

CARDIOVASCULAR SYSTEM: BIOPHYSICS OF CIRCULATION CARDIAC BIOPHYSICS

MIKLÓS KELLERMAYER

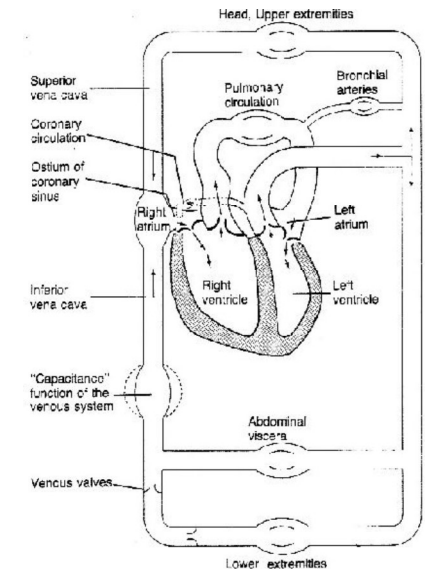
The vascular system is a closed vessel system returning into itself

A. Function:

Maintenance of environmental parameters of cells ("steady state")
Transport:
Gases
Metabolites
Hormones, signal transmitters
Immunoglobulins
Heat

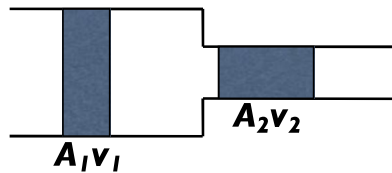
B. Hemodynamic requirements:

Slow (matches diffusion-driven processes)
Steady (no fluctuations)
Unidirectional



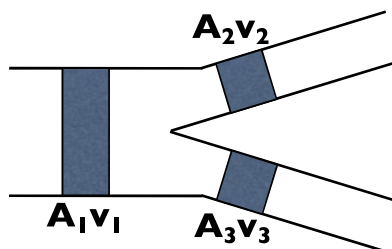
Fluid flow in bifurcating vessel system

Continuity equation



$$A_1v_1 = A_2v_2 = \text{const}$$

A = cross-sectional area
 v = flow rate



$$A_1v_1 = A_\Sigma(v)_{\text{average}} = \text{const}$$

A_Σ = total cross-sectional area

THERMODYNAMIC CURRENTS

- Natural processes are rarely reversible.
- If there are inequalities in the intensive variables at different locations within the system, thermodynamic currents arise.
- Thermodynamic currents aim at the restoration of equilibrium.
- Extensive variables flow.

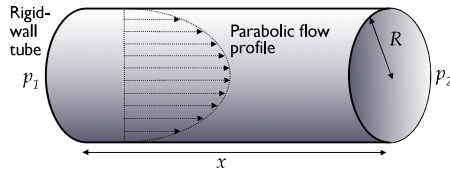
Thermodynamic current	Relevant intensive variable (its difference maintains current)	Current density	Physical law
Heat flow	Temperature (T)	$J_E = -l \frac{\Delta T}{\Delta x}$	Fourier
Volumetric flow	Pressure (p)	$J_V = -\frac{R^2}{8h} \frac{\Delta p}{\Delta x}$	Hagen-Poiseuille
Electric current	Electric potential (ϕ)	$J_Q = -\frac{1}{r} \frac{\Delta j}{\Delta x}$	Ohm
Material transport (diffusion)	Chemical potential (μ)	$J_n = -D \frac{\Delta c}{\Delta x}$	Fick

Laws of flow in viscous fluids II.

Hagen-Poiseuille's law



Thermodynamic current	Relevant intensive variable (its difference maintains current)	Current density	Physical law
Volumetric flow	Pressure (p)	$J_V = -\frac{R^2}{8\eta} \frac{\Delta p}{\Delta x}$	Hagen-Poiseuille



$$J_V = \frac{V}{tA} = \frac{R^2}{8\eta} \frac{\Delta p}{\Delta x}$$

N.B. 1: $A = R^2 \pi \Rightarrow I_V = \frac{V}{t} = -\frac{R^4 \pi}{8\eta} \frac{\Delta p}{\Delta x}$

N.B. 2: $I_V = -\frac{R^4 \pi}{8\eta \Delta x} \Delta p \Rightarrow -\Delta p = R_{tube} \cdot I_V \Rightarrow U = R \cdot I$
Ohm's law!

