

## Physical Foundations of Dental Materials Science

### 7. Mechanical properties of materials 1. Elasticity

Keywords:

- ❖ 1 Stress-strain
- ❖ 2 Elasticity
- ❖ 3 Deformations

**E-book**  
chapter 14, 15.

**Problems:** 4.1, 4.3, 4.4, 4.5, 4.6, 4.9, 4.11, 4.16, 4.17, 4.18, 4.21, 4.22, 4.23, 4.24.

1

## Mechanical properties of materials

Stiffness, elasticity, toughness, hardness are the most important parameters when considering mastication, implantology or orthodontics.

Mechanical stress (force) is applied on material.

↓

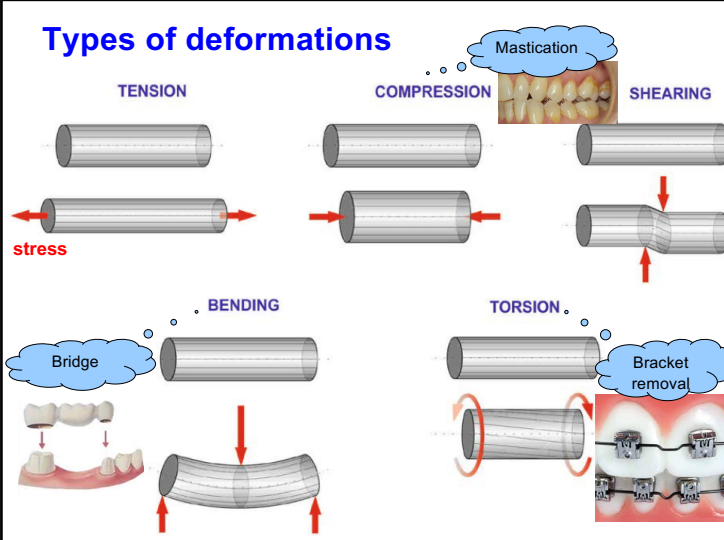
The consequence is usually some kind of deformation.  
(change in shape depends on the direction and point of application)

↓

Depending on the materials mechanical properties, deformation may be reversible or irreversible.

2

## Types of deformations



**TENSION**

**COMPRESSION**

**SHEARING**

**BENDING**

**TORSION**

stress

Mastication

Bridge

Bracket removal

3

**elastic** *adjective* able to resume its normal shape spontaneously after being stretched or compressed

**rigid** *adjective* unable to bend or be forced out of shape; not flexible

**plastic** *adjective* relating to the permanent deformation of a solid without fracture by the temporary application of force

**strong** *adjective* able to withstand force, pressure, or wear

**weak** *adjective* liable to break or give way under pressure; easily damaged

**solid** *adjective* firm and stable in shape; not liquid or fluid, strongly built or made of strong materials

**tough** *adjective* resistant to fracture or breaking

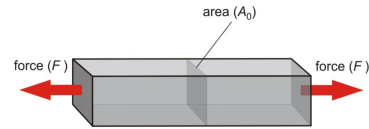
**brittle** *adjective* liable to break easily

4

## Basic concepts

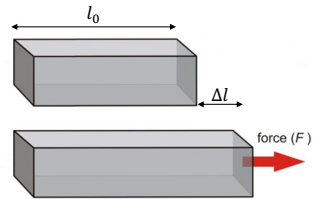
### Stress

$$\sigma = \frac{F}{A_0} \quad \text{Dimension: } \left[ \frac{N}{m^2} = Pa \right]$$



### Strain (deformation)

$$\varepsilon = \frac{\Delta l}{l_0} \quad \text{Dimensionless: } \left[ \frac{m}{m} \right]$$

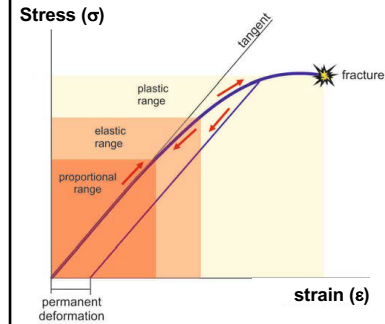


Strain is proportional to stress!

$$\sigma \sim \varepsilon$$

5

## Stress-strain diagram



### Elastic range

Range of reversible deformation. Unloaded length ( $l_0$ ) recovers when released. Hysteresis may occur.

### Proportional range (part of elastic range)

Deformation is linearly proportional to the load. No hysteresis. (see Hooke's law: Biophysics, Resonance lab)

### Plastic range

After a critical stress value, object undergoes irreversible change of its structure. Unloaded length ( $l_0$ ) does not recover. Permanent deformation of object.

