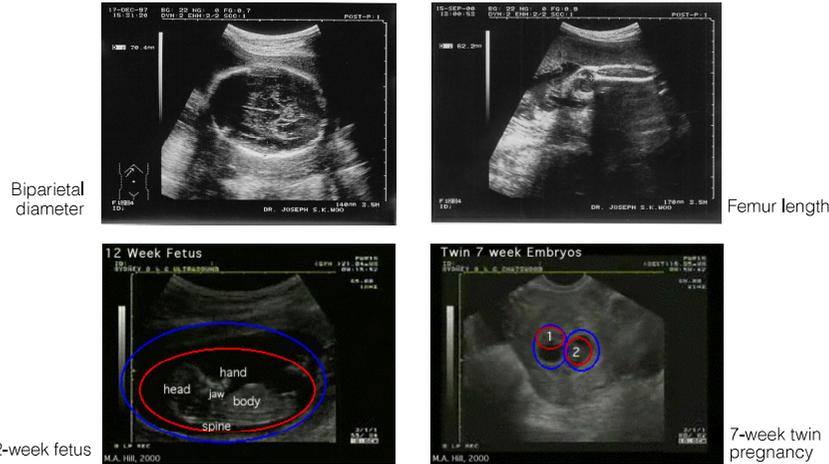
With fast scanning, real-time images may be recorded.



# DIAGNOSTIC APPLICATIONS OF ULTRASOUND

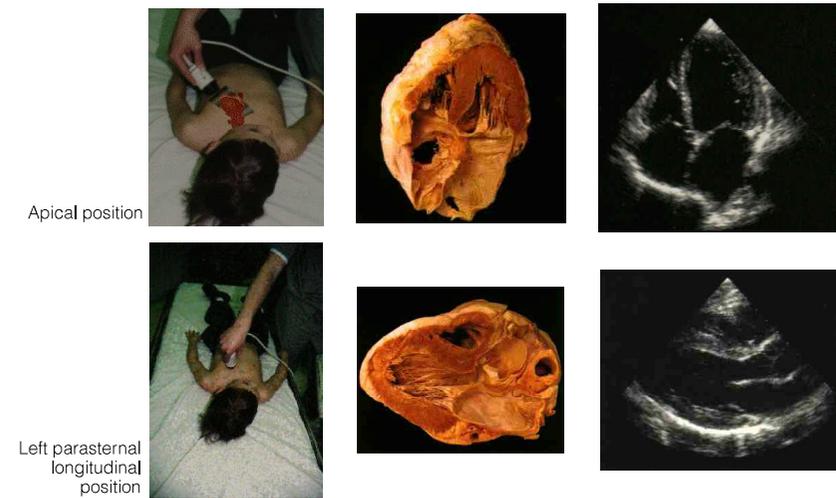
A 2D B-mode in obstetrics and gynecology

Gestational age, developmental pathology, placenta position, fetus position.



# DIAGNOSTIC APPLICATIONS OF ULTRASOUND

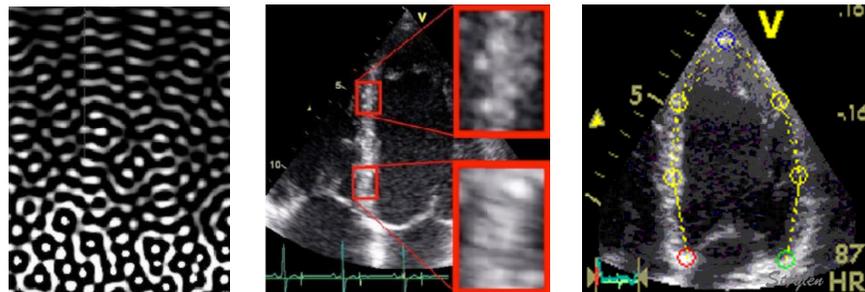
A 2D B-mode in cardiology



# DIAGNOSTIC APPLICATIONS OF ULTRASOUND

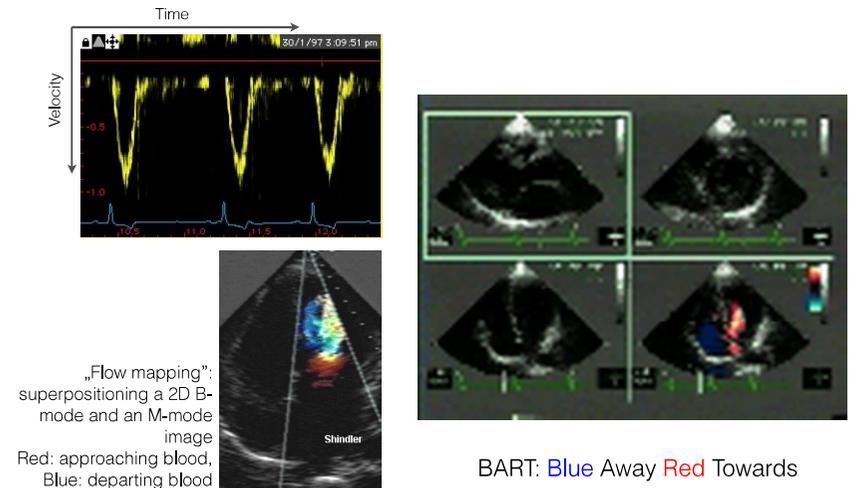
A 2D B-mode in cardiology

Speckle tracking



# DIAGNOSTIC APPLICATIONS OF ULTRASOUND

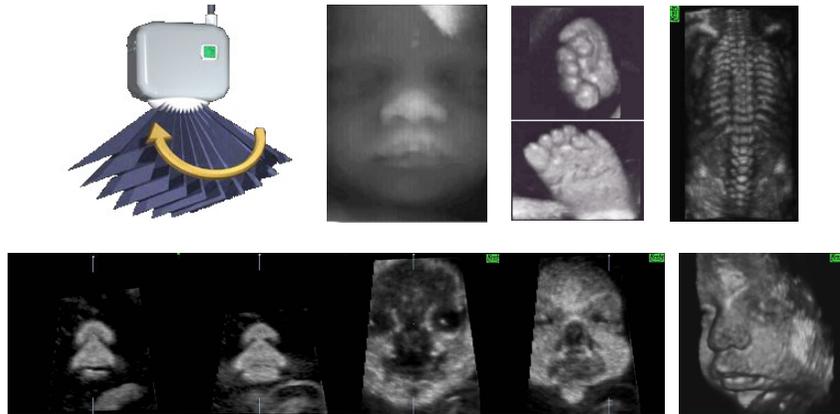
Cardiological applications: Doppler cardiography



# DIAGNOSTIC APPLICATIONS OF ULTRASOUND

3-dimensional ultrasound

Rapid transducer capable of rotating the fan-like beam. Computer-based image reconstruction.



# DIAGNOSTIC APPLICATIONS OF ULTRASOUND

4-dimensional ultrasound: temporally resolved 3D ultrasound



# DIAGNOSTIC APPLICATIONS OF ULTRASOUND

3-dimensional ultrasound

The spatially resolved images may be presented and manipulated at will.