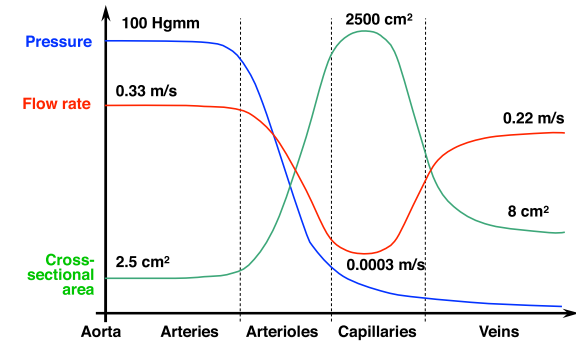
N.B. 3: $\frac{\Delta v}{\Delta r} \sim r \Rightarrow \left(\frac{\Delta v}{\Delta r} \right)_{\max} = R \Rightarrow \tau_{\max} = R$

Shear stress is maximal at the tube wall because of the parabolic flow profile.

V = volume
 t = time
 R = tube radius
 η = viscosity
 p = pressure
 x = tube length
 $V/t = I_V$ = volumetric flow rate
 $\Delta p / \Delta x$ = pressure gradient, maintained by $p_2 - p_1$ (negative!)
 A = cross-sectional area of tube
 I_V = volumetric flow rate

Structure and physical properties of the vascular system

	Diameter	Total cross-sectional area
Aorta	25 mm	2.5
Artery	4 mm	20
Arteriole	30 μ	40
Capillary	8 μ	2500
Venule	20 μ	250
Vein	5 mm	80
Vena cava	30 mm	8



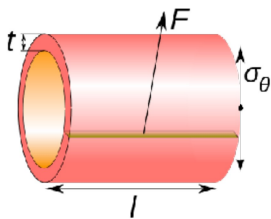
- **Pressure** on blood vessel wall: "**blood pressure**". Pressure drop along vessel maintains blood flow.
- Reason of **pressure drop**: flow resistance - most of energy is converted to heat.
- **Flow rate** and total **cross-sectional area** change inversely (based on equation of continuity, $A_v = \text{constant}$).
- Flow rate typically does not exceed the **critical** (see Reynolds number), and flow remains laminar. (Exceptions: behind aortic valve, constricted vessels, low-viscosity conditions, Korotkoff sound).
- **Arterioles** (vessels containing smooth muscle, under vegetative innervation) are pressure-regulators: "**resistance vessels.**"
- Most of blood volume in veins: "**capacitance vessels.**"

Wall tension and blood pressure

Circumferential stress (σ_θ) depends on blood pressure: (Young-Laplace - equation)

$$\sigma_\theta = \frac{P \cdot r}{t}$$

P = blood pressure
 r = radius of tube
 t = wall thickness

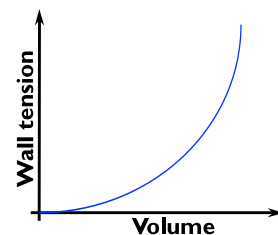


$$\sigma_\theta = \frac{F}{t \cdot l}$$

F = force
 l = tube length

Wall tension or circumferential stress is the average force exerted circumferentially (perpendicular to both the axis and the radius) in the cylinder wall.

Vessel wall displays non-linear elastic properties



Determinants of vascular elasticity:

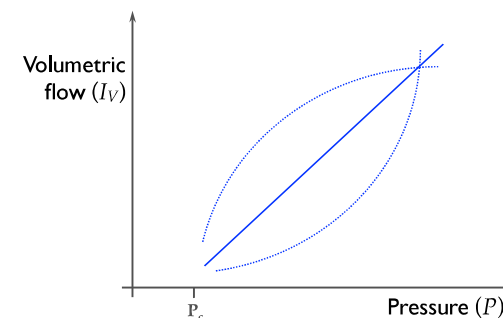
Elastin
Collagen
Smooth muscle

Implications of vascular elasticity:

Storage of potential (elastic) energy
Dampening of pressure pulses
Constant flow rate