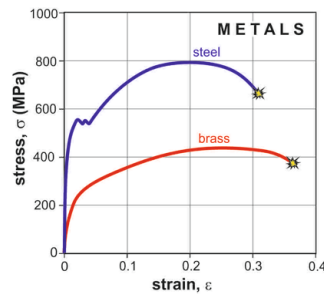
### Fracture

Desintegration of object.

6

## Typical stress-strain curves

### Metals



Short elastic range

Serious plastic range

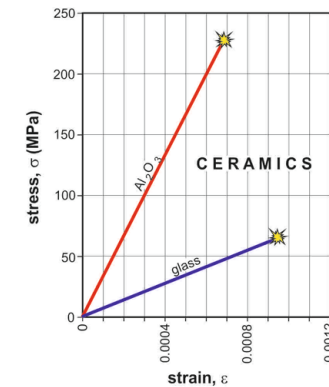
Metals are highly deformable

$\varepsilon_{\max} \sim 0.3$  (~30%)

7

## Typical stress-strain curves

### Ceramics



Extremely short elastic range  
 $\varepsilon_{\max} < 0.001$  (less than ~0.1%)

No plastic range!

Ceramics are brittle, they rupture after a short extension/compression....



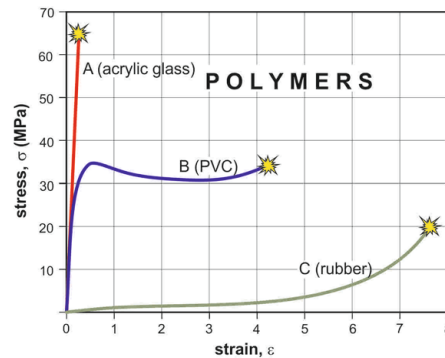
8

8

7

## Typical stress-strain curves

### Polymers



Polymers show various behaviours

Typically they are deformable  $\epsilon_{\max}$  from 0.1 to 8

Acrylic glass  
No plastic range - brittle

PVC  
Large plastic range  
Plastic polymer

Rubber  
Elastic polymer  
 $\epsilon_{\max}$  up to 7-8 (~700-800%)

9

## Additional factors determining the stress-strain diagram

The main decisive is the material's structure (e.g. amorphous or crystalline)

1. Type of stress. (For example the behavior of ceramics is different in the case of tension or elongation.)
2. The shape, size commonly the geometry of the object. (It is more difficult to bend a thicker rod than a thin.)
3. The run-time of the stress: *stress rate*. (For example the glass is broken into pieces using a hammer but a bullet launched by a gun produces a small hole only.)  
Mechanical properties – introduction
4. Temperature. (Some metals are very plastic and tough at room temperature but become more brittle cooling them.)  
These conditions must be presented in the stress-strain diagram.

10

## Hooke's law of elasticity

Strain is proportional to stress!

$$\sigma \sim \epsilon$$

$$\sigma = E\epsilon$$

$$\frac{F}{A_0} = E \frac{\Delta l}{l_0}$$

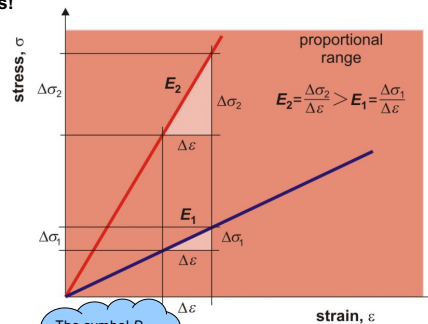
$$F = \frac{EA_0}{l_0} \Delta l$$

$$F = k\Delta l$$

Proportionality coefficients:

**Young's modulus**  
(material stiffness)

$$E = \frac{\sigma}{\epsilon} = \frac{F}{A_0} \frac{l_0}{\Delta l} \quad E = \left[ \frac{N}{m^2} \right] = Pa$$



The symbol  $D$  is also used for spring constant!

**Body stiffness**

$$k = \frac{F}{\Delta l} = \frac{EA_0}{l_0} \quad k = \left[ \frac{N}{m} \right]$$

11

## Quantification of stiffness

Young's modulus of various materials

$$GPa = 10^9 N/m^2$$

### Spring constant

Easy to measure  
Depends on size and shape of object

### Young's modulus

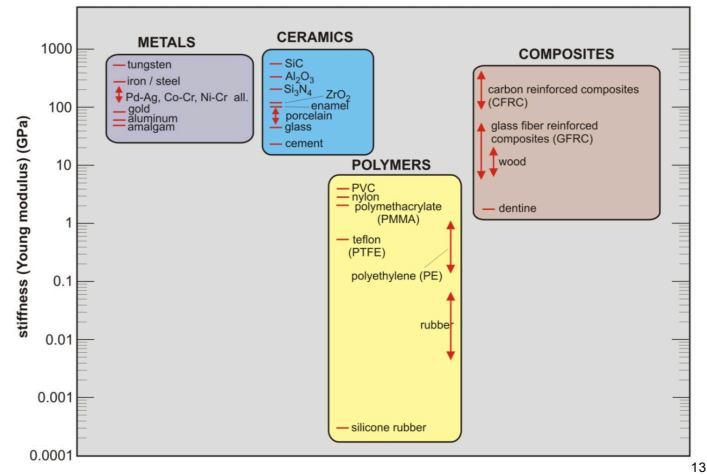
Hard to measure (we need to know the object's dimensions)  
Shape independent

1/E – reciprocal of E is used to express compliance!

material	E (GPa)
dentine	≈ 15
enamel	≈ 100
silicon rubber	≈ 0.0003
steel	200-230
amalgam	50-60
glass	60-90
porcelain	60-110
gold	79
gold alloys	75-110
Pd-Ag alloys	100-120
titanium	110
titanium alloys	105-120
Co-Cr alloys	120-220
Ni-Cr alloys	140-190

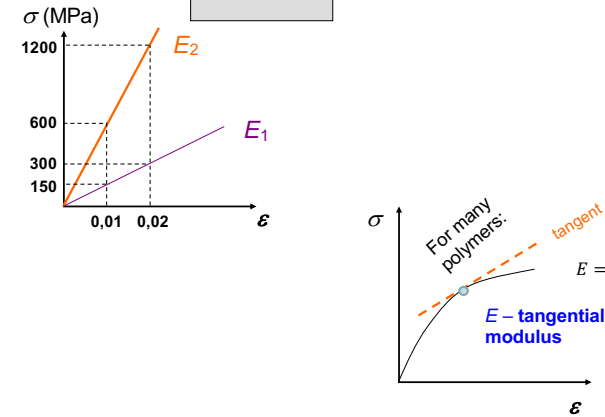
12

## Stiffness



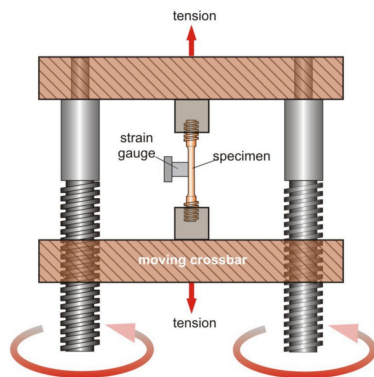
13

Example:



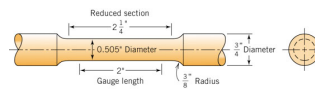
14

## Testing



The result of such measurement is determined by:

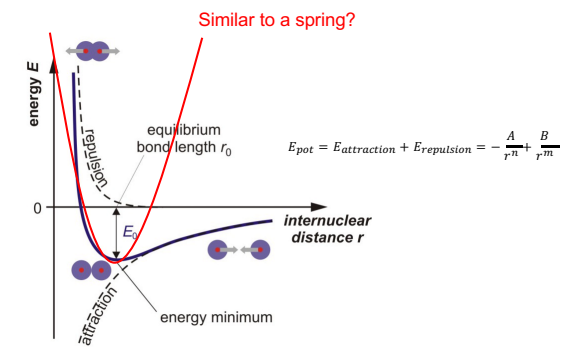
- Type of stress (tension, ...)
- sample geometry
- Timecourse of stress
  - constant
  - changing
- temperature