Relationship between flow intensity and pressure

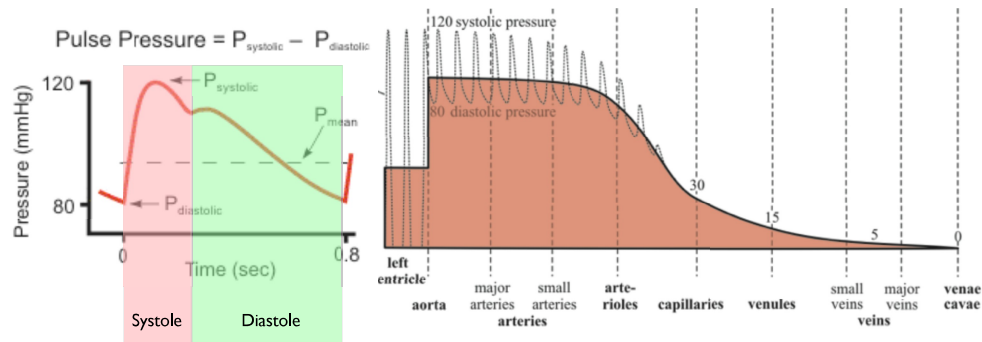
Below certain pressure vessels collapse and flow ceases



N.B.:

- The curves intersect the pressure axis at values greater than 0 (critical closing pressure, P_c).
- P_c in arteries, at resting conditions, is ~ 20 Hgmm.
- During blood pressure measurement we compress the limb by raising the cuff pressure above the local P_c .

Dynamic pressure-changes in the arterial system



Because of vessel wall elasticity, pressure fluctuations are damped.

Capillary circulation, fluid exchange

1. Capillaries:

Length: 400-700 μm
Diameter: 0.5 μm

2. Open state depends on function

Number of open capillaries in muscle:
Rest - 5/mm²
Activity - 200/mm²

3. Capillary fluid exchange

fluid movement between blood plasma and interstitium
driven by: difference in blood pressure and colloid osmotic pressure
Colloid osmotic (oncotic) pressure:
osmotic pressure caused by the presence of colloidal proteins (2.6 kPa)



	Arterioles	Capillaries	Venules
Bood pressure	4.0 kPa	2.6 kPa	1.3 kPa
Colloid osmotic pressure	2.6 kPa	2.6 kPa	2.6 kPa

Auxiliary factors of circulation

1. Arterial elasticity

elastic fibers \rightarrow storage of potential energy

2. Venous valves (Harvey's experiment)

"Exercitatio anatomica de motu cordis et sanguinis in animalibus" (1628)

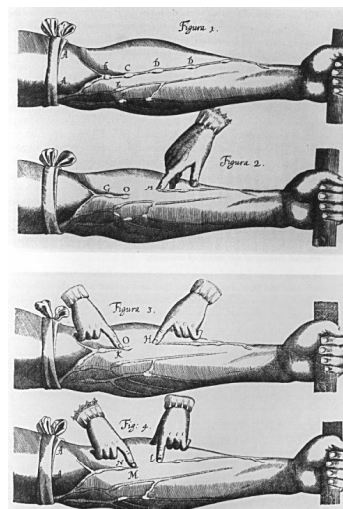


3. Muscle action

4. Negative intrathoracic pressure

5. "Up-and-down" movement of atrioventricular plane

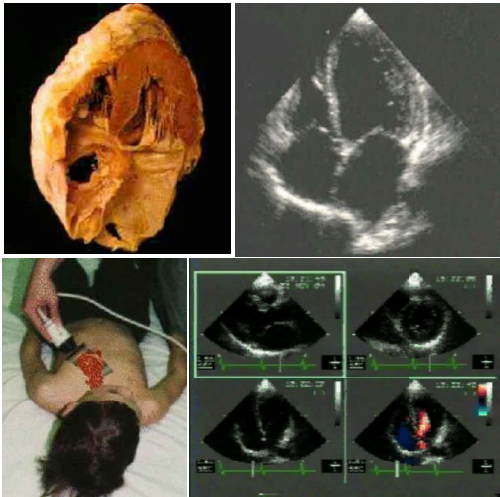
Harvey's experiment (1628)



CARDIAC BIOPHYSICS

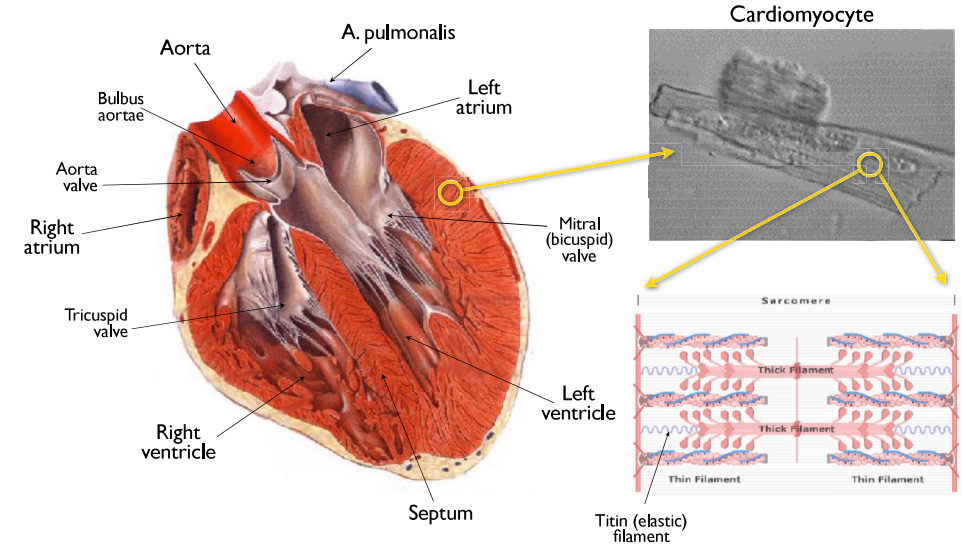
Heart:

Pump of the circulatory system

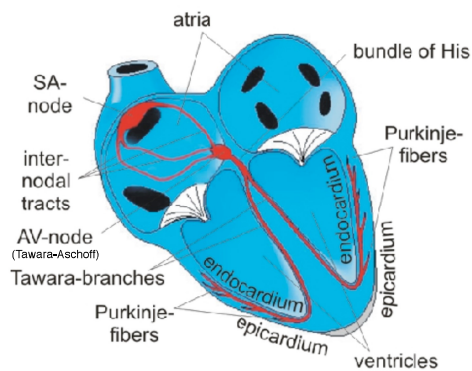


	Number of contractions	Expelled blood volume
1 min	~70	~6 l
1 day	~100.000	~8600 l
Life (70 yrs)	~2.5 x 10 ⁹	~220 x 10 ⁶ l