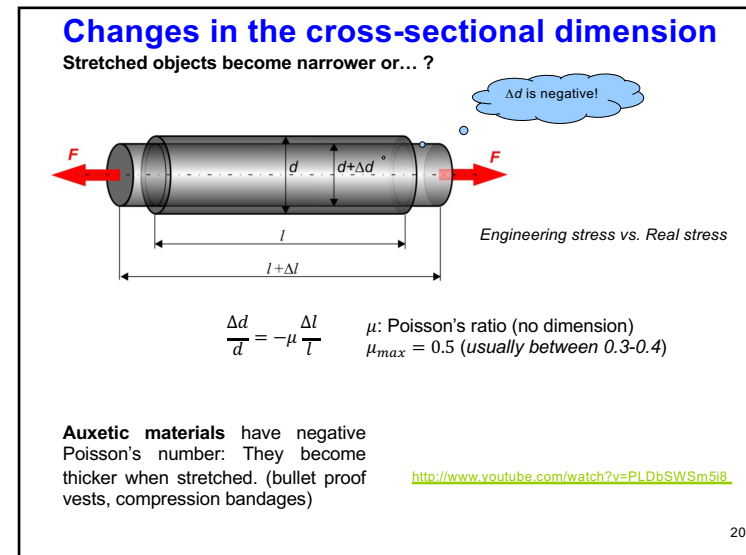
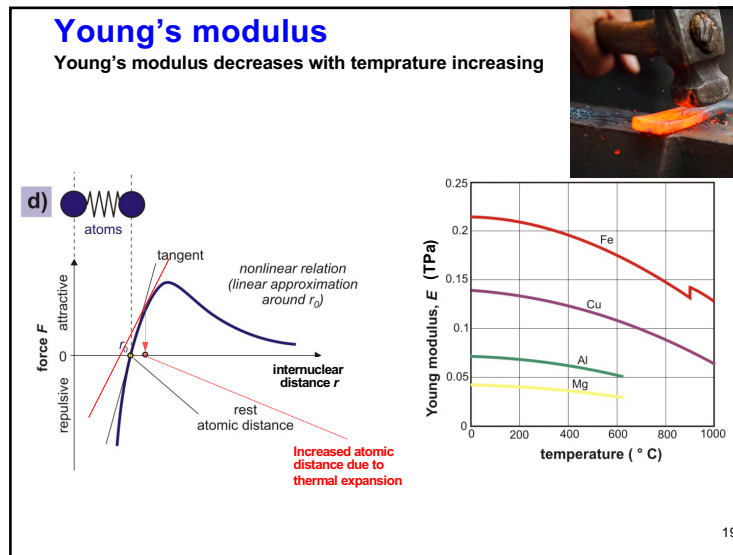
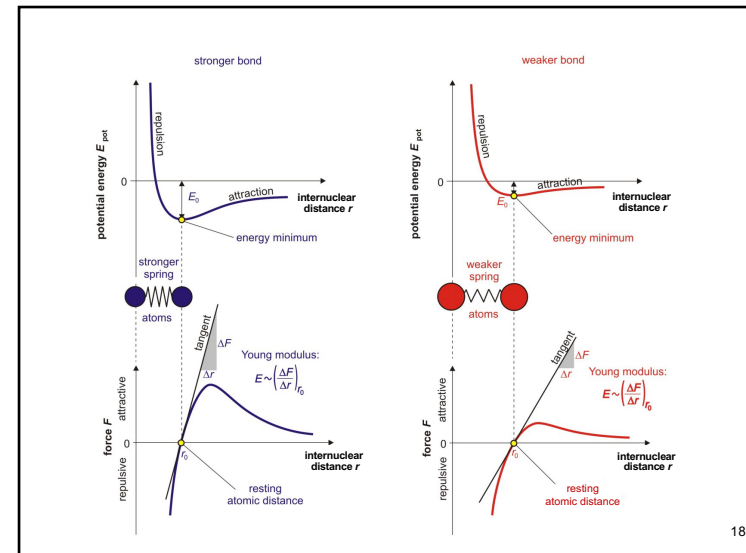
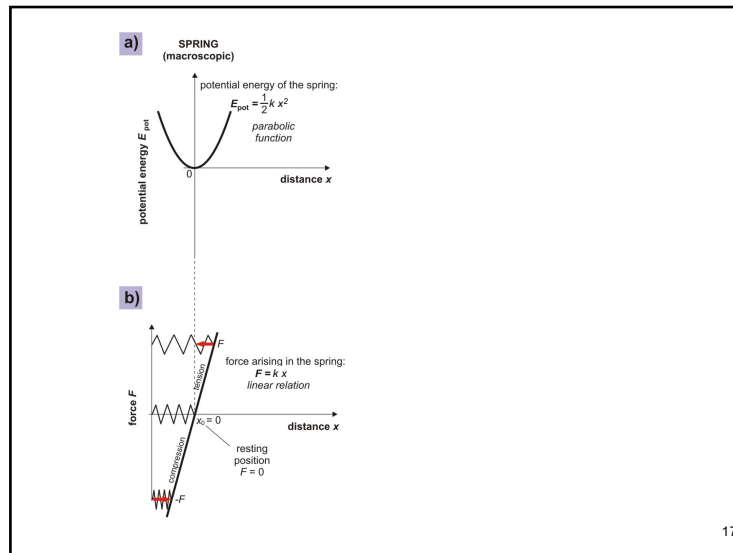
15

## Repetition

Potential energy of chemical bonds (Medical biophysics I/2)



16



## Deformations in other directions

### Compression

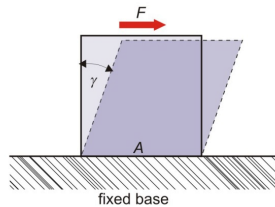
Same as stretch, but signs of stress and strain are opposite, Hooke's law is valid.