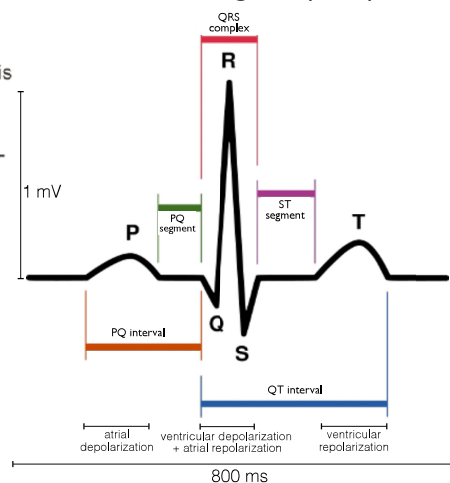
Schematic structure of the human heart



Activation of coordinated cardiac contractions

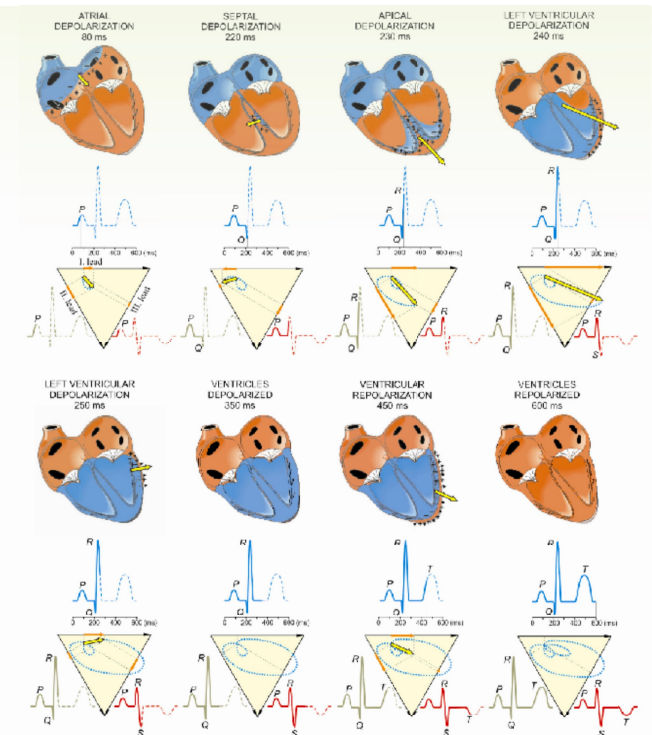


Electrocardiogram (ECG)



EKG:

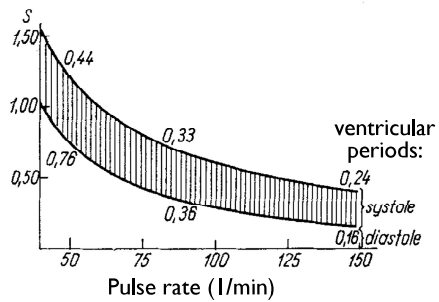
Vectorial projections (according to leads) of the resultant dipole (integral vector) that changes in time and space during myocardial depolarization and repolarization.



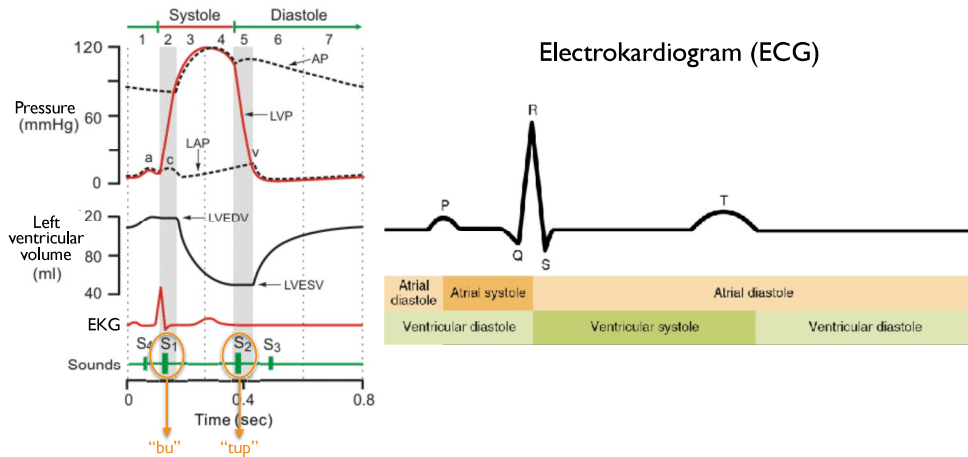
The cardiac cycle

Contraction (systole) - relaxation (diastole) cycle of the heart

	systole	diastole
atrium	0,1 s	0,7 s
ventricle	0,3 s	0,5 s

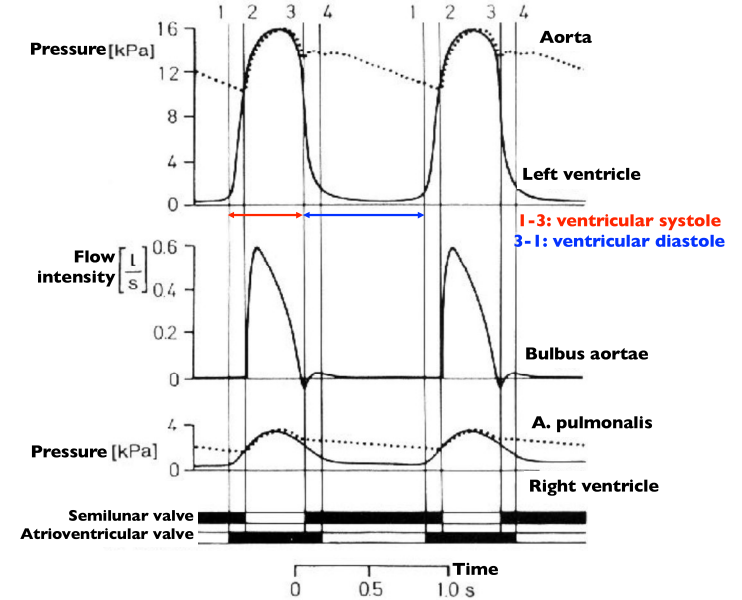


Events of the cardiac cycle 2.

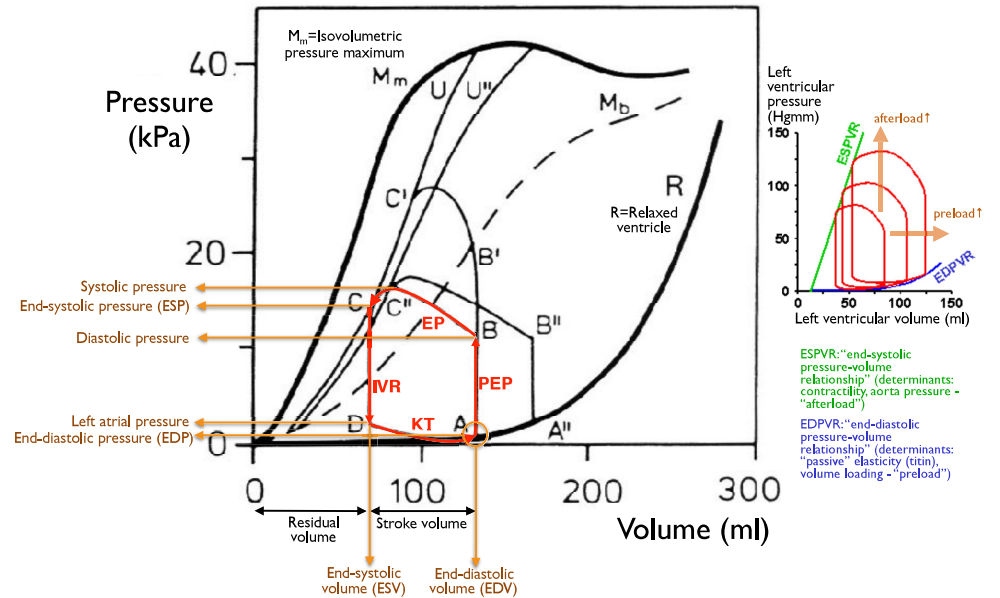


Events of the cardiac cycle I.

1-2: pre-ejection period (PEP) **2-3:** ejection period (EP) **3-4:** isovolumetric relaxation (IVR) **4-1:** ventricular filling (VF)

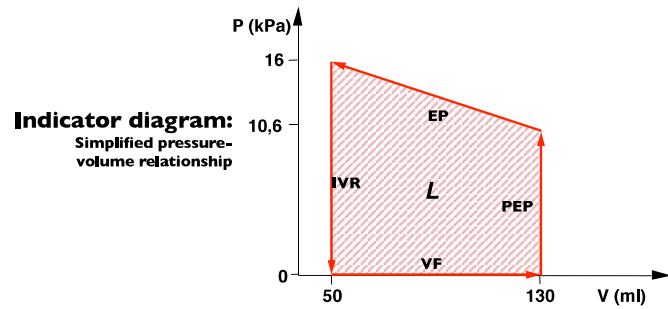


Pressure-volume diagram of left ventricle



Work of the heart

(work of the left ventricle)



$$L = p\Delta V + \frac{1}{2}mv^2$$

$p\Delta V$ =static (volumetric) component
 $1/2mv^2$ =dynamic component
 p =pressure
 ΔV =**stroke volume**

$$13,3 \cdot 10^3 \text{ N/m}^2 \times 0,08 \cdot 10^{-3} \text{ m}^3 + \frac{1}{2} 0,08 \text{ kg} \times (1 \text{ m/s})^2 = 1,06 \text{ Nm} + 0,04 \text{ Nm} = 1,1 \text{ J}$$