### Shear

Force is parallel to the surface,

Shear stress:  $\sigma_{\text{shear}} = \frac{F_{\text{shear}}}{A}$

Strain is characterized by the  $\gamma$  angle



$$\sigma_{\text{shear}} = G\gamma$$

$G$ : Shear modulus  
 $\gamma$ : in radians!

$$G = \frac{E}{2(1 + \mu)}$$

Depends on Young's modulus and Poisson's ratio!

21

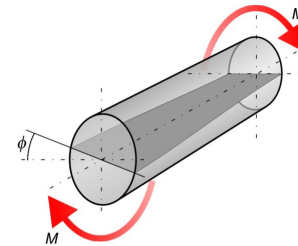
21

## Deformations in other directions

### Torsion

Can be derived from shear. Torque ( $M$ ) is applied on the object.

Angle of torsion ( $\phi$ ) is measured in radians!



$$M = G \frac{r^4 \pi}{2l} \phi$$

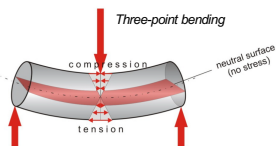
$G$ : Shear modulus  
(contains  $E$  and  $\mu$ )

$r$ : radius  
 $\phi$ : angle of torsion  
 $l$ : length

22

22

## Deformations in other directions



### Bending

Compression on the side of force applied, tension on the opposite side of object. Neutral surface at the middle – does not deform



Cantilever deflection

$$F = 3E \frac{\Theta}{l^3} s$$

$G$ : Force  
 $E$ : Young's modulus  
 $\Theta$ : secondary moment of area  
 $s$ : deflection  
 $l$ : length

Body stiffness in case of deflection

CROSS-SECTIONS SECONDARY MOMENT OF AREA



$$\Theta = \frac{\pi}{4} r^4$$



$$\Theta = \frac{\pi}{4} (r_2^4 - r_1^4)$$



$$\Theta = \frac{1}{12} a b^3$$

In case of bending the force required depends stronger on the shape!

23

23

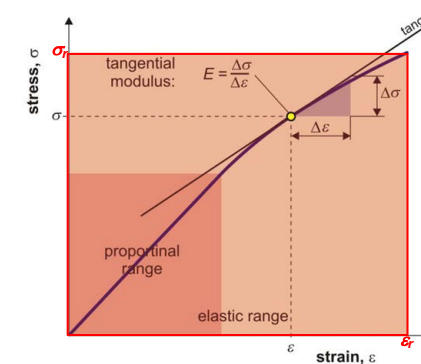
## Elasticity beyond the proportional range

### Elastic limit

End of the elastic range on the y-axis ( $\sigma_f$ ) – maximum reversible strain

### Elastic strain recovery

End of the elastic range on the y-axis ( $\epsilon_f$ ) – maximum reversible stress



Tangential Young's modulus

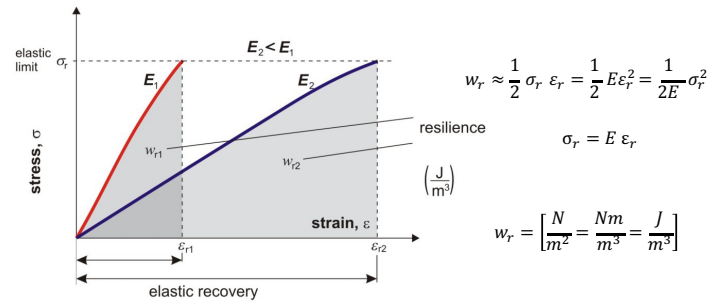
$$E = \frac{\Delta \sigma}{\Delta \epsilon}$$

24

24

## Resilience

Work done on the material per unit volume till the elastic limit.



25

Problems: 4.1, 4.3, 4.4, 4.5, 4.6, 4.9, 4.11, 4.16, 4.17, 4.18, 4.21, 4.22, 4.23, 4.24.

